

Combined Photothermal Therapy and Chemotherapy of Oral Squamous Cell Carcinoma Guided by Multifunctional Nanomaterials Enhanced Photoacoustic Tomography

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Background: Squamous cell carcinoma of the head and neck is the sixth most common cancer worldwide, with 40% occurring in the oral cavity. Although the level of early diagnosis and treatment of OSCC has improved significantly, the five-year survival rate of advanced patients remains unsatisfactory. However, the main challenges before us are how to get an early and accurate diagnosis and how to formulate effective treatment. Nanoparticle-based chemo-photothermal therapy has proven to be a promising non-invasive approach to treating oral squamous cell carcinoma treatment.

Methods: In this study, we tried to design and synthesize multifunctional hyaluronic acid (HA) modified gold nanorods/mesoporous silica-based nanoparticles loaded with doxorubicin hydrochloride (DOX) for photoacoustic imaging (PAI) guided cooperative chemo-photothermal therapy.

Results: The resultant nanocomposite shows favorable biocompatibility, relatively low cytotoxicity, ideal drug loading capability and strong PAI signals. In addition, they showed an excellent photothermal conversion efficiency of 49.02% for photothermal therapy (PTT). Moreover, in vivo and in vitro experiments have shown that synergistic chemo-photothermal therapy has better therapeutic effects than chemotherapy alone or PTT ($P < 0.05$). After being injected into the CAL-27 tumor-bearing mice, the DOX-AuNRs@mSiO₂-HA nanoparticles could accumulate rapidly at the tumor sites and achieve complete ablation of tumors when combined with near-infrared laser irradiation, without obvious side effects on normal tissues.

Conclusion: Our research provides a solid demonstration of the potential of DOX-AuNRs@mSiO₂-HA as a multifunctional platform in PAI-guided photothermal chemotherapy for oral squamous cell carcinoma.

Keywords: mesoporous silica coated gold nanorods, photoacoustic imaging, chemo-photothermal therapy, oral squamous cell carcinoma

Introduction

Up to now, cancer continues to be the world's malignant disease and the leading cause of death.¹⁻³ Head and neck cancer is the sixth largest malignant tumor worldwide, of which 40% occur in the oral cavity and nearly 90% of which is classified as oral squamous cell carcinoma (OSCC).⁴ For early stage cancers, radiotherapy and surgery can effectively play a role. Whereas advanced cancers typically require combinations of surgery, chemotherapy and radiotherapy.⁵ OSCC

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is preventable and curable at an early stage, but the majority of cases can only be diagnosed at an advanced stage. Moreover, advanced therapy is difficult to achieve rational effect and its prognosis is terrible.^{6,7} The 5-year survival rate of advanced OSCC patients is still unsatisfactory, which is mainly related to the early diagnosis difficulty, easy recurrence after treatment, large systemic adverse effects and so on,^{8–10} making OSCC one of the most challenging diseases and remain a global health concern regardless of several advances made in the field of OSCC diagnostics and therapeutics.¹¹

Currently, precision medicine and targeted therapy are increasingly popular with anticancer treatments.¹² With the rapid development of modern imaging technology, photoacoustic imaging (PAI) is an emerging non-ionizing and non-invasive diagnostic technique, which enables tissue visualization with high resolution and in-depth resolution.^{13–15} Relatively recently, the use of PAI in the field of the oral cavity has been widely reported. In the diagnosis and assessment of the curative effect of OSCC, PAI plays an important role, especially in the localization of tumor areas and the detection of metastatic lymph nodes.^{16–18} Another conspicuous characteristic of PAI is that it offers the possibility of combining diagnosis to treatments, such as photothermal therapy (PTT).^{19–22} PTT is a therapeutic method that uses targeted recognition technology to gather materials with excellent photothermal conversion efficiency near tumor tissue, and converts light energy into heat energy to kill cancer cells under the irradiation of near-infrared light.^{23–25} Consequently, as a promising substitute for effective cancer treatment, it has attracted considerable attention. Owing to physiological complexity of serious diseases such as cancer, current developments have gently shifted from a focus on monotherapy to combine or multiple therapies since the synergy of therapeutic agents or techniques give rise to ostentatious super additive (namely “1 + 1 > 2”) therapeutic effects.²⁶

Cancer nanomedicine is considered to be a relatively new interdisciplinary field of research, involving chemistry, engineering, drug delivery and medicine, aimed at promoting greater development of cancer diagnosis and treatment.^{27–30} Gold nanoparticles (Au nanoparticles) are commonly used nanoparticles, which have been widely employed in PAI, PTT and targeted drug delivery because of its simple synthesis method, high yield, stable chemical properties, and adjustable surface plasmon resonance.^{31–36} Nevertheless, the low loading capacity of anticancer drugs prevented Au nanoparticles being used for clinical

purposes. Mesoporous silica nanoparticles, as a drug delivery system of high specific surface area, large pore volume, easy surface modification, good biocompatibility and convenient drug loading, have been widely used to coat gold nanorods in order to improve the long-term stability, hydrophilicity and drug delivery ability.^{37–40} Even more importantly, the mesoporous silica coating is a good way to overcome the toxicity of metal nanoparticles, because the silica shell has biochemical stability and corrosion resistance under extreme conditions.^{41–43}

In cancer treatment, targeted anticancer drugs can be more effective than conventional chemotherapy.⁴⁴ Hyaluronic acid (HA) is a natural, biodegradable and non-immunogenic polymer with high affinity for CD44 receptor, which has been proven to be involved in various of tumor biological activities including tumor proliferation, progression and metastasis.^{45,46} The HA shell wraps the drug to play a protective role, enhances the stability of the drug, and achieves sustained release of the drug.^{47,48} Herein, mesoporous silica-coated gold nanoparticles with a large volume of pores have been successfully obtained, which can be used for the chemophotothermal synergistic therapy of tumor. Excellent photothermal conversion efficiency and high-resolution photoacoustic (PA) signal were obtained simultaneously by the synthesized gold nanomaterials system. Meanwhile, doxorubicin hydrochloride (DOX), an effective anti-tumor chemotherapy drug, was loaded into the mesoporous silica of AuNRs@mSiO₂ through electrostatic interaction, namely van der Waals forces.^{49–51} HA molecules were coupled to AuNRs@mSiO₂ nanoparticles via amide bonds. To sum up, our DOX- AuNRs@mSiO₂-HA nanoparticles have shown excellent prospects as an effective platform for tumor targeting and PAI-guided chemo-photothermal synergistic therapy for oral cancer.

Experimental Details

Materials

Sodium borohydride (NaBH₄), HAuCl₄ Chlorauric acid trihydrate (HAuCl₄·3H₂O), Cetyltrimethylammonium bromide (CTAB), silver nitrate (AgNO₃), ascorbic acid, tetraethyl orthosilicate (TEOS) and 3-Aminopropyltriethoxysilane (APTES) were purchased from Shanghai Sigma-Aldrich. DOX and HA were obtained from Ruixi Biological Technology Co., Ltd. Cell Counting Kit-8 (CCK-8) was purchased from Dojindo Laboratories (Japan). A LIVE/DEAD Viability/Cytotoxicity Kit was obtained from the Shanghai Bestbio Biotechnology Co. Ltd. DAPI was purchased from

Shanghai Beyotime Biotechnology Co. Ltd. The human tongue squamous cell carcinoma CAL-27 cell line and the human oral keratinocytes HOK cell line were obtained from the American Type Culture Collection (ATCC). Deionised water (Millipore Milli-Q grade) with resistivity of 18.2 MΩ was used in all the experiments.

Synthesis of AuNRs Nanoparticles

Depending on the published program, AuNRs were synthesized and some minor modifications were made.⁵² Firstly, CTAB-capped Au seeds were established by chemical reduction of HAuCl₄ with NaBH₄. 7.5 mL 0.1 M CTAB was mixed with 250 μL 0.01 M HAuCl₄ and the volume was fixed on 9.4 mL by adding water. Next, 0.6 mL of ice-cold NaBH₄ aqueous solution (0.01 M) was added to the above mentioned mixed solution to form nano-gold seeds, which were stirred for 2 min and placed at 30°C for 2 h. The seeds were immediately formed and used within 2~5 h. The growth solution for owners consists of 200 mL of 0.1 M CTAB, 10 mL of 0.01 M HAuCl₄, 0.8 mL of 10 mm AgNO₃, 4 mL of 0.5 M H₂SO₄ and 1.6 μL of 0.1 M ascorbic acid. After adding 500 μL of the above managed seeds, stirring for two minutes and then standing at 30°C overnight. Then, the nanoparticles were collected by centrifugation, and washed twice with deionized water at a speed of 8000 rpm for 20 min each time. Finally, the owners were dispersed in 250 mL of deionized water.

Synthesis of AuNRs@mSiO₂ Nanoparticles

Add a certain amount of CTAB (0.8 mm) to 250 mL AuNRs obtained above, and pH was up-regulated in 10 with the 0.1m NaOH solution, then stirred at 33°C for half an hour to mix well. Following this step, 750 μL of 20% TEOS reagent diluted with methanol was added to the owner's solution three times with an interval of half an hour. After the reaction for 24 h, the obtained owners were harvested by centrifugation (12,000 rpm, 30 min). Washing with water and ethanol twice, and finally dispersing in 20 mL of ethanol.

Synthesis of AuNRs@mSiO₂-NH₂ Nanoparticles

To prepare amino-modified nanoparticles (AuNRs@mSiO₂-NH₂), 50 μL of 3-aminopropyltriethoxysilane (APTES) was added to the above-mentioned

AuNRs@mSiO₂ ethanol solution at 60°C for 24 h. Subsequently, it was centrifuged and washed three times with ethanol. To remove the surfactant CTAB remaining in the pores, AuNRs@mSiO₂-NH₂ was dispersed in 20 mL of ammonium nitrate ethanol solution (8 mg mL⁻¹), refluxed overnight, and then centrifuged and washed twice.

Synthesis of DOX-AuNRs@mSiO₂ Nanoparticles

The amount of DOX loaded into the AuNRs@mSiO₂-NH₂ nanoparticles was determined by UV-Vis spectrophotometer. DOX (20 mL, 1 mg mL⁻¹) was mixed with AuNRs@mSiO₂-NH₂ nanoparticles (16 mL, 2.5mg mL⁻¹), and stirred at 30°C for 24 h. After centrifugation, DOX-loaded AuNRs@mSiO₂-NH₂ nanoparticles were obtained and washed with deionized water three times to remove the DOX adsorbed on the surface. The free DOX in the supernatant was determined by UV-Vis spectrophotometer at 480 nm. The DOX-loading efficiency (LE) was calculated by Eq.1:

$$LE(\%) = \frac{W_{initialDOX} - W_{remanentDOX}}{W_{AuNRs@mSiO_2-NH_2}} \times 100\%(mg.mg^{-1})$$

Synthesis of DOX-AuNRs@mSiO₂-HA Nanoparticles

At first, 20 mg of HA was dispersed in 15 mL of deionized water and hydrated for 24 h, and then 8 mg of EDC and 5 mg of the NHS was mixed and stirred for 4 h to activate the carboxyl group of HA. Finally, DOX-AuNRs@mSiO₂ was added to the HA solution, stirred for 24 h, and the final product could be obtained after centrifugal washing.

Characterization

The morphology and size of the prepared nanoparticles were characterized by transmission electron microscopy (TEM) (JEM 1400, JEOM, Japan). According to the instructions in the manufacturer's operating manual, use the zeta potential analyzer (Malvern, UK) to detect the zeta potential distribution. The absorption spectra of free Dox, AuNRs, AuNRs@mSiO₂-NH₂, DOX-AuNRs@mSiO₂, DOX-AuNRs@mSiO₂-HA was acquired using a visible spectrometer (UV-2600, Shimadzu, Japan). Laser-confocal scanning imaging was obtained using a Laser-confocal scanning imaging (Zeiss LSM780, Oberkochen, Germany). Photoacoustic (PA)

characterization was conducted with a homemade multi-spectral PA microscopy (MSPAM) system.

Drug Release Experiments

Three portions of the prepared DOX-AuNRs@mSiO₂-HA nanoparticles at equal amount were dispersed at pH = 5.0 PBS (1.0 mL) and transferred protracted semipermeable dialysis bags at 37°C. The amount of DOX released into the solution was determined by measuring the absorbance at 480 nm with a UV-Vis spectrophotometer at selected time intervals. In order to prove that the laser irradiation and hyaluronidase treatment can induce the drug release, other experiments were conducted under the same procedures. Immerse the sample in PBS with near infrared region (NIR) irradiation (808 nm, 2.0 W cm⁻²) for 5 min, or dissolved it on PBS containing hyaluronidase. The concentration of DOX in the supernatant was evaluated by UV-Vis spectrophotometer.

Photothermal Effect Experiments

The photothermal effect of AuNRs@mSiO₂-HA nanoparticles was studied by 808 nm laser. The 808 nm laser equipment with adjustable power output (0.5–2 W cm⁻²) was used as the light source, and AuNRs@mSiO₂-HA nanoparticles (0–200 µg mL⁻¹) with different concentrations were dispersed in an EP tube. Use a digital thermometer to monitor the real-time changes of temperature every 10 s. Meanwhile, AuNRs@mSiO₂-HA was irradiated under 808 nm laser for 600 s, and then naturally cooled for 600 s to evaluate the photo-stability. The entire process was repeated five times. In addition, the temperature variation of the AuNRs@mSiO₂-HA nanoparticles was recorded under 808 nm laser irradiation (2.0 W cm⁻²) until a steady temperature was reached. Photothermal conversion efficiency (η) was calculated by Roper's method.

In vitro PAI Experiments

The PA performance of the AuNRs@mSiO₂-HA nanoparticles was evaluated by our MSPAM system. In our MSPAM system (Figure S1), the energy source for exciting materials was a nanosecond pulse OPO laser with tunable wavelength (Continuum, USA), and an ultrasonic transducer with a center frequency of 25 MHz (Olympus, USA) was used to detect the generated acoustic signal. A piece of copper wire was soaked in an agar made solid model and further imaged by our MSPAM system. As shown in Figure S2, the deepest depth of the copper wire that could be imaged can reach 2.3 mm. This result verifies

the imaging depth of our MSPAM system. In addition, the full width at half maxima (FWHM) of the line-spread function (LSF) defining the lateral resolution of the PAI system is 37.6 µm (Figure S3). To test the linearity of the PA signal as a function of AuNRs@mSiO₂-HA nanoparticles, 0.2 mL of the AuNRs@mSiO₂-HA nanoparticles aqueous suspension with different Au concentrations (0, 0.2, 0.4, 0.8 and 1.0 mg mL⁻¹) were added to the agar-phantom container and evaluated by our MSPAM system.^{53,54} A complete PA image of the phantom was collected at 808 nm.

Cell Culture

The human tongue squamous cell carcinoma CAL-27 cell line was selected for in vitro and in vivo experiment in this study. The human oral keratinocytes cell line was chosen for in vitro experiment in this study. The HOK cells were cultured in DMEM medium supplemented with 10% fetal bovine serum (FBS) in the humidified incubator (37°C, 5% CO₂). The HOK cells were cultured in DMEM: F-12 medium supplemented with 10% fetal bovine serum (FBS) and 1% penicillin and streptomycin in the humidified incubator (37°C, 5% CO₂).

Cellular Uptake Experiments

To investigate the uptake ability of DOX-AuNRs@mSiO₂-HA nanoparticles, CAL-27 and HOK cells were seeded in the 12-well plate for 24 h, with 2×10^5 cells each well. Then, the culture medium was removed, and DOX-AuNRs@mSiO₂ nanoparticles, DOX-AuNRs@mSiO₂-HA nanoparticles were added into the well for 2, 4, 8, and 12 h. The fluorescence intensity of cells was measured by flow cytometry to investigate the correlation of uptake of nanoparticle concentration and incubation time. Similarly, the CAL-27 cells were seeded on 35-mm glass bottomed dish for 24 h. Then, DOX-AuNRs@mSiO₂-HA nanoparticles were added into the dishes and incubated for 2 h, 4 h and 8 h, respectively. After that, the cells were stained with DAPI. After 20 min incubation, cells were washed three times with PBS and then fixed with 4% paraformaldehyde for 30 min at room temperature. Finally, cells were viewed under the confocal microscope.

In vitro Cytotoxicity Evaluation Against HOK Cells and CAL-27 Cells

The cytotoxicity of empty AuNRs@mSiO₂-HA nanoparticles, free DOX and DOX-loaded AuNRs@mSiO₂-HA

nanoparticles were evaluated by Cell Counting Kit-8. HOK cells were seeded in a 96-well plate at a density of 3×10^4 per well and incubated in the atmosphere of 95% air and 5% CO₂ at 37°C with 10% fetal bovine serum and 1% penicillin and streptomycin for 24 h. Cal-27 cells were seeded in a 96-well plate at a density of 5×10^4 per well and incubated in the atmosphere of 95% air and 5% CO₂ at 37°C with 10% fetal bovine serum for 24 h. Then, various concentrations of empty AuNRs@mSiO₂-HA nanoparticles, free DOX and DOX-loaded AuNRs@mSiO₂-HA nanoparticles were added, respectively. In another plate, the suspensions of AuNRs@mSiO₂-HA nanoparticles and DOX-AuNRs@mSiO₂-HA nanoparticles with different concentrations were added into CAL-27 cells with 808-nm NIR laser irradiation for 5 min. One row of a 96-well plate was added culture medium only to be a blank control. Ten microliters of the CCK-8 reagent was added to each well and then incubated for 2 h and the OD value at 450 nm was read using the micro plate reader. Cell viability was calculated by the percentage of OD value of the study group over the control group.

Live/Dead Cell Viability Assay

CAL-27 cells were cultured in the 48-well plate for 24 h, DOX-AuNRs@mSiO₂-HA suspension was added into dishes co-incubated for another 6 h. Then CAL-27 cells were irradiated under 808 nm laser for 5 mins. Afterwards, cells were stained with casein acetomethoxyl (calcein-AM) and propidium iodide (PI) for 15 min. Fluorescence images of cells were captured by a fluorescence microscope. The $\lambda_{\text{ex}}/\lambda_{\text{em}}$ of calcein-AM and PI were 499/515 nm and 495/635 nm, respectively.

Animal and Tumor Model

Female BALB/c nude mice (4–6 weeks old) were purchased from Guangdong Medical Laboratory Animal Center Co., Ltd. All animal procedures were performed in accordance with the Guidelines for Institutional Animal Care and Use Committee and approved by the approval of the Animal Care and Usage Committee of Guangzhou Medical University (GY2019-009). A human OSCC xenograft tumor model of mice was established by injecting 0.1mL CAL-27 cells suspension (4×10^6) into the right flank of the female BALB/c nude mice.

The mice were used for subsequent experiments until the tumor size reached approximately 80 mm³, and the tumor volume was calculated according to the following equation: tumor volume (mm³) = $0.5 \times (\text{tumor length}) \times$

(tumor width).² The xenograft-bearing mice were randomly assigned into four groups: control group (injected with PBS), LASER group, DOX-AuNRs@mSiO₂-HA group (injection with 0.2 mL DOX-AuNRs@mSiO₂-HA, 1 mg mL⁻¹, based on gold ion), and DOX-AuNRs@mSiO₂-HA + LASER group (injection with 0.2 mL DOX-AuNRs@mSiO₂-HA, 1 mg mL⁻¹, based on gold ion). The nanoparticles and PBS were intravenously injected via tail vein.⁵⁵ Herein, PTT treatment groups were subjected to NIR laser irradiation (power density of laser, 2 W cm⁻²) for 5 min at 8 h post injection.

In vivo PAI Experiments

To evaluate the in vivo photoacoustic performance of the DOX-AuNRs@mSiO₂-HA for the CAL-27 subcutaneous tumor, the CAL-27 tumor-bearing nude mice were intravenously injected with the as-prepared nanoparticles (200 μ L, 1 mg mL⁻¹). For PAI, tumor-bearing mice with intravenously injected nanoparticles aqueous solution were anesthetized (with 1% sodium pentobarbital). PA images of the tumor site were obtained at different time intervals (0, 2, 4, 8, 12 and 24 h) and captured by our MSPAM system with 845 nm laser excitation.

Histological Examinations

For histological examination, the tissues and tumors of mice were harvested immediately after the mice were sacrificed. After that, 4% paraformaldehyde solution was used to fix for hematoxylin and eosin (H&E) staining. All of the sections were examined with an inverted light microscope.

Statistical Analysis

Data were analyzed with an analysis of variance (one-way ANOVA) using GraphPad Prism 9 software to evaluate the differences between test groups. Statistical significance was defined as $p < 0.05$. All data were presented as mean \pm standard deviation (SD). All figures presented in this article were obtained from five independent experiments with similar results.

Result and Discussion

Fabrication of DOX-AuNRs@mSiO₂-HA nanoparticles is elucidated in Figure 1. Firstly, we constructed AuNRs coated with mesoporous silica nanoparticles. Then, the anticancer drug DOX was loaded into the AuNRs@mSiO₂ nanoparticles via electrostatic interaction. Finally, the amine functioned AuNRs@mSiO₂ by the post

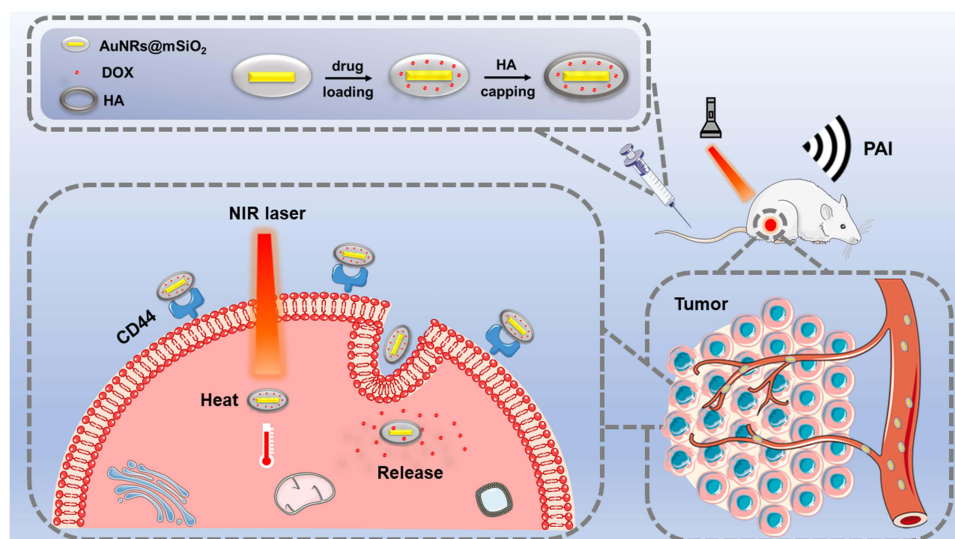


Figure 1 Schematic illustration of the preparation of HA-modified owners coated mesoporous silica nanoparticles as a carrier of DOX for photoacoustic imaging (PAI) and photothermal-chemo therapy of tumors.

grafting method was attached to HA through the EDC-mediated amidation reaction, forming DOX-AuNRs@mSiO₂-HA nanoparticles for photothermal and chemotherapy applications. Meanwhile, CD44 receptor-specific endocytosis of nanoparticles was also demonstrated in Figure 1. When DOX-AuNRs@mSiO₂-HA nanoparticles have been injected into a tumor model, the conjugated HA molecules could make DOX-AuNRs@mSiO₂-HA specifically deliver in cancer cells by the CD44-HA. Subsequently, HA shell was able to be degraded by hyaluronidase, which triggered the release of DOX. Under NIR irradiation, the PAI and photothermal-chemotherapy of DOX-AuNRs@mSiO₂-HA nanoparticles could be triggered, which led to a synergistic effect for killing cancer cells. In this study, we hypothesized that the drug loaded AuNRs@mSiO₂ would effectively reach the tumor site by the EPR effect and by the specific CD44 binding on tumor cells. Once bound to CD44, the nanoparticles would be internalized by receptor-mediated endocytosis, hopefully leading to rapid degradation of the nanoparticles by Hyal-1 and the burst release of the anticancer drug for enhanced therapeutic efficacy.

Synthesis and Characterization of DOX-AuNRs@mSiO₂-HA

The preparation of AuNRs was carried out by a seed-mediated growth method that has been considered as a simple and cost-effective method of preparation for

nanocomposite.⁵⁶ The morphology and size of as-prepared AuNRs was characterized by the TEM, which was displayed in Figure 2A. The TEM image showed that the as-prepared AuNRs was about rod shape and highly uniform size. The aspect ratio of high-quality AuNRs was 3.8 (average width, 18 ± 3 nm; length, 75 ± 8 nm). As shown in Figure S4A, the prepared owners have a weak transverse plasmon band at 510 nm and a strong longitudinal plasmon band at 750 nm. However, AuNRs required further modifications as drug-delivery platforms. Mesoporous silica nanoparticles have been widely accepted to coat AuNRs to achieve long-term stability, hydrophilicity, and drug delivery capacity.⁵⁷ As illustrated in Figure 2B, the TEM image of the prepared AuNRs@mSiO₂ core-shell nanoparticles showed that the owners were coated with mesoporous silica shells (16 nm thickness), offering an opportunity for AuNRs@mSiO₂ to be used as a general drug carrier. However, due to both the increase in the refractive index of the surrounding medium and the changes in nanoparticles geometric,^{58,59} the longitudinal surface plasmon resonance peak exhibited a small red-shift (40 nm) after silica coating (Figures S4B and 2E). After the addition of DOX and HA, the shell of DOX-AuNRs@mSiO₂-HA was slightly thicker than that AuNRs@mSiO₂ due to HA coating (Figure 2C). Once the DOX was absorbed on the surface of nanocomposite, the absorption spectrum of DOX-AuNRs@mSiO₂ had a small peak near 480 nm, locating at a similar place to that of free DOX (Figure 2D). In addition, as depicted

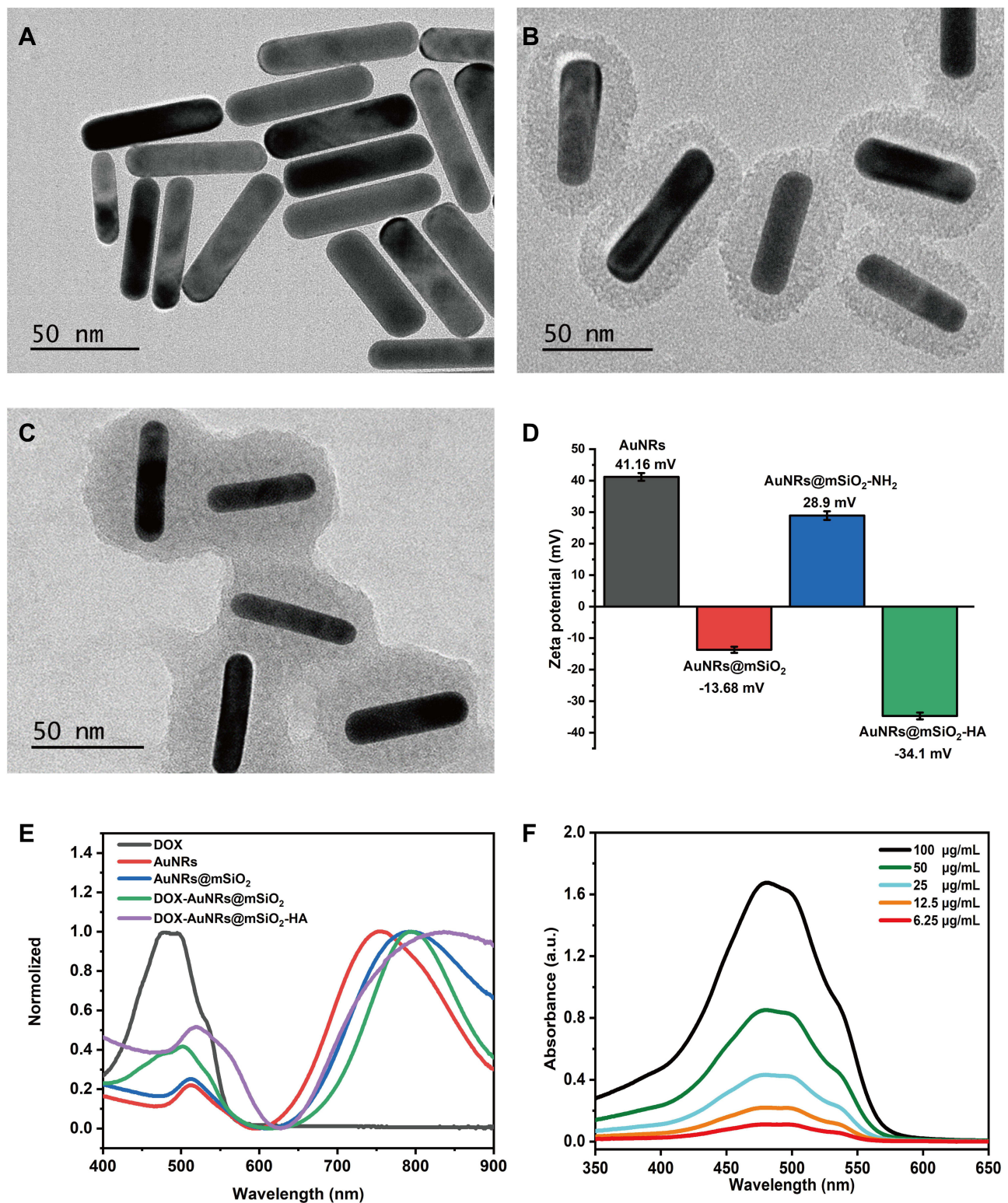


Figure 2 Characterizations of nanocomposites. (A) TEM image of GNRs. Inset scale bar = 50 nm. (B) TEM image of AuNRs@mSiO₂. Inset scale bar = 50 nm. (C) TEM images of DOX-AuNRs@mSiO₂-HA. Inset scale bar = 50 nm. (D) Zeta potential distributions of AuNRs, AuNRs@mSiO₂, AuNRs@mSiO₂-NH₂, and AuNRs@mSiO₂-HA. (E) Absorbance spectrum of DOX, AuNRs, AuNRs@mSiO₂, DOX-AuNRs@mSiO₂, and DOX-AuNRs@mSiO₂-HA. (F) Absorbance spectrum change of DOX.

in Figure 2E, a further red-shift accompanying slight damping of the band was observed upon DOX adsorption. All results demonstrated that DOX was successfully loaded on the surface of mSiO₂-capped AuNRs-based nanocarrier. The surface charge of the nanoparticles was monitored by a dynamic light scattering instrument (Figure 2F). The surface charge of AuNRs was +41.16 mV since CTAB molecules were served as player surfactants. After attachment of the mesoporous silica, the potential was decreased to -13.68 mV because the mesoporous silica itself was negatively charged, and the potential rose to +28.9 mV due to its positive charge when connected to -NH₂. After grafting HA via covalent conjugation to the surface of AuNRs@mSiO₂, the zeta potential was -34.1 mV. This effect suggests that the AuNRs@mSiO₂ has been successfully modified by HA. As shown in Figure S5, no aggregation phenomenon was found after storage in the PBS and blood environment at different time points, and it remained dark brown, which led to the stability of DOX-AuNRs@mSiO₂-HA nanoparticles.

In vitro Photothermal Effect

Considering that the owners possess absorption coefficients, the photothermal efficiency of AuNRs-based nanocomposites was further evaluated in vitro by an 808 nm diode laser. As shown in Figure 3A, the photothermal conversion efficiency of AuNRs@mSiO₂-HA at different concentrations was assessed under the 808 nm laser irradiation for 5 min (2 W cm⁻²). The temperature of the AuNRs@mSiO₂-HA aqueous suspension rose rapidly with the prolonged laser irradiation time or the increasing concentration of AuNRs@mSiO₂-HA aqueous (Figure S6A-C). Following an illuminance of 600 s, the terminal temperature of the AuNRs@mSiO₂-HA aqueous suspension was increased by 26.3°C at a concentration of 200 µg mL⁻¹. In the meantime, the temperature increment of pure water is negligible, which can be visually testified by infrared thermal images of as-prepared products (Figure 3C). Furthermore, the photothermal conversion performance of the rod-based AuNRs@mSiO₂-HA was obviously dependent on the laser-power (Figure 3B). The AuNRs@mSiO₂-HA exhibited excellent chemical stability and stable photothermal conversion performance. The stability of the photothermal effect was evaluated through five laser on/off cycles. As shown in Figures 3D and S6D, the temperature of the AuNRs@mSiO₂-HA aqueous suspension (100 µg mL⁻¹, 200 µg mL⁻¹) could still reach

the similar level after repeated NIR laser irradiation for five cycles, indicating the attractive photothermal stability and re-usability of AuNRs@mSiO₂-HA during a long-range laser exposure. Photothermal conversion efficiency (η) is a crucial parameter used to evaluate the photothermal agents. On the basis of the heating-cooling curve in Figure 3E, the photothermal conversion efficiency of AuNRs@mSiO₂-HA was calculated to be 49.02% via the quantification method by Roper,⁶⁰ which was higher than the previously reported photothermal conversion nanomaterials, including Ag₂S nanoparticles (28.35%),⁶¹ gold nanoclusters (30.0%),⁶² gold nanocages (41.7%)⁶³ and so on. Due to its outstanding photothermal conversion efficiency and photothermal stability, AuNRs@mSiO₂-HA with high photothermal efficiency has great PTT potential at mild temperatures.

DOX Release from DOX-AuNRs@mSiO₂-HA

A standard curve of DOX was drawn (Figure S7) and the sample concentration was determined based on the standard DOX curve. The loading capacity of the AuNRs@mSiO₂ was evaluated by measuring the DOX concentration in solution before and after loading into the nanoparticles using UV-Vis spectrophotometer at 480 nm, and the drug loading capability of DOX-AuNRs@mSiO₂-HA was 8.0% ± 0.9%. The DOX release behavior of DOX-AuNRs@mSiO₂-HA nanoparticles was further evaluated. As shown in Figure 3F, approximately 24.3% of DOX released from DOX-AuNRs@mSiO₂-HA nanoparticles over 24 h. This result indicated a high affinity and subsequent tight retention of the surface of DOX-AuNRs@mSiO₂-HA nanoparticles toward DOX molecules, which is beneficial for preventing premature release and result in sustained in vivo therapeutic effect. To further understand the influence of NIR radiation on DOX release performance, DOX-AuNRs@mSiO₂-HA nanoparticles dispersion was irradiated with 808 nm laser (2 W cm⁻², 5 min). As shown in Figure 3F, nearly 62.3% of DOX molecules were released from DOX-AuNRs@mSiO₂-HA nanoparticles eventually. The burst release of DOX was mainly due to the rapid temperature increasing of AuNRs@mSiO₂ dispersion under NIR irradiation, which facilitates the DOX molecule thermal motion and the escape of DOX molecules from the mesochannels of AuNRs@mSiO₂ nanoparticles.⁶⁴ Additionally, a rapid release of DOX was observed at pH = 5.0 with hyaluronidase, and the cumulative amount of DOX increased

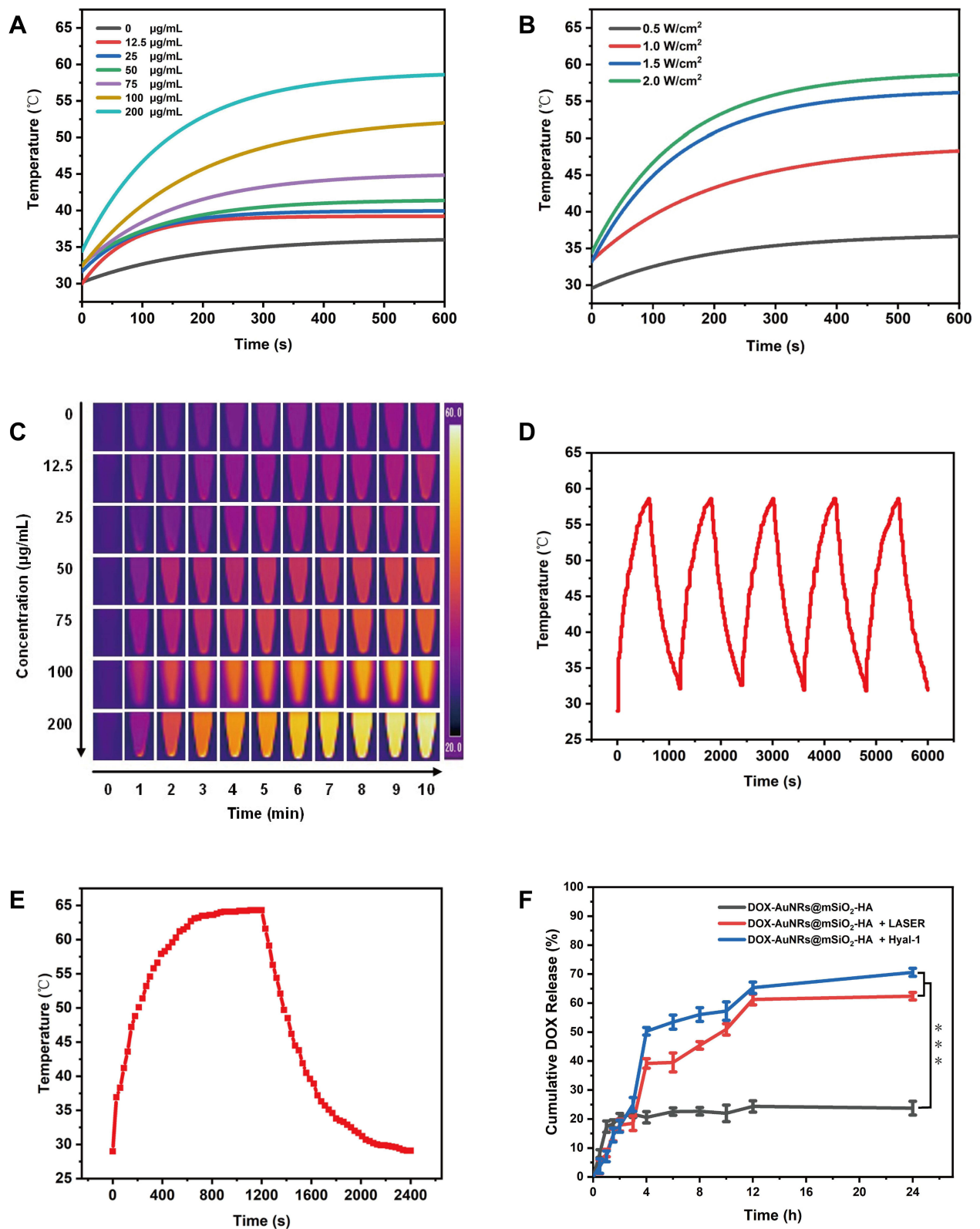


Figure 3 Temperature-rising assessment and drug release of AuNRs@mSiO₂-based nanocomposites. **(A)** Temperature change of the AuNRs@mSiO₂-HA aqueous solution under NIR laser irradiation (2.0 W cm⁻², 808 nm). **(B)** Temperature elevation in the AuNRs@mSiO₂-HA aqueous solution (1.0 mL, 200 µg mL⁻¹) with NIR laser exposure as a function of power density. **(C)** IR thermographic maps of the cavities containing AuNRs@mSiO₂-HA aqueous solution subjected to 10 min of NIR irradiation (2.0 W cm⁻², 808 nm). **(D)** Temperature evolution of AuNRs@mSiO₂-HA aqueous solution (1.0 mL, 200 µg mL⁻¹) over five lasers ON/OFF cycles of NIR laser irradiation (2 W cm⁻², 808 nm). **(E)** The photothermal response of AuNRs@mSiO₂-HA aqueous solution (1.0 mL, 200 µg mL⁻¹) exposed by NIR laser (2.0 W cm⁻², 808 nm) until reaching a stabilized temperature and then the laser was turned off. **(F)** DOX release profiles from DOX-AuNRs@mSiO₂-HA in PBS at different pH values. Data are expressed as mean ± S D (n = 3). ***P < 0.001.

significantly to 70.6% within 24 h. This effect may be due to the fact that hyaluronidase has showed its capacity to degrade HA into small fragments and promote drug release. All results demonstrated that the DOX-AuNRs@mSiO₂-HA could achieve Hyal/NIR dual-responsive release, making it possible for minimizing the drug stimulation of normal cells and improving anti-tumor efficacy.

In vitro PAI of AuNRs@mSiO₂

The high absorption coefficient of the AuNRs@mSiO₂ NIR region makes them effective contrast agents for PAI. As shown in Figure 4A, the PA signal of the AuNRs@mSiO₂ solutions was enhanced with the increasing concentrations of nanoparticles, displaying a concentration dependent manner. The quantitative result exhibited a well-correlated linear relationship in Figure 4B ($R^2 = 0.97592$). These results suggest that AuNRs@mSiO₂ are excellent candidates as positive PAI contrast agents.

In vitro Chemo-Photothermal Therapy

Encouraged by the excellent photothermal effect and the exceptional DOX loading capacity of AuNRs@mSiO₂-HA, its bio-application has been investigated. The biocompatibility of AuNRs@mSiO₂-HA was initially performed on HOK cells by a standard CCK-8 assay in vitro. No distinct cytotoxicity in HOK was observed even at higher concentrations up to 200 $\mu\text{g mL}^{-1}$ after 24 h of treatment with the AuNRs@mSiO₂-HA in our tested dose range, indicating the excellent biocompatibility of blank AuNRs@mSiO₂-HA (Figure 4C). To further confirm the synergistic therapeutic effect of DOX-AuNRs@mSiO₂-HA, CAL-27 cells were incubated with AuNRs@mSiO₂-HA, free DOX and DOX-AuNRs@mSiO₂-HA at various concentrations. The cytotoxicity of the DOX-AuNRs@mSiO₂-HA group was significantly lower than that of the free DOX group at an equivalent concentration of DOX, which should be attributed to the sustained release of DOX molecules. As shown in Figure 4D, the cell viability of CAL-27 cells incubated with DOX-AuNRs@mSiO₂-HA without NIR laser irradiation was maintained beyond 72.76% over this wide range of concentrations, further demonstrating their intrinsic biocompatibility. Such low cytotoxicity of DOX-AuNRs@mSiO₂-HA pushed us to evaluate their potential therapeutic effects on tumor cells through the desired stimulus. However, the cell viability dramatically decreased with the increased concentration of materials because of the combined effect of induced hyperthermia and released

anticancer drug DOX from the liquid PCM. In contrast, the cell viability of DOX-AuNRs@mSiO₂-HA + LASER group reduced significantly. More than 90% of cancer cells were killed at a particle concentration of 25 $\mu\text{g mL}^{-1}$, when the particle concentration increased to 50 $\mu\text{g mL}^{-1}$, almost all the CAL-27 cells were destroyed. To sum up, DOX-AuNRs@mSiO₂-HA +LASER irradiation had an exceptional synergistic therapy effect. To further investigate the photothermal therapy efficiency of DOX-AuNRs@mSiO₂-HA in vitro, the CAL-27 cells cultured in DOX-AuNRs@mSiO₂-HA at different times were irradiated with a laser at 808 nm (1 W cm⁻²). The cells were co-stained with calcein AM and propidium iodide and taken a photo by fluorescence microscopy. As shown in Figure 4E, the results of confocal fluorescence images indicate that the lethal effect of phototherapy was maintained in agreement with the CCK-8 results.

Cellular Uptake Ability

To verify that AuNRs@mSiO₂-HA nanoparticles could be phagocytosed, cellular uptake experiments were performed by HOK and CAL-27 cells incubated with gradient concentration of DOX-AuNRs@mSiO₂-HA for different periods of time (0, 2, 4, and 8 h). The fluorescence intensity and content of intracellular DOX were monitored through flow cytometry. As shown in Figure 5A–D, the DOX fluorescence intensity greatly increased with the prolonged co-incubation time or the increased concentration of materials, demonstrating that the cellular uptake was highly controllable by adjusting these parameters. These results indicate that CAL-27 cells have the capability to take DOX-AuNRs@mSiO₂-HA. As the primary HA receptor, CD44 is a cell surface glycoprotein that has been implicated in various cancers and has participated in the extravasation and migration of tumor cells. The CAL-27 cells express high levels of CD44, so that DOX-AuNRs@mSiO₂-HA has accumulated in HA mediates tumor cell uptake.

To further examine the time-dependent cell uptake and the intracellular release behavior of DOX-loaded AuNRs@mSiO₂-HA, the CLSM images of CAL-27 cells incubated with DOX-loaded AuNRs@mSiO₂-HA at different time points (2, 4 and 8 h) were collected. As shown in Figure 5E, the CLSM images were obtained for the red fluorescence of DOX and the blue fluorescence of DAPI after the nuclei were stained. With the increase of the incubation time, the DOX molecules gathered in the cell nucleus gradually increased, which suggested that DOX-

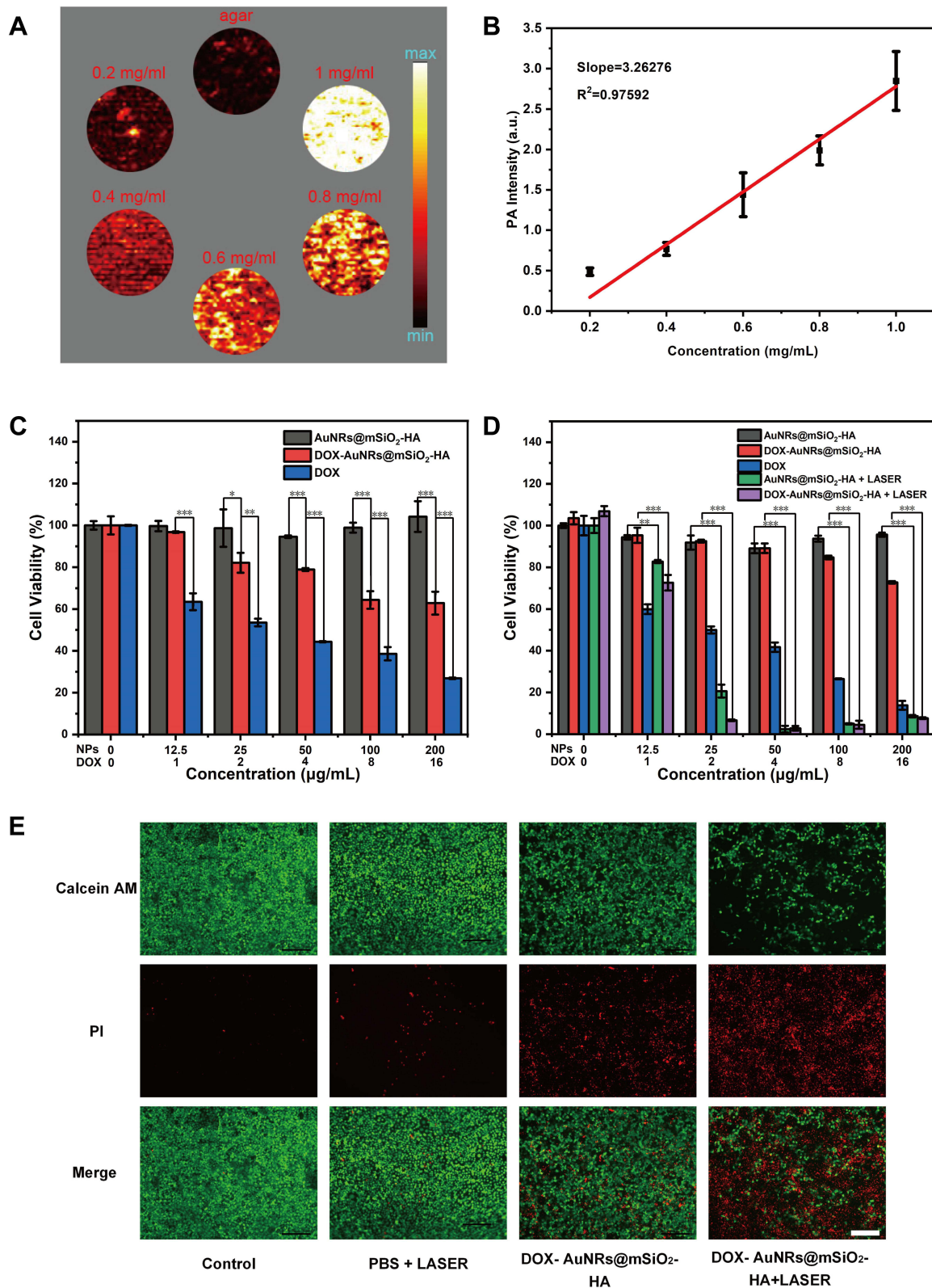


Figure 4 PAI and Combined therapy in vitro. **(A)** PA images with different AuNRs@mSiO₂ concentrations. **(B)** PA linear relationship of PA signal intensities with different AuNRs@mSiO₂ concentrations. **(C)** Relative cell viability of HOK cells after incubation with different concentrations of DOX, AuNRs@mSiO₂ and DOX-AuNRs@mSiO₂-HA for 24 h. **P* < 0.05; ***P* < 0.01; ****P* < 0.001. **(D)** Relative cell viability of CAL-27 cells after incubation with different concentrations of DOX, AuNRs@mSiO₂ and DOX-AuNRs@mSiO₂-HA for 24 h, followed by irradiation with 808 nm laser (1W cm⁻²) for 5 min. ***P* < 0.01; ****P* < 0.001. **(E)** Fluorescence microscope images of Calcein AM (green fluorescence, live cells) and Propidium iodide (PI, red fluorescence, dead cells) costained CAL-27 cells incubated with PBS, LASER, DOX-AuNRs@mSiO₂-HA and DOX-AuNRs@mSiO₂-HA + LASER (100 μg mL⁻¹). The scale bar is 100 μm.

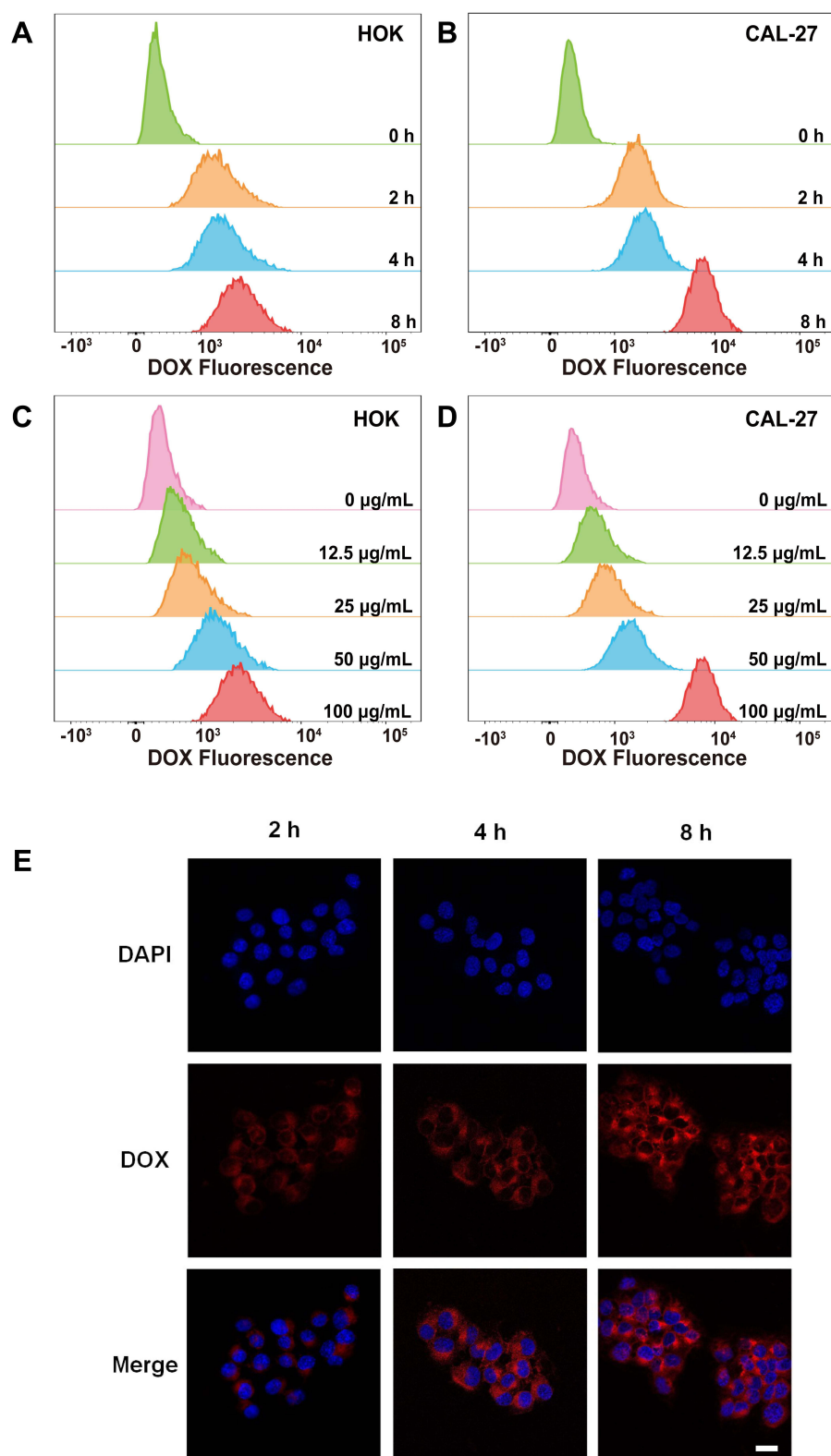


Figure 5 Cellular uptake study. (A) Intracellular DOX fluorescence intensity of HOK cells measured by flow cytometry after incubating cells with 100 µg mL⁻¹ DOX-AuNRs@mSiO₂-HA for 0, 2, 4 and 8 h. (B) Intracellular DOX fluorescence intensity of CAL-27 cells measured by flow cytometry after incubating cells with 100 µg mL⁻¹ DOX-AuNRs@mSiO₂-HA for 0, 2, 4 and 8 h. (C) Intracellular DOX fluorescence intensity of HOK cells measured by flow cytometry after incubating cells with DOX-AuNRs@mSiO₂-HA for 8 h. (D) Intracellular DOX fluorescence intensity of CAL-27 cells measured by flow cytometry after incubating cells with DOX-AuNRs@mSiO₂-HA for 8 h. (E) Confocal laser scanning microscope (CLSM) images of CAL-27 cells showing colocalization of nucleus and DOX filmed at 2, 4, 8 h after incubating cells with DOX-AuNRs@mSiO₂-HA at 37 °C. Nucleus stained with DAPI. The scale bar is 20 µm.

loaded nanoparticles could facilitate cellular internalization and final delivery of DOX to the cell nuclei. It can be concluded that the DOX-AuNRs@mSiO₂-HA has great potential as a promising nanocarrier for the administration of drugs against oral cancer cells.

In vivo PAI of AuNRs@mSiO₂-HA

Take advantage of the high absorption of NIR, AuNRs@mSiO₂-HA can also be used as a contrast agent in PAI, which provides the local distribution of nanoparticles in the tumor region. As shown in Figure 6A, CAL-27 tumor-bearing mice with a tumor volume of approximately 100 mm³ were randomly divided into four groups of five mice per group. With the guidance of PAI, AuNRs@mSiO₂-HA suspensions (200 µL, 1 mg mL⁻¹) were injected into tumor-bearing mice by injection into the tail vein. PA signals in the tumor region were recorded at different time points (0, 2, 4, 8, 12, 24 h). As shown in Figure 6B and C, the PA signal increased gradually within the first 8-h post-injection at tumor site and then decreased, which indicated that the maximum nanoparticles enrichment in the tumor region was achieved at 8 h post-injection.

In vivo Chemo-Photothermal Therapy

Inspired by the excellent accumulation and anti-tumor effect in vitro of DOX-AuNRs@mSiO₂-HA, the efficacy of in vivo therapy was further evaluated in mice. After injection of particulate suspensions through the caudal vein, the tumors are completely exposed to 808 nm laser at 8 h after the injection. The temperature of the tumor site in the DOX-AuNRs@mSiO₂-HA group increased from 28.6 to 55.7 °C after laser irradiation (Figure 6D), while the temperature of the mice in the PBS group did not increase significantly after 5 min of laser irradiation. As shown in Figure 6E, the digital photographs of tumors on the 12th day after treatment show that tumors in DOX-AuNRs@mSiO₂-HA + LASER group are completely ablated. The body weight curves of the four groups showed no significant difference from each other, which implied that treatments did not affect the normal development of the mice during our experiment (Figure 6F). We found that tumor volumes in the control groups increased rapidly during the experiment (Figures 6G and 7A). In comparison, the DOX-AuNRs@mSiO₂-HA and PBS+LASER groups showed a slower tumor growth rate than the control groups, which means the therapeutic effect of single chemotherapy or PTT alone was limited. When mice injected with DOX-

AuNRs@mSiO₂-HA were exposed to the laser, the tumor growth was significantly suppressed within the first 12 days. Moreover, the tumors were gradually ablated in the last 8 days of the experiment, which indicated DOX-AuNRs@mSiO₂-HA + LASER had a better anti-tumor and therapeutic efficacy than any other group, and the synergistic effect of PTT and chemotherapy is effective. These results agree fairly well with the tumor growth curves. As illustrated in Figure 7B, the follow-up time for these treated mice was recorded. After irradiation with NIR light, the DOX-AuNRs@mSiO₂-HA group was the best in terms of the survival rate among all the experimental groups. Xu and co-authors found that the multifunctional nanoplatform loaded with DOX was used to treat the tumor-bearing mouse model of breast cancer, in contrast, the chemo-photothermal therapy group showed the best anti-tumor efficacy.⁶⁵ Furthermore, H&E staining of tumor slices showed that most of the cells in the tumors of mice of DOX-AuNRs@mSiO₂-HA +LASER group were severely damaged, while the cells in the tumors of mice of the other treatment groups were only partially destroyed (Figures 7C and S8). The above results indicated that DOX-AuNRs@mSiO₂-HA had good photothermal properties and could carry out effective Chemo-Photothermal therapy. To further confirm the biocompatibility of DOX-AuNRs@mSiO₂-HA, mice were dissected within 30 days of treatment, and their tumors and major organs were subjected to histological analysis. As shown in Figure 7D, there was no obvious organ damage and inflammation compared to the PBS group. The safety and low toxicity of DOX-AuNRs@mSiO₂-HA were also demonstrated to be good. These results suggested that DOX-AuNRs@mSiO₂-HA nanoparticles could serve as an effective platform for cancer chemo-photothermal therapy in vivo relatively low systemic toxicity.

Conclusion

In conclusion, we have successfully fabricated novel DOX-AuNRs@mSiO₂-HA which possesses ultrahigh strong PAI signal, prominent photothermal conversion and drug loading ability. The in vitro cellular and in vivo animal experiments demonstrated that DOX-AuNRs@mSiO₂-HA could simultaneously exert chemotherapy and photothermal effect under the laser irradiation. Overall, this AuNRs@mSiO₂-HA PTT platform combined with chemotherapy showed massive potential as a nanotheranostic for the diagnosis and treatment of precision cancer therapy. However, the animal model of our study is the model of

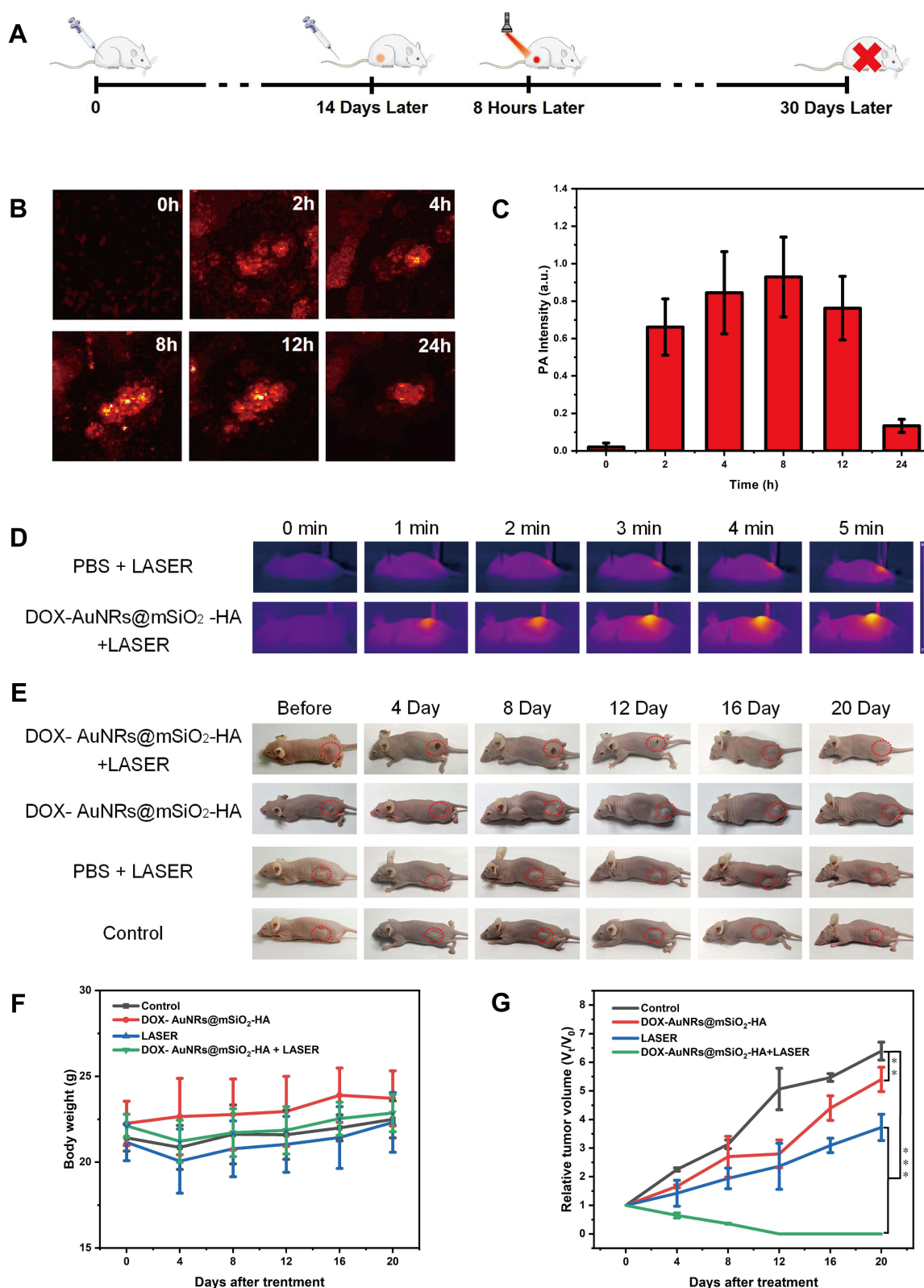


Figure 6 In vivo PAI and PTT of CAL-27 tumor-bearing mice. **(A)** Scheme of CAL-27 tumor-bearing mouse development and Chemo-Photothermal Therapy. **(B)** PAI in the tumor region after intravenously injected DOX-AuNRs@mSiO₂-HA are recorded at different time points after intravenous administration. **(C)** PA intensity in the tumor region after intravenously injected DOX-AuNRs@mSiO₂-HA are recorded at different time points after intravenous administration. **(D)** Photothermal images of CAL-27 tumor-bearing mice injected with PBS and DOX-AuNRs@mSiO₂-HA (200 μ L, 1 mg mL⁻¹) under NIR laser irradiation (808 nm, 2W cm⁻²) for 5 min at 6-h post-injection. **(E)** Representative photos of CAL-27 tumor-bearing mice after different days before (0 d) and after (4, 8, 12, 16 and 20 d) different treatments. **(F)** Average body weights of mice from each group after various treatments: (1) Control, without treatment; (2) DOX-AuNRs@mSiO₂-HA, injection of DOX-AuNRs@mSiO₂-HA only; (3) LASER, irradiation with laser only; (4) DOX-AuNRs@mSiO₂-HA + LASER, injection of DOX-AuNRs@mSiO₂-HA and irradiation with a laser. **(G)** Relative volumes of tumors after the above treatments, normalized to their initial volumes. ** $P < 0.01$; *** $P < 0.001$.

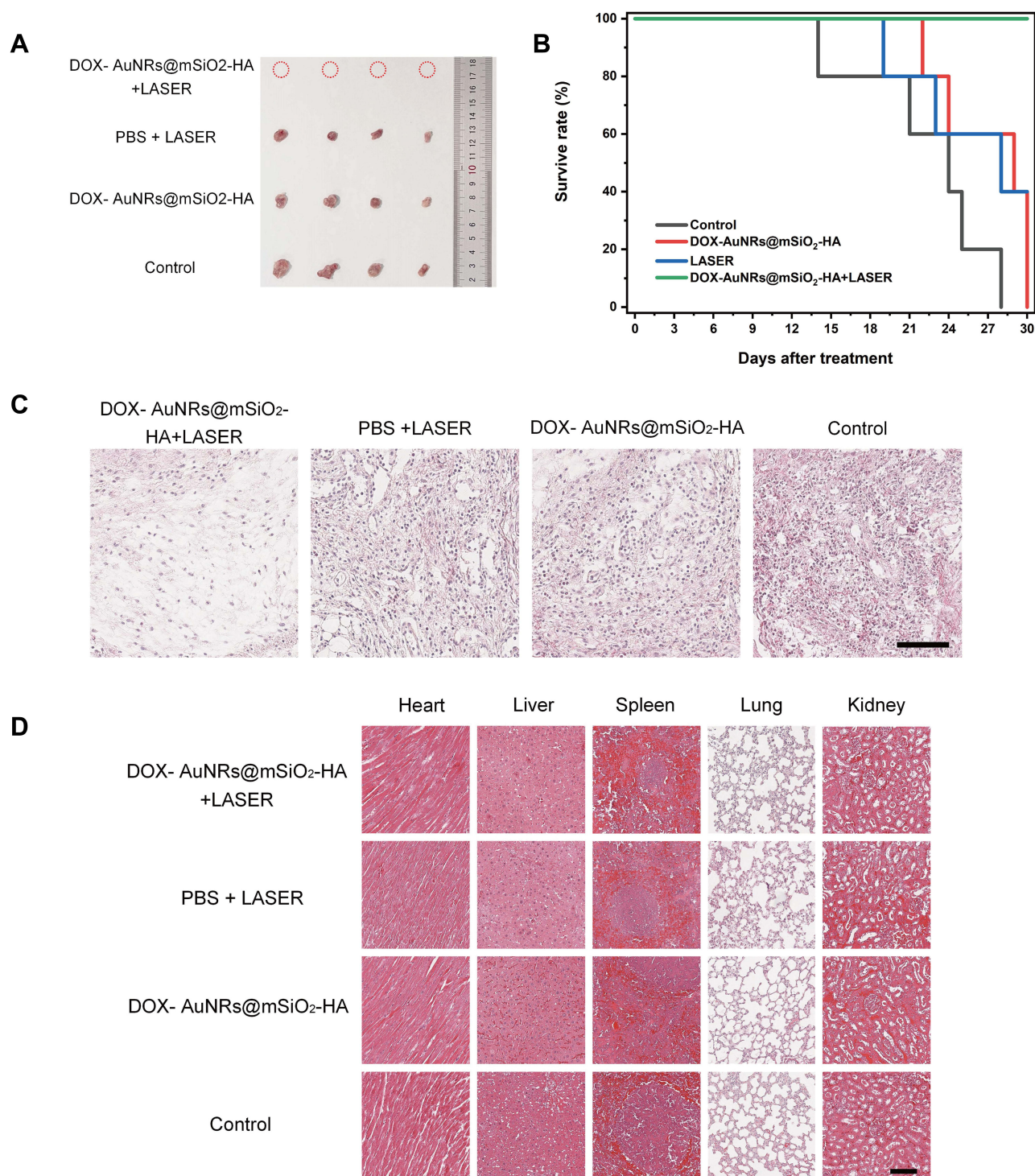


Figure 7 In vivo antitumor activity of different types of CAL-27 tumor-bearing mice. **(A)** Optical images of the dissected tumors from CAL-27 tumor-bearing mice in different treatment groups at day 30 after sacrificing the mice. **(B)** Survival curves of CAL-27 tumor-bearing mice in various groups after NIR-light irradiation treatment. **(C)** Histological section of tumor stained with hematoxylin and eosin after intravenous administration of DOX-AuNRs@mSiO₂-HA. The scale bar is 100 μ m. **(D)** Histological section of vital organs (heart, liver, spleen, lung and kidney) stained with hematoxylin and eosin after intravenous administration of DOX-AuNRs@mSiO₂-HA. The scale bar is 100 μ m.

back ectopic transplanted tumor in tumor-bearing mice, which is mainly limited by the imperfection of the imaging device and treatment device. Moving forward, we will

further enhance experimental equipment and conduct comprehensive research on the diagnosis and treatment of primary oral cancer.

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Disclosure

The authors reported no conflicts of interest in this work.

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