

Inhaled insulin for controlling blood glucose in patients with diabetes

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Abstract: Diabetes mellitus is a significant worldwide health problem, with the incidence of type 2 diabetes increasing at alarming rates. Insulin resistance and dysregulated blood glucose control are established risk factors for microvascular complications and cardiovascular disease. Despite the recognition of diabetes as a major health issue and the availability of a growing number of medications designed to counteract its detrimental effects, real and perceived barriers remain that prevent patients from achieving optimal blood glucose control. The development and utilization of inhaled insulin as a novel insulin delivery system may positively influence patient treatment adherence and optimal glycemic control, potentially leading to a reduction in cardiovascular complications in patients with diabetes.

Keywords: diabetes, inhaled insulin, cardiovascular disease, blood glucose

Introduction

Diabetes mellitus is a chronic disease resulting from an inability of the pancreas to produce enough of the regulatory hormone insulin and/or from ineffective systemic use of the insulin that it does produce (WHO 2006). One result of insulin insufficiency is hyperglycemia, or elevated blood glucose (BG), a cardinal manifestation of uncontrolled diabetes that is indicative of a loss of normal metabolic homeostasis. Over time, hyperglycemia and its secondary effects negatively impact both macro- and microvascular targets, resulting variably in cardiovascular disease, stroke, blindness, renal failure, peripheral nerve damage, changes in the skin and joints, lower limb amputations, and premature death (The DCCT/EDIC Research Group 2000; Roglic et al 2005; Yach et al 2006).

The WHO estimates that more than 180 million people worldwide have diabetes (WHO 2006). This number is likely to more than double by 2030 (Wild et al 2004). In 2000, an estimated 2.9 million deaths worldwide were attributable to diabetes (Roglic et al 2005; WHO 2006). It is also estimated that 60% of all cases of diabetes can be directly attributed to obesity (Yach et al 2006). With a global rise in the incidence of obesity, the societal and economic impact of diabetes will only increase without effective intervention (Centers for Disease Control and Prevention 2005; Yach et al 2006).

Glycosylated hemoglobin (Hb_{A1c}) is the most commonly used surrogate measure of average BG concentration over the life of the red blood cell (approximately 3 months). Subcutaneous administration of insulin is currently the primary mechanism for regulating Hb_{A1c} levels in patients who are severely insulin deficient (type 1 diabetes mellitus, T1DM) and in patients with insulin resistance and/or an insufficient insulin supply in whom lifestyle changes and/or oral anti-diabetic medications (OAMs) fail to elicit adequate metabolic response (type 2 diabetes mellitus, T2DM).

Initial insulin management of T2DM typically involves initiation of a single injection of long acting insulin (American Diabetes Association 2007). Although this treatment

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may allow nearly 60% of subjects to achieve target BG control with an Hb_{A1c} value below 7% (Riddle et al 2003, 2006), this level of control is difficult to achieve in broad clinical practice using basal-only therapy, and additional strategies to intensify therapy may be needed.

Intensification of diabetes management often involves multiple (3 or more) daily injections of insulin and frequent BG monitoring (Diabetes Control and Complications Trial Research Group 1993; Schaumberg et al 2005). Although intensive management can prove effective in controlling Hb_{A1c} levels and reducing the risk of diabetes complications (Diabetes Control and Complications Trial Research Group 1993), many patients with diabetes are reluctant to initiate or adhere to insulin therapy due to anxiety over multiple injections, inconvenience and social stigma (Hauber et al 2005; White 2006).

The last 20 years has seen a revolution in research and development of alternative, injection-free insulin delivery methods. One of the most promising of these noninvasive candidates is inhaled insulin. In this article, we review the importance of insulin-mediated glycemic control in the prevention of diabetes-related cardiovascular disease, the development and current status of inhaled insulin as a novel drug delivery system, and the future potential of inhaled insulin as an effective therapy for reducing cardiovascular morbidity and mortality resulting from uncontrolled BG.

Overview of diabetes and cardiovascular disease

There is a strikingly high incidence of cardiovascular-related morbidity and mortality in individuals with diabetes; approximately 50% of all diabetes-related deaths are attributed to coronary artery disease (Jelesoff et al 1996). This finding is not surprising, considering the multiple mechanisms by which insulin and circulating glucose regulate normal cardiovascular function. Indeed, systemic changes related to chronic hyperglycemia directly contribute to the development of hypertension, atherosclerosis, thrombotic events, and cardiomyopathy (King and Wakasaki 1999; Stenina 2005b; Watala 2005; Yamagishi and Imaizumi 2005; Ahmed and Goldstein 2006; Raman et al 2007).

Although much progress has been made in recent years, the mechanistic relationship between insulin resistance, hyperglycemia and the broad spectrum of diabetic complications remains an area of active research. Aspects of this field of study have been reviewed by many investigators (King and Wakasaki 1999; Saltiel and Kahn 2001; Brownlee

2005; Stenina 2005a) and will not be comprehensively reviewed here.

Diabetes can arise from a number of initiating conditions that collectively lead to common downstream outcomes (Figure 1). At the cellular level, a variety of cell types develop altered sensitivity to insulin through little known mechanisms (Saltiel and Kahn 2001; Brownlee 2005; Yamagishi and Imaizumi 2005). Specifically, insulin docking with the insulin receptor on the target cell surface normally activates multiple cascades of intracellular signaling. In insulin resistance, one key pathway that includes the signaling kinases phosphatidylinositol-3-kinase and AKT fails to activate, disrupting normal intracellular insulin responsiveness and preventing key proteins involved in glucose uptake from being upregulated by insulin. As a result, cellular uptake of glucose is attenuated, circulating BG remains high, and tissues such as the endothelial lining of blood vessels passively accumulate glucose.

This rise in intracellular glucose increases glycolysis through the hexosamine metabolic pathway, damages cellular proteins and mitochondria through the accumulation of advanced glycation end products, and creates intracellular oxidative stress. The net effect of these changes is altered gene transcription and protein production, leading to a progressive impairment of normal cell function (Saltiel and Kahn 2001; Brownlee 2005; Yamagishi and Imaizumi 2005).

These progressive changes in normal cell and tissue function can lead to a spectrum of complications in patients with diabetes, including altered metabolism involving a shift from mixed glucose and fat use for energy production to the use of solely one or the other, altered vascular tone and responsiveness leading to hypertension, and altered production and/or secretion of proteins involved in vasorelaxation, inflammation, and coagulation (Figure 1). As a result, patients with diabetes can develop vascular disorders that may result in blindness, kidney disease and renal failure, loss of limbs from poor peripheral circulation, and blood vessel-occluding plaques and blood clots, leading to heart attacks and stroke (American Diabetes Association 2007).

Support for both elevated BG and endothelial cell oxidative stress as contributors to these processes is mounting. Recent evidence that these factors are both interrelated and co-contributors to diabetes disease processes comes from reports that intensive glycemic control reduces circulating levels of markers of inflammation (Schaumberg et al 2005) and normalizes endothelial function in patients with T1DM through the simultaneous control of hyperglycemia and oxidative stress (Ceriello et al 2007). Improved integrative

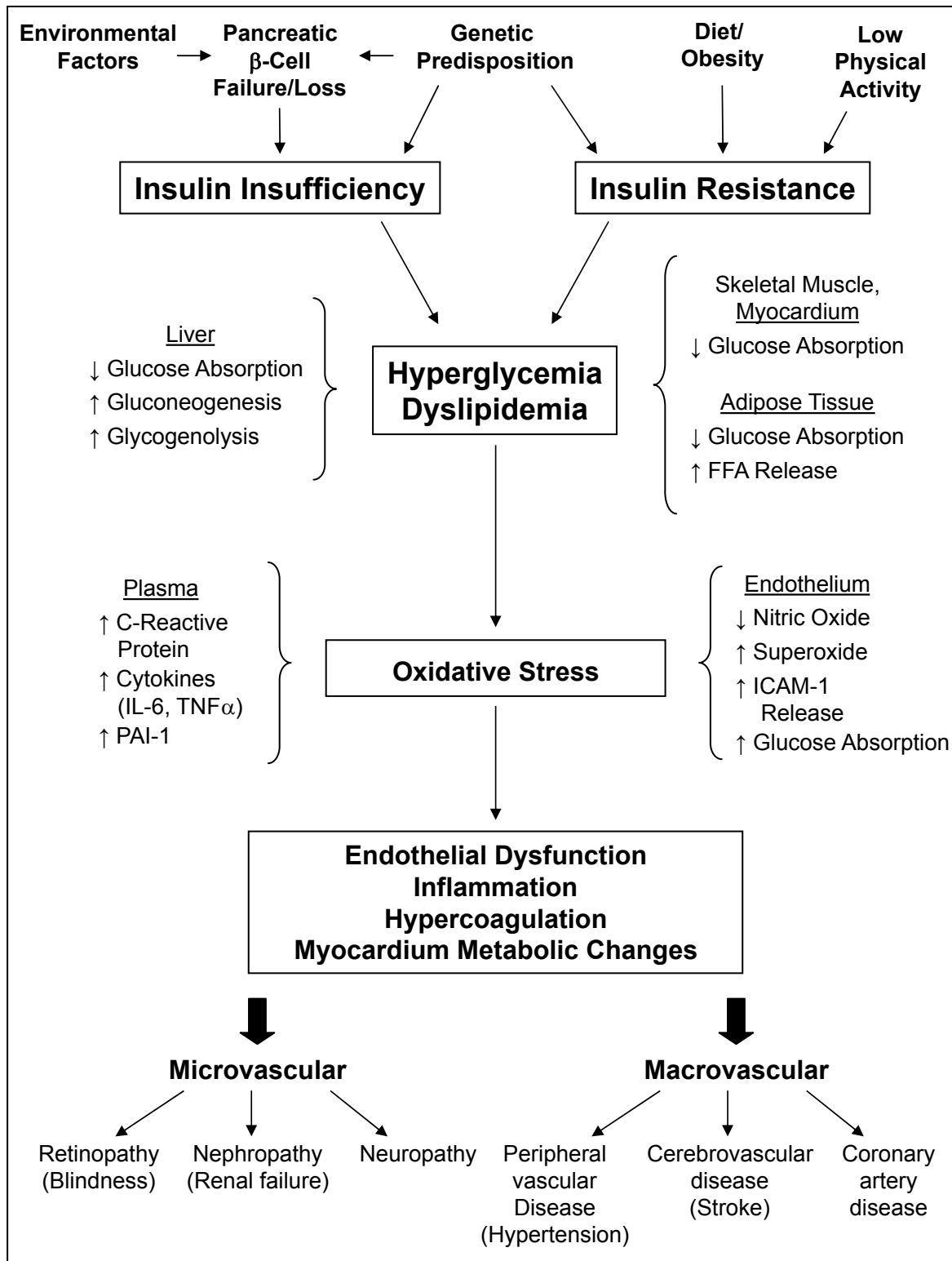


Figure 1 Summary of diabetes causes and progression. Diabetes represents a collection of disease processes involving progressive systemic loss of tissue sensitivity to insulin signaling and/or the loss of pancreatic β -cell number or function. Changes at the level of intracellular signaling include decreased expression of glucose transport proteins (GLUT4), decreased production of endothelial vasodilators (nitric oxide), increased intracellular oxidative stress (O_2), and release into the systemic circulation of pro-inflammatory (C-reactive protein, IL-6, TNF α) and coagulation (PAI-1, ICAM-1) mediators. These changes are both caused by and lead to decreased glucose absorption in several organs, increased levels of both circulating glucose (hyperglycemia) and non-esterified fatty acids (dyslipidemia), passive glucose diffusion into cells with unregulated glucose uptake, changes in vascular endothelial tone, and formation of atherosclerotic plaques. Glycosylation of intracellular and systemically circulating proteins, increased luminal fatty acid deposition, altered cellular metabolism, and increased clotting contribute to an increased risk for the microvascular and macrovascular risks associated with uncontrolled diabetes.

approaches to diabetes therapy may come from these lines of investigation, but presently, achieving normal BG regulation remains a primary therapeutic goal in diabetes.

Importance of controlling Hb_{A1c}, fasting blood glucose and postprandial blood glucose

The central element in the development and progression of diabetes is the progressive loss of insulin production and/or insulin sensitivity, leading to dysregulation of systemic glucose utilization and increased BG concentrations. This rise in BG results in an increase in the covalent addition of glucose and its degradation products to both intracellular and circulating proteins (such as hemoglobin), which can contribute to altered vascular tone and atherosclerosis. Large clinical trials have demonstrated a direct correlation between Hb_{A1c} concentration and cardiovascular disease and mortality (Khaw et al 2004). Fasting BG concentration and postprandial BG (PPBG) concentration are also used as indicators of effective short term BG regulation. Whereas fasting BG has long been used as a rapid indicator of insulin sufficiency, PPBG is thought to provide separate evidence of a person's ability to adequately respond to a food challenge. Inadequate PPBG regulation occurs quite frequently in patients with T2DM, can occur even when metabolic control appears to be good, and may represent a separate risk factor for diabetic complications (Bonora et al 2006).

The role of therapeutic interventions that specifically target PPBG control is a matter of considerable debate (Cefalu 2007; Nathan 2007). There is general agreement, however, that any intervention that fails to achieve target Hb_{A1c} goals should be intensified, and, as discussed above, this will frequently require the addition of meal time insulin to a basal-only insulin regimen. Several studies have indicated that premixed insulin products (ie, products that contain both rapid-acting and basal insulin components) may allow patients to achieve superior Hb_{A1c} control compared to basal-only regimens (Malone et al 2004, 2005, Raskin et al 2005). Regardless of the type of therapy used, successful management of BG concentrations has been shown to decrease the risk of both the microvascular and macrovascular complications of T1DM and T2DM (UK Prospective Diabetes Group 1991; Diabetes Control and Complications Trial Research Group 1993; Writing Team for the Diabetes Control and Complications Trial 2003; Nathan et al 2005).

For patients with pancreatic β -cell failure and insulin insufficiency, insulin therapy is critical for BG regulation and for patient survival. With T2DM, however, the need for insulin

supplementation usually develops later in the disease process. There are a number of therapies other than insulin, including oral anti-hyperglycemic medications (OAMs), which are available for initial BG control in this population. These medications include older agents such as the sulfonylureas and metformin, used alone or in combination with cholesterol-lowering statins, and the insulin-sensitizing thiazolidinediones. One newer class of drugs consists of incretin mimetics (glucagon-like peptide 1 agonists or analogues) and incretin enhancers (dipeptidyl peptidase-4 [DPP-4] inhibitors). Incretins are gastric hormones that control postprandial hyperglycemia by slowing gastric emptying, enhancing glucose-mediated insulin release, and controlling elevated postprandial glucagon (Blonde et al 2006; Drucker and Nauck 2006). Drugs in this class that have received recent United States Food and Drug Administration and European Union approval include the incretin mimetic Byetta® (exenatide, Amylin Pharmaceuticals, San Diego, CA and Eli Lilly and Company, Indianapolis, IN) and the DPP-4 inhibitor Januvia™ (sitagliptin phosphate, Merck and Co., Whitehouse Station, NJ). This newer drug class shows consistent if moderate reductions in Hb_{A1c} levels in controlled clinical trials (Heine et al 2005; Herman et al 2005). Weight loss has also been reported with the use of Byetta (Buse et al 2007).

Despite the availability of a growing number of treatment options for glycemic control in patients with T2DM, most patients taking OAMs do not achieve the recommended target of Hb_{A1c} below 7% (The ACE/ADA Task Force on Inpatient Diabetes 2006), let alone the more aggressive goals supported by other advisory bodies (Diabetes Medical Guidelines Task Force 2002). This group of patients may require insulin treatment to supplement or replace OAMs; however, significant reluctance to initiating insulin therapy has been documented in both patients with T2DM and their clinicians. The reasons for this reluctance include the fear of needles with anticipated pain of daily injections, the inconvenience of injection and monitoring regimens, fear of hypoglycemia, perceptions of failure in disease progression, and concern about weight gain (Zambanini et al 1999; Korytkowski 2002; Richardson and Kerr 2003; Peyrot et al 2005; Peyrot et al 2006). Unfortunately, delays in initiating insulin therapy in patients with inadequate glycemic control can increase the risk of developing serious complications (Brown et al 2004).

Overview of inhaled insulin delivery devices

In the search for alternative routes for systemic delivery of insulin, several possibilities have been explored, including

nasal, buccal (oral cavity), and pulmonary routes. Of these options, the lung, with its highly vascularized and relatively permeable large alveolar surface area ($\sim 100 \text{ m}^2$), currently presents the best option for an alternative route for insulin delivery. The idea of administering insulin through the lungs was first proposed in 1924 and inhaled delivery of locally targeted pharmacological therapies is used routinely (Patton 2006). However, difficulties related to bioavailability, formulation and particle size, and the mechanics of deep lung protein delivery have, until recently, precluded routine insulin inhalation therapy. The impending worldwide epidemic rise in diabetes incidence has prompted a resurgence of interest in this area. Investigators have established several criteria for effective delivery of precise doses of proteins to the systemic circulation via the lung. These criteria include an optimal aerodynamic particle size, breath holding time, inspiratory flow rate, and adequate lung function (Heinemann 2002; Patton 2006). The ideal device should deliver a consistent insulin dose to the deep lung and be relatively easy and convenient to use. An insulin delivery system meeting these criteria will increase insulin acceptance by both patients and providers, thus facilitating earlier initiation of insulin therapy, better BG control, and better treatment outcomes.

There are a number of companies currently developing insulin inhalation systems and this rapidly developing field has been the subject of several recent reviews (Mastrandrea and Quattrin 2006; Muchmore and Gates 2006; Patton 2006; Rosenstock et al 2007a). The only inhaled insulin product that currently has marketing authorization is Exubera® (Pfizer/Nektar), but several others, including AERx® iDMS (Novo Nordisk), Technosphere® (MannKind) and AIR® Inhaled Insulin (Alkermes/Eli Lilly) are being studied in Phase 3 clinical trials. These devices use a variety of liquid and powder insulin preparations, unique delivery devices and unique technical methodologies (Table 1).

Although there is some variability between these different insulin inhalation devices in time to peak BG-lowering activity and duration of activity, they share the common feature of rapid onset of activity (10–20 minutes) and relatively short duration (Patton 2006). For most of these devices, the time to maximal insulin activity is similar to that of rapid-acting subcutaneous insulin lispro, making them suitable for preprandial insulin dosing to control postprandial spikes in BG concentration. Recent reports on the clinical evaluation of the efficacy of inhaled versus subcutaneous insulins are summarized for patients with T1DM in Table 2 and for patients with T2DM in Table 3. Overall glycemic control was similar between inhaled insulin and subcutaneous

insulin delivery in most of these studies, with similar safety profiles (discussed below). Importantly, the availability of inhaled insulin may promote acceptance of insulin therapy in patients with diabetes, which in turn may improve initiation of and compliance with insulin treatment (Freemantle et al 2005, 2006).

Safety

Since diabetes is a chronic disease, one important concern in the development of inhaled insulin is whether it can be used safely over an extended period of time. The major areas of concern regarding the safety of long term use involve the incidence of low BG concentrations or hypoglycemia, increases in circulating anti-insulin antibodies, and changes in pulmonary function.

Hypoglycemia

In two recent clinical trials, hypoglycemia occurred less frequently but to a slightly higher degree of severity with inhaled insulin compared to subcutaneous insulin in patients with T1DM or T2DM (Hollander et al 2004; Quattrin et al 2004; Rosenstock et al 2007a). A meta-analysis of 16 open-label clinical trials of inhaled insulin in more than 4000 patients was recently reported (Ceglia et al 2006). Results of this analysis showed that severe hypoglycemia was more likely to occur in patients with T2DM using inhaled insulin versus those using OAMs alone (risk ratio [RR]: 3.1; confidence interval [CI]: 1.0–9.1), but that this risk was no greater when compared with patients using subcutaneous insulin.

A number of studies have shown that fasting BG is lower during inhaled insulin treatment as compared to meal time insulin injection regimens (Hollander et al 2004; Quattrin et al 2004; Garg et al 2006; Skyler et al 2007). Low fasting BG may increase the risk of nocturnal hypoglycemia, although only one publication to date specifically reports nocturnal hypoglycemia rates during inhaled insulin treatment (Garg et al 2006). In this report, the rates for any hypoglycemia and severe hypoglycemia in patients with T1DM were similar between inhaled insulin and injected insulin groups. However, better fasting BG levels that were achieved with inhaled insulin were associated with an increased rate of nocturnal hypoglycemia. This effect was observed only among patients who used a rapid acting insulin analog during the injection phase of this crossover study; patients who used regular human insulin during the injection phase did not have this propensity (Garg et al 2006). This observation suggests that behavioral guidance regarding insulin dosing, meals and snacks, and activity levels may be

Table 1 Current insulin inhalation systems

Phase	Name	Developer (partner)	Delivery system
Marketed*	Exubera®	Nektar Therapeutics (Pfizer Inc.)	Dry-powder, single-dose blister packs (1–3 mg); breath actuated inhaler
Phase III	AIR®	Alkermes (Eli Lilly)	Dry-powder phospholipid matrix; small mechanical and breath-actuated inhaler
	AERx® iDMS	Aradigm (Novo Nordisk)	Liquid aerosol; patient guided by microprocessor feedback inhaler system
	Technosphere®	MannKind	Dry-powder, encapsulated in microspheres with diketopiperazine derivative; breath-actuated inhaler
Phase II	Inhaled Insulin	Abbott Laboratories/KOS Pharmaceutical	Crystalline, breath-actuated propellant inhaler
Phase I	Microdose Dry Powder Inhaler	Qdose Ltd. (Microdose Technology)	Dry-powder; breath actuated, electronically controlled inhaler
	ProMaxx Microspheres	Baxter Biopharma	Dry-powder microsphere; propellant metered-dose inhaler and two types of dry-powder inhalers: Cyclohaler and Disphaler
	Alveair™	CoreMed	Liquid aerosol polymer/bio-adhesive formulation
	BioAir	BioSante Pharmaceuticals	Coated dry particles

*Marketing authorization in Europe and the USA (2006).

able to lower the risk of hypoglycemia. Studies using the AIR Insulin System to assess the efficacy of such behavioral modifications are underway.

Anti-insulin antibodies

Administration of exogenous insulin has been associated with an increased production of anti-insulin antibodies. These increases are common, especially in patients with T1DM. At similarly efficacious doses, inhaled insulin appears to trigger an enhanced production of anti-insulin antibodies compared with subcutaneous insulin. However, increased antibody levels have not been correlated with adverse events, or with relevant clinical correlates of Hb_{A1c} levels, insulin dose, hypoglycemia, or changes in pulmonary function (Cefalu et al 2005; Heise et al 2005; Fineberg et al 2005; Skyler et al 2005, 2007). The possible significance of increases in anti-insulin antibodies continues to be assessed in long term safety studies.

Pulmonary function

The potential impact of chronic deep-lung deposition of exogenous proteins on pulmonary function presents another potential safety concern. Cough is a common but transient side effect of initiating inhaled insulin therapy. Coughing episodes were generally described as mild and non-progressive and occurred at a similar frequency (~25%) to those observed in

patients undergoing other forms of inhalation therapy (Owens et al 2006). In the same meta-analysis described above, an increased risk of mild-to-moderate, non-progressive cough was identified in patients on inhaled insulin (Ceglia et al 2006).

However, in short term observational studies, no change or only small changes were observed between inhaled insulin and other treatment groups in pulmonary function tests (PFTs) (Table 2, Table 3) (Weiss et al 2003; Hermansen et al 2004; Rosenstock et al 2005; Cefalu et al 2006). When patients using inhaled insulin were followed for up to 2 years, changes in lung function from baseline were small when measured by forced expiratory volume in 1 second (FEV₁, <1%) and carbon monoxide diffusing capacity (DL_{CO}, <2%), the two most widely accepted indices of pulmonary function (Skyler et al 2007). These changes occurred within the first 3 months of initiating treatment and were not progressive. Current recommendations for the only marketed inhaled insulin dictate that all patients initiating inhaled insulin therapy undergo baseline PFTs that include spirometry and assessment of FEV₁ values. Inhaled insulin should not be used in patients whose FEV₁ is below 70% of predicted values. It is also recommended that patients should be reassessed after 6 months and yearly thereafter, and that use of inhaled insulin should be discontinued if

Table 2 Summary of published efficacy and/or safety studies in patients with type 1 diabetes (T1DM)

Clinical development stage	Study description			Glycemic control	Safety
	Duration	Evaluable subjects (n)	INH vs comparator	Hb _{A1c} (%)	FEV ₁ (L) ^a
Phase III (Skyler et al 2007)	24 months	n = 580	Exubera® vs SC insulin	[4.0 vs 3.8]	−0.051 vs −0.034 ^{ab} [−0.437 vs −0.287]
(Skyler et al 2005)	6 months	n = 328	Exubera® + NPH vs REG + NPH	−0.3 vs −0.1 [9.3 vs 9.9*]	−0.016 vs 0.008 [−0.750 vs −0.229*]
(Dumas et al 2005)	24 weeks	n = 226	Exubera® vs SC mixed	−0.4 vs −0.5 [6.8 vs 5.5*]	−0.070 vs −0.027 [−0.973 vs −0.246]
(Fineberg et al 2005)	2-year extension (pooled trials)	n = 1353	Exubera® vs SC insulin	No correlation between antibodies and glycemic control	No correlation between antibodies and lung function
(Quattrin et al 2004)	6 months	n = 334	Exubera® vs SC insulin	−0.2 vs −0.4 [8.6 vs 9.0*]	−0.065 vs 0.002 [−1.685 vs −0.031*]
(Rosenstock et al 2004)	1 year (extension)	n = 102	Exubera® vs SC insulin (in both T1DM and T2DM)	−0.78 vs −1.06 [2.52 (INH)]	−0.03 vs 0.02 [−1.05 vs −2.53]
(Skyler J for the Exubera Phase 2 Study Group 2004)	4 years (extension)	n = 112	Exubera® 4th year vs Exubera® baseline	−0.48 (INH) [1.5 vs 2.58]	−0.057 (non-INH, −0.071) [−0.376 (non-INH, −0.673)]
(Barnett AH for the Exubera Phase III Study Group 2004)	12 months (extension)	n = 627	Exubera® + OA vs OA(s)	−2.0 vs −1.8 [NS]	NS [NS]
Phase II (Garg et al 2006)	12 weeks	n = 259	AIR® vs SC insulin + insulin glargine	−0.2 vs −0.1 [7.9 vs 7.7]	NA [−1.6 vs −0.6 [†]]
(Heise et al 2005)	24 weeks	n = 47	Exubera® vs SC insulin	No correlation between antibodies and glycemic control	NA
(Skyler et al 2001)	12 weeks	n = 72	Exubera® vs SC insulin	−0.6 vs −0.8 [33 vs 31]	−2.17 vs −1.02 [−5.78 vs −7.71]

^aReported treatment differences in values for Hb_{A1c} [overall hypoglycemia (events/subject months)] and for FEV₁ [changes (in liters) from baseline in DL_{co} (ml/min/mmHg)].

^bThe significant difference between treatment groups in FEV₁, developed during the first 3 months and was nonprogressive thereafter.

*p < 0.05 [also for data expressed as 95% confidence interval (CI)].

†p < 0.001.

Abbreviations: Hb_{A1c}, glycosylated hemoglobin; INH, inhaled insulin; NA, (data) not available; NPH, neutral protamine Hagedorn insulin; NS, not significant (reported as 'no difference', values not provided); OA, oral antidiabetic agents; REG, regular human insulin; ROS, rosiglitazone; UL, ultralente insulin.

PFT values decrease by more than 20% (Exubera package insert).

Attributes and efficacy of the AIR Insulin System

The AIR Insulin System is comprised of three elements: AIR Inhaled Insulin, the AIR Insulin Inhaler, and the Directions for Use circular. AIR Inhaled Insulin is composed of a combination of rDNA native human insulin and an excipient based on a normal component of alveolar surfactant. AIR Inhaled Insulin is packaged as a dry powder in capsules designed to deliver doses approximately equivalent

to either 2 U (0.9 mg capsule fill weight of insulin) or 6 U (2.6 mg capsule fill weight of insulin) of injected insulin. The two strengths provide dosing flexibility for individual patients. A higher dose formulation is currently undergoing clinical testing.

The AIR Insulin System incorporates unique features for pulmonary delivery of pharmaceutical products. The technology is based upon the inhalation of dry-powder aerosols composed of relatively large low-density particles. Individual particles contain both the active agent and an excipient dispersed throughout the particle. Even though the particles have a relatively large geometric size (median > 5 µm), their

Table 3 Summary of published efficacy and/or safety studies in patients with type 2 diabetes (T2DM)

Clinical development stage	Study description		Glycemic control	Safety	
	Duration	Evaluable subjects (n)	INH vs comparator	Hb _{A1c} (%) ^a [Overall hypoglycemia (events/subject months)]	FEV ₁ (L) ^a [DL _{co} (ml/min/mmHg) ^a]
Phase III					
(Barnett et al 2006a)	24 weeks	n = 414	Exubera + metformin vs glibenclamide + metformin	−2.12 vs −2.05 [0.18 vs 0.08]	−0.09 vs −0.04 [−0.43 vs −0.78]
(Barnett et al 2006b)	24 weeks	n = 423	Exubera + sulphonylurea vs metformin + sulphonylurea	−2.06 vs −1.83* [0.31 vs 0.17]	−0.07 vs −0.04 [−0.27 vs 0.05]
(Cefalu et al 2005)	2 years	n = 304	Exubera [®] + OA vs OA ^b	−1.8 vs −1.50 [0.120 vs 0.148]	−0.077 vs −0.67 [−0.703 vs −0.735]
(DeFronzo et al 2005)	3 months	n = 143	Exubera [®] vs rosiglitazone	−2.3 vs −1.4* [0.7 vs 0.05]	−0.016 vs −0.001 [−0.973 vs −0.829]
(Hollander et al 2004)	6 months	n = 298	Exubera [®] + UL vs REG + NPH	−0.7 vs −0.6 [1.4 vs 1.6*]	−0.05 vs −0.91 [−0.79 vs −0.71]
(Rosenstock et al 2005)	3 months	n = 309	Exubera [®] vs Exubera [®] + OA vs OA	−1.4 [†] vs −1.9 [†] vs −0.2 [1.7 vs 1.3 vs 0.1]	−0.002 and −0.028 ^d [−0.388 and −0.303]
(Skyler J for the Exubera Phase 2 Study Group 2004)	4 years (extension)	n = 112 ^c	Exubera [®] 4th year vs Exubera [®] baseline	−0.48 [1.5 vs 2.58]	−0.057 (non-INH, −0.071) [−0.376 (non- INH, −0.673)]
Phase II					
(Rosenstock et al 2006)	4 weeks	n = 102	AIR Insulin standard vs intensive training	PPBG −0.11 vs 0.23	−0.12 vs −0.08 [−1.01 vs −1.83]
(Rosenstock J et al 2005)	12 weeks	n = 119	Technosphere vs placebo	−0.76 vs −0.32 [‡] [NS (no events)]	ND [NS]
(Cefalu et al 2005)	3 months	n = 26	Exubera [®] + UL vs baseline injection regimen of 2–3 injections/day	−0.71* (INH) [0.83]	NA [NA]
(Hermansen et al 2004)	12 weeks	n = 107	AERx [®] iDMS vs SC insulin	−0.69 vs −0.77 [1.05 vs 1.52]	−3.2 vs −3.5 [−2.0 vs −1.1]
(Weiss et al 2003)	12 weeks	n = 107	AERx [®] iDMS + NPH (HS) vs SC Actrapid + NPH(HS) insulin	−2.3 vs −0.1 [‡] [0.64 vs 0.06 [‡]]	−0.09 vs −0.03 [−1.10 vs −1.26]

^aReported values are changes from baseline except where italicized (treatment difference).

^bOnly the two controlled studies are reported here.

^cData derived from pooled T1DM and T2DM patients.

^dMean treatment differences: Exubera vs OA and Exubera + OA vs OA, respectively.

*p < 0.05 [also for data expressed as 95% confidence interval (CI)].

[†]p < 0.001.

[‡]p < 0.0001.

Abbreviations: Hb_{A1c}, glycosylated hemoglobin; HS, at bedtime; INH, inhaled insulin; NA, (data) not available; NPH, neutral protamine Hagedorn insulin; NS, not significant (reported as 'no difference', values not provided); OA, oral antidiabetic agents; REG, regular human insulin; UL, ultralente insulin.

low density (<0.4 g/mL) results in an effective aerodynamic particle with a diameter range affords access to the deep lung. Relative to standard inhalation aerosols, the larger and less dense AIR Insulin particles require less energy to disperse prior to delivery to the lungs. This relatively low agglomeration and high dispersability permit efficient delivery of both small and large drug doses to the deep lung in a single inhalation from a simple, breath-actuated inhaler (Edwards et al 1997,

1998). Once deposited in the lung, the particles provide rapid and reliable uptake of protein therapeutics into the systemic circulation.

The AIR Insulin Inhaler is a small, hand-held, dry powder device that is capsule-based and breath-actuated (Rosenstock et al 2007a). It is designed such that the appropriate aerosol dose is delivered to the patient using the energy derived from a single inhalation of modest intensity. The inhaler

is a passive device with moderate resistance to inspiratory flow, which invites patients to inhale at a moderate rate in order to optimize deep lung deposition. Delivery of a similar powder based on the AIR technology has been characterized *in vivo* by high and reproducible emitted doses (87%) and high lung deposition (51% of the total dose) independent of peak inspiratory flow rate across a broad range (12–86 L/min) (DeLong et al 2005).

The AIR Insulin System is currently undergoing Phase III clinical testing, including long-term (24-month) safety and efficacy studies in patients with T1DM or T2DM, and additional safety evaluations in patients with comorbid lung disease and diabetes. Other studies that compare the efficacy and safety of AIR Insulin to monotherapy with insulin glargine are also underway. These studies, along with information on Hb_{A1c} from early phase clinical trials with AIR insulin, are described in separate reviews (Muchmore and Gates 2006; Rosenstock et al 2007a).

Patient training, satisfaction and preference for inhaled insulin therapy

Some of the reported barriers to strict glycemic control in patients with diabetes include reluctance to initiate insulin therapy and poor patient adherence because of pain and fear of injection, inconvenience, and social stigma associated with injections. Satisfaction surveys assessing the flexibility and ease of use, pain, side effects, and social acceptance of inhaled insulin have been overwhelmingly favorable (Hollander et al 2004; Quattrin et al 2004; Hayes et al 2007a). In patients with either T1DM or T2DM who have previously used subcutaneous insulin for diabetes management, 80% preferred inhaled insulin over conventional subcutaneous insulin for their meal time insulin therapy (Rosenstock et al 2004). In a recent report of self-directed versus intensive patient training for use of the AIR Insulin Inhaler, it was found that patients can be self-directed without detrimental effects on metabolic (Rosenstock et al 2007b) or patient-reported (Hayes et al 2007b) outcomes, including measures of vitality, diabetes-associated symptoms, fear of hypoglycemia, and insulin-delivery system satisfaction. These data support the AIR Insulin Inhaler as a patient-friendly insulin delivery method that should appeal to both clinicians and patients. Importantly, this sufficiency of patient-directed training should allow precious diabetes education resources to be deployed in other important aspects of diabetes care beyond teaching the mechanics of inhaled insulin administration.

Contraindications to the use of inhaled insulin

There are several patient populations for whom the use of inhaled insulin is not recommended. Women who are pregnant should not use it, and its use has not been approved for children or adolescents. Current tobacco smokers or patients who have smoked in the preceding six months are also not candidates for inhaled insulin. Smoking has been shown to increase the rate and extent of inhaled insulin absorption (Himmelman et al 2003; Becker et al 2006; Pan et al 2007), while acute passive exposure to smoke decreases the rate and extent of absorption (FDA Endocrinologic and Metabolic Drugs Committee 2005). Smoking cessation, nicotine replacement therapy, and acute smoking re-exposure are also associated with clinically significant alterations in inhaled insulin pharmacokinetics and glucodynamics (Pan et al 2007). Thus smokers or former smokers at risk of recidivism should not use inhaled insulin.

Patients with compromised lung function, such as those with asthma or chronic obstructive pulmonary disease (COPD), are also not candidates for Exubera, the inhaled insulin that is currently marketed, due to unpredictable absorption rates and possible problems with simultaneous use of bronchodilators (Exubera package insert). AIR Inhaled Insulin was recently reported to be well tolerated by patients with COPD, and to elicit time-exposure and time-action profiles similar to subcutaneous insulin lispro (Rave et al 2007). However, there was reduced insulin absorption and decreased metabolic effects when this population was compared with healthy subjects. Clinical evaluations of the use of inhaled insulins in these populations are ongoing (Rosenstock et al 2007a).

Summary and conclusions

Diabetes is a significant worldwide health problem. Insulin resistance and deregulated BG control are established risk factors for microvascular complications and cardiovascular disease, with risk reduced by adequate BG control and intensive diabetes therapy. Despite the availability of a variety of medications for BG regulation, most patients do not achieve optimal BG control. Inhaled insulin is a new, safe means to deliver insulin that may increase patient compliance with insulin therapy, helping them to achieve optimal glycemic control and possibly reducing their risk of developing cardiovascular complications. However, diabetes is a chronic illness requiring lifetime intervention. Thus, long term studies are still required in order to ensure the continued efficacy and safety of this new treatment for diabetes.

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