

Nanomaterial-Based Electrically Conductive Hydrogels for Cardiac Tissue Repair

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Abstract: Cardiovascular disease is one of major causes of deaths, and its incidence has gradually increased worldwide. For cardiovascular diseases, several therapeutic approaches, such as drugs, cell-based therapy, and heart transplantation, are currently employed; however, their therapeutic efficacy and/or practical availability are still limited. Recently, biomaterial-based tissue engineering approaches have been recognized as promising for regenerating cardiac function in patients with cardiovascular diseases, including myocardial infarction (MI). In particular, materials mimicking the characteristics of native cardiac tissues can potentially prevent pathological progression and promote cardiac repair of the heart tissues post-MI. The mechanical (softness) and electrical (conductivity) properties of biomaterials as non-biochemical cues can improve the cardiac functions of infarcted hearts by mitigating myocardial cell death and subsequent fibrosis, which often leads to cardiac tissue stiffening and high electrical resistance. Consequently, electrically conductive hydrogels that can provide mechanical strength and augment the electrical activity of the infarcted heart tissue are considered new functional materials capable of mitigating the pathological progression to heart failure and stimulating cardiac regeneration. In this review, we highlight nanomaterial-incorporated hydrogels that can induce cardiac repair after MI. Nanomaterials, including carbon-based nanomaterials and recently discovered two-dimensional nanomaterials, offer great opportunities for developing functional conductive hydrogels owing to their excellent electrical conductivity, large surface area, and ease of modification. We describe recent results using nanomaterial-incorporated conductive hydrogels as cardiac patches and injectable hydrogels for cardiac repair. While further evaluations are required to confirm the therapeutic efficacy and toxicity of these materials, they could potentially be used for the regeneration of other electrically active tissues, such as nerves and muscles.

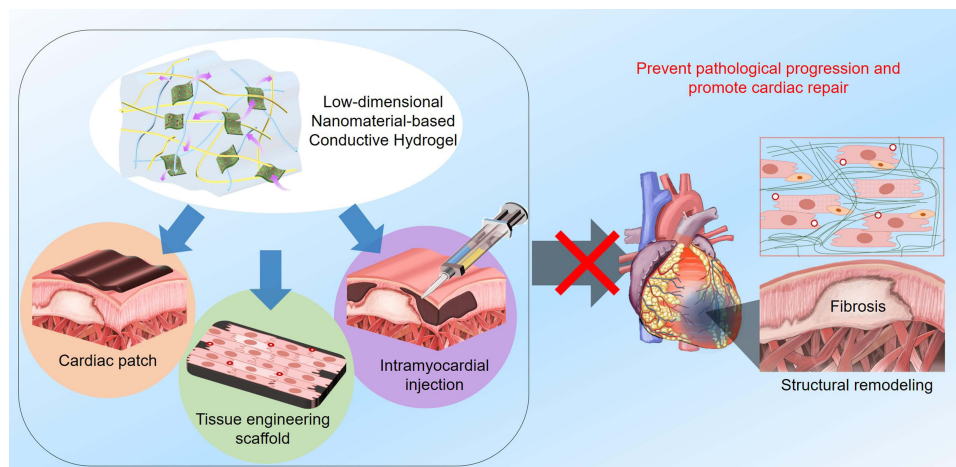
Keywords: nanomaterials, conductive, hydrogel, cardiac tissue engineering

Introduction

Cardiovascular diseases are fatal, accounting for more than 17.9 million deaths annually worldwide.^{1,2} Particularly, ischemic heart disease, which ultimately manifest as myocardial infarction (MI), is a major cause of cardiovascular disease-associated deaths.¹ For example, MI cases were reportedly 8.8 million (3.1%, age ≥ 20 years) in the United States in 2015–2018 and 104,280 of the patients (all years) died in 2019.¹ MI is a consequence of myocardial cell death, mainly driven by myocardial ischemia due to atheromatous plaque rupture and thrombus formation in the coronary artery, which leads to insufficient blood flow and oxygen supply to the heart muscle.³ The infarcted heart tissues undergo ventricular remodeling, which includes necrosis, structural remodeling, ventricular wall thinning, chamber dilatation, and eventually fibrosis.^{4,5} (Figure 1) This pathological process post-MI (ischemic cardiomyopathy) is associated with development of heart failure. Heart transplantation is currently the most feasible method for heart repair after MI; however, it has several critical issues, such as insufficient number of donors and risks of infection.⁶ Hence, developing other efficient MI treatments is highly necessary.

After MI, cardiomyocytes (CMs) in the heart muscles undergo severe cell death. The damaged heart tissues suffer the pathological remodeling due to the insufficient self-regeneration capability of the heart tissues, which eventually causes fibrous collagen fiber deposition in the infarcted zone. These fibrotic tissues lead to cardiac tissue wall thinning and

Graphical Abstract



stiffening.² (Figure 1) In addition, CMs in the non-conductive fibrotic area are not electrically interconnected with other cells.¹³ This electrical disconnection impairs synchronous cardiac cell coupling and cardiac contraction/relaxation. Improper electrical signaling in infarcted areas frequently causes fatal ventricular arrhythmia and sudden cardiac cell death.¹³ For infarcted heart, mechanical support to the infarcted myocardium can alleviate its pathological remodeling. Hence, biomaterial-based treatment (eg, cardiac patches and hydrogel injection into myocardium) can potentially augment the mechanical functions of the infarcted heart.^{5,7,8} Concurrently, electrically conductive materials have been found to improve electrophysiological cardiac functions.^{9–12} Numerous studies have been focused on regenerating infarcted heart function, such as artificial heart transplantation, drugs, cell therapy, and biomaterial implants.^{14–19} Among these, biomaterials have been actively examined for cardiac repair.^{20,21} Biomaterial-based approaches can offer several benefits, such as ease in production, versatility in modification, and therapeutic activity. Biomaterials can be designed and engineered to deliver specific mechanical, electrical and biological cues to infarcted heart to enhance its regeneration. In addition, biomaterials can be used together with drugs and cells to further enhance their therapeutic efficacy for regeneration of heart function.

Hydrogels are three-dimensional (3D) hydrophilic polymeric networks.²² They are structurally and functionally similar to the natural extracellular matrix (ECM).² The mechanical properties of hydrogels are similar to those of the cardiac tissue (eg, elastic modulus, toughness, and stretchability), which can provide mechanical support to infarcted hearts and attenuate pathological remodeling.^{23,24} For cardiac tissue engineering, hydrogels have been produced in the

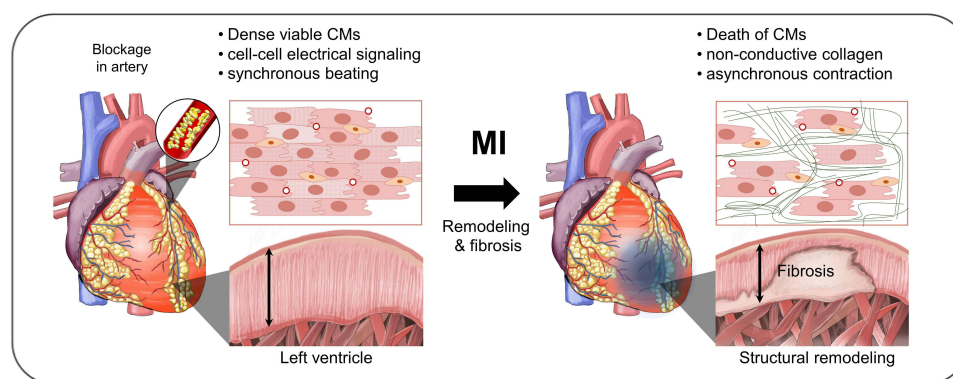


Figure 1 Myocardial infarction (MI) and pathological progression of the infarcted heart showing ventricular remodeling and fibrosis.

form of a patch and filler which can mechanically support heart tissue functions; furthermore, they have been engineered by controlling their composition and manufacturing processes.^{8,25} Additionally, hydrogels can be used as delivery vehicles,^{26–29} and can address the issues associated with directly injecting therapeutic components (drugs and cells) into the cardiac muscle, such as sustained drug release or enhanced cell viability.^{30,31} The sustained release of therapeutic substances can be achieved by creating specialized interactions between polymeric chains and drug substances. For cell delivery, the 3D microenvironments of hydrogels can enhance the viability and therapeutic functions of the delivered cells.^{32–35}

Recently, electrically conductive hydrogels have garnered significant attention in biomedical fields for bioelectrode and tissue engineering applications.^{36–39} Because conventional hydrogels are electrically insulating, conductive hydrogels are usually fabricated by formulating conductive materials with hydrophilic polymers.^{40,41} As a result, conductive hydrogels can be engineered to exhibit mechanical and electrical properties similar to those of normal cardiac tissue.^{25,42–44} Note that the native myocardium tissue typically shows 1 mS/cm and 20–500 kPa of conductivity and Young's modulus, respectively.^{45,46} Electrically conductive biomaterials can promote cardiac contraction/relaxation functions and electrical coupling,⁴² induce the maturation of CMs in the infarcted heart,⁴³ and prevent its progression to arrhythmia.⁴⁷ Consequently, conductive hydrogels can be a good option to mechanically support heart tissues and effectively transmit electrical signals within the myocardium for cardiac tissue repair post-MI. Various electrically conductive materials (eg, conductive polymers, metals, and nanomaterials) have been used to produce conductive hydrogels for cardiac tissue engineering. Among them, one-dimensional (1D) and two-dimensional (2D) nanomaterials present unique material characteristics (eg, high electrical conductivity, large surface areas, strong molecular interactions with various [macro]molecules, and versatility in modification), which benefit the development of functional conductive hydrogels capable of effectively modulating cardiac cell behaviors and stimulating cardiac tissue regeneration.⁴⁸ These unique properties of low-dimensional nanomaterials can be used to develop the high-performance conductive hydrogels presenting desirable biological, electrical, and mechanical characteristics for cardiac repair. Consequently, we focused on the nanomaterial-based conductive hydrogels for cardiac repair in this review. In the first section, we describe the fabrication of conductive hydrogels using different types of low-dimensional nanomaterials. Subsequently, the studies with various conductive hydrogels containing low-dimensional nanomaterials for cardiac repair are described. Next, the applications of conductive hydrogels in cardiac treatments, mainly as patches and injectable hydrogels, are reviewed along with recent results. Finally, conductive hydrogels with newly discovered low-dimensional nanomaterials are described.

Conductive Hydrogels for Cardiac Repair

Fabrication of Conductive Hydrogels

Conductive hydrogels are typically fabricated by incorporating conductive components into hydrogel networks. These composite hydrogels were prepared by the in situ formation of a conductive network within the pre-formed hydrogels or polymerization of a pre-polymer solution containing conductive materials.⁴⁹ To fabricate conductive hydrogels with nanomaterials, pre-polymer solutions containing conductive 1D or 2D nanomaterials are prepared and subjected to gelation via various polymerization methods (eg, photopolymerization, thermal polymerization, and self-assembly).^{50–52} Importantly, low-dimensional conductive components should be homogeneously dispersed and stabilized within the polymer matrices to obtain an appropriately conductive network.^{53–55} Therefore, the molecular interactions between conductive components and polymeric chains should be carefully examined. Conductive components can be covalently conjugated with polymer matrices to enhance the dispersion of conductive components and the stability of the resultant conductive hydrogels.^{44,56,57} The fabrication methods also greatly influence the characteristics of the prepared conductive hydrogels, such as conductivity, stability, biosafety, and processability. For example, conductive hydrogels can be fabricated simply by blending and cross-linking. However, several issues, such as the non-uniform distribution of the conductive components within a hydrogel and the potential instability and toxicity resulting from the leakage of conductive components, frequently cause difficulties in their biomedical applications.^{44,58} Alternatively, the chemical conjugation of a conductive component to a hydrogel network can improve conductivity, long-term stability, and safety; however, this process is relatively complicated and requires an additional washing step to remove unreacted chemicals and by-products.^{59,60} Overall, the performance of conductive hydrogels is affected by various factors, such as the

polymer type, crosslinking type and degree, conductive component type, and composition.⁶¹ For example, biodegradable conductive hydrogels can be prepared by formulating conductive components and natural biodegradable polymers (eg, gelatin, collagen, chitosan, and alginate) or synthetic hydrolyzable polymers (eg polyesters, polyanhydrides, and polycarbonates).^{62–67} Furthermore, multifunctional conductive hydrogels (eg mechanical, sensory, anti-freezing, adhesive and self-healing properties) can be designed and fabricated using polymers with specific biological, chemical, and physical properties.⁶⁸

Various conductive nanomaterials, including carbon-based nanomaterials and MXenes, have been developed (Figure 2). One- and two-dimensional nanomaterials have unique characteristics, such as high electrical conductivity, large surface area, various molecular interactions, and flexibility, which make them promising for developing new functional materials in various fields, such as energy, optics, electronics, and medicine.^{69–73} Other conductive components, such as conductive polymers and metal nanomaterials, can also be useful for producing conductive hydrogels and have shown utility in various applications, including cardiac tissue engineering.^{39,74–76} However, several challenges remain concerning material stability, mass production, and effectiveness.⁷⁷ Therefore, we focused on conductive hydrogels composed of non-metallic low-dimensional nanomaterials with respect to their fabrication and potential uses in cardiac repair. It should be noted that the biosafety or toxicity of most nanomaterials has not been clearly determined because their interpretations differ depending on the type, structure, and functionalization of nanomaterials, and in vitro and in vivo experimental conditions. Accordingly, the clinical feasibility of conductive hydrogels composed of different 1D and 2D nanomaterials should be carefully evaluated in future studies.

Applications of Conductive Hydrogels in Cardiac Treatment

For cardiac regeneration, conductive hydrogels have been administered via intramyocardial injection, intrapericardial injection, or by attaching to the epicardium of the heart.^{5,78,79} Administration of a hydrogel by injection mainly supports the mechanical function of the myocardium within the local cardiac tissue. On the other hand, a cardiac patch assists the mechanical function of the heart by preventing excessive dilation. In addition, therapeutic molecules can be loaded into hydrogels for local delivery in the myocardium (hydrogel injection) or from the heart surface (attachment). These conductive hydrogels can also serve as in vitro platforms to study cardiac cell/tissue responses to mechanical and electrical environments and develop functional tissue engineering scaffolds for cardiac repair (Figure 2).

Injectable hydrogels can be administered with minimal invasiveness.⁸⁰ Various injectable hydrogels have been developed for tissue engineering and drug delivery applications. For example, temperature-responsive polymers, pH-responsive polymers, mild chemical reactions, photopolymerization, and magnetic polymerization have been developed to produce injectable hydrogel systems.⁸¹ The conductive hydrogel injected into the myocardium can provide a 3D

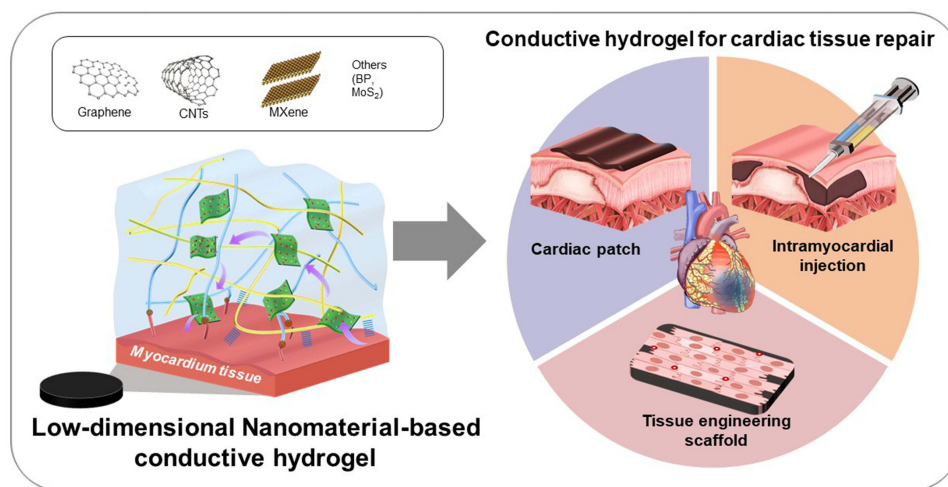


Figure 2 Conductive hydrogels containing low-dimensional non-metallic nanomaterials and their various applications in cardiac repair.

electrical bypass around the MI site and aid in restoring the electrical communications between cells and/or tissue.^{82,83} Various conductive materials can be incorporated into injectable hydrogel systems to produce injectable conductive hydrogels. Specifically, injectable conductive hydrogels can be formed after intramyocardial or intrapericardial injection through in situ crosslinking of pre-polymers containing conductive materials based on various reactions, such as photo-crosslinking, click reactions, Schiff base reactions, and Michael reactions.^{84,85} Wang et al designed an injectable conductive hydrogel via in situ polymerization of tetraaniline-polyethylene glycol (TA-PEG) and thiolated hyaluronic acid (HA-SH) via Michael addition.⁸⁶ Adipose-derived stem cells (ADSCs) and lipofectamine nanocomplexes containing plasmid DNA-eNOs (endothelial nitric oxide synthase) were loaded into the gels and subsequently injected into the infarcted heart. They demonstrated an increased expression of eNOs in the myocardium with upregulated proangiogenic factors and structural and functional cardiac improvements, as indicated by electrocardiography, cardiography, and histological analysis. (Figure 3A) However, these hydrogels had low conductivity (0.023 S/m) and the conducting polymer (tetraaniline) showed drawbacks, such as lack of biosafety and stability in vivo.^{87,88} Intrapericardial injection of hydrogels is an attractive treatment option for cardiac repair.^{89–91} The pericardium is a double-walled sac that plays a key role in protecting cardiac tissues from infection and provides lubrication for heart movements.^{91–93} The space between the double-walled sac, called the pericardial cavity, is usually filled with pericardial fluid. Hydrogel injection into this pericardial cavity does not require fixation of the injected hydrogel using surgical sutures or adhesives, and supports the mechanical properties of heart tissues. Zhu et al injected a decellularized ECM hydrogel embedded with mesenchymal stem cell-derived exosomes and induced pluripotent stem cell-derived cardiac progenitors into the pericardial cavity.⁹¹ Although conductive hydrogels have not yet been tested for pericardial injection, an injectable conductive hydrogel might be beneficial to promote heart regeneration after MI by providing physical support and electrical bypass to the heart.

Conductive cardiac patches are another promising application of conductive hydrogels for inducing cardiac tissue regeneration.^{47,94} Unlike injection into the myocardium, a cardiac patch does not require invasion of the myocardium or pericardium. Conductive hydrogel patches can provide a 2D electrical bypass surrounding the epicardium.⁴⁷ Cardiac patches, including conductive hydrogels, are usually fixed onto the epicardium using conventional surgical sutures, staples, or light irradiation,^{94,95} which can lead to bleeding, blockage of blood supply, or further inflammatory responses.

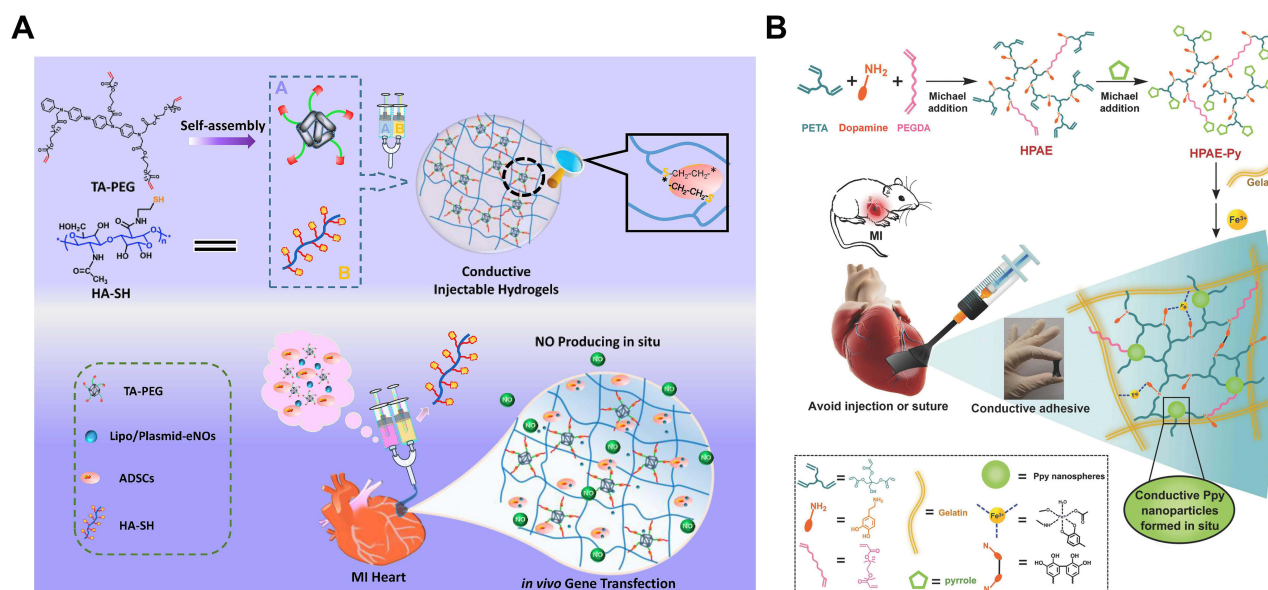


Figure 3 Conductive hydrogels for cardiac repair. (A) Intramyocardial injection of a conductive hydrogel consisting of TA-PEG and HA-SH loaded with ADSCs and Lipofectamine/plasmid-eNOs. (B) Conductive cardiac patch composed of HPAE, gelatin, and PPy nanospheres. The composite was paintable and in situ formed as a conductive and adhesive cardiac patch on the epicardium of infarcted heart.

Notes: (A) Reprinted with permission from Wang VV, Tan B, Chen J et al. An injectable conductive hydrogel encapsulating plasmid DNA-eNOs and ADSCs for treating myocardial infarction. *Biomaterials*. 2018;160:69–81.⁸⁶ Copyright (2018) Elsevier. (B) Reprinted with permission from Liang S, Zhang Y, Wang H et al. Paintable and Rapidly Bondable Conductive Hydrogels as Therapeutic Cardiac Patches. *Adv Mater*. 2018;30(23):1,704,235.⁴⁴ ©Wiley 2018.

Therefore, the adhesive property of conductive hydrogels is desired to stably immobilize conductive patches onto the epicardium. The adhesiveness of hydrogels can be achieved through physical or chemical interactions between hydrogel components and cardiac tissue.^{7,44} For example, Tang et al prepared an adhesive cardiac patch using commercial fibrin glue.⁹⁶ However, commercial bioadhesives (eg, cyanoacrylates and fibrin glue) often exhibit cytotoxicity, high stiffness, insufficient adhesion, and structural instability.^{95,97–99} Recently, several adhesive hydrogels were developed in the forms of paintable gels,⁴⁴ sprayable gels,¹⁰⁰ and lyophilized tapes^{101,102} to improve adhesion strengths at cardiac tissue interfaces. Liang et al developed paintable and rapidly bondable conductive hydrogels via Fe^{3+} -triggered polymerization of pyrrole-conjugated hyperbranched poly(amino ester) with gelatin.⁴⁴ This conductive and adhesive hydrogel could be painted onto the epicardium, and it bonded strongly to the beating heart, remained intact for four weeks, and significantly restored cardiac function and revascularization of the infarcted myocardium. (Figure 3B) However, in view of cytotoxicity, the residual pyrrole monomers in the in situ-formed paintable hydrogel may be a potential concern. In addition, the resultant conductive hydrogel had very low conductivity (0.0651 S/m).⁴⁴ Few studies have reported on adhesive and conductive cardiac patches. Nevertheless, adhesive and conductive hydrogel patches composed of low-dimensional nanomaterials (eg, carbon nanotube (CNT), graphene, and MXene) are expected to be promising for efficient cardiac repair.

Nanomaterials-Incorporated Conductive Hydrogels for Cardiac Repair

Carbon-Based Nanomaterials

Carbon-based nanomaterials have diverse structures and chemical properties. Such diverse structures of carbon nanomaterials are attributed to various hybridization modes (sp , sp^2 , and sp^3) between the carbon atoms.¹⁰³ The ratios of each hybridization determine the structures of the carbon nanomaterials as 0D, 1D, and 2D, which correspond to quantum dots, carbon nanotubes, and graphene, respectively.¹⁰⁴ Allotropes, with their unique advantages, can be extensively used in a variety of applications, including the fabrication of conductive hydrogels. The electrical properties of a carbon nanostructure increase as the anisotropy and degree of replication increase. For example, typical CNT and graphene exhibit excellent electrical conductivities of 10^4 – 10^8 S/m and 10^4 – 10^5 S/m, respectively.^{105–107} Carbon nanomaterials are very small and have high surface-area-to-mass ratios. For example, graphene is an atomically thin 2D material with lateral sizes ranging from tens to thousands of nanometers. These unique structures enable efficient conductive network formation, intimate interactions with biological components (eg, proteins), and effective electrical transmission with cells and tissues in relatively small amounts. Additional functionalization of the carbon nanomaterials can improve the performance of the prepared conductive hydrogels by modulating their interactions with other components (eg, solvents, nanomaterials, matrices, and biological molecules) and/or themselves. In this section, we focus on conductive hydrogels composed of various carbon-based nanomaterials for cardiac tissue applications.

CNTs

CNTs are 1D cylindrical nanostructured carbon materials with high anisotropy and extremely high aspect ratio.¹⁰⁸ Based on the number of cylindrical graphene layers, CNTs are classified into single-walled (SWCNTs; 0.4–2 nm in diameter) or multi-walled (MWCNTs; 2–100 nm in diameter) CNTs.¹⁰⁹ CNTs typically exhibit high electrical conductivities, flexibilities, and mechanical strengths.¹⁰⁴ CNTs have been used in a wide range of biomedical applications, including in drug delivery and tissue engineering.^{110–112} For fabricating CNT-incorporated conductive hydrogels, CNTs must be well dispersed in a hydrophilic polymer matrix and aqueous solution, owing to the inherent hydrophobicity of CNT.^{113,114} To this end, CNTs are commonly functionalized with substances containing polar functional groups, such as carboxyl acid groups, to be hybridized with various hydrophilic polymers to form a conductive hydrogel.¹¹⁵

CNT-based conductive hydrogels have been produced using various polymers for cardiac tissue applications.^{52,116} Shin et al prepared CNT–gelatin methacrylate (GelMA) hydrogels and reported their excellent mechanical integrity, electrophysiological functions, and potential to be used as cardiac patches.⁴⁶ Myocardial tissues cultured on the 50 μm thick CNT–GelMA showed higher synchronous beating rates and lower excitation thresholds than those cultured on CNT-free hydrogel controls. Li et al chemically conjugated SWCNTs with temperature-responsive poly

(N-isopropylacrylamide) (PNIPAAm) and intramyocardially injected this composite hydrogel with brown adipose stem cells (BASCs) into infarcted hearts.⁵² They found that myocardial injection of PNIPAAm/SWCNT hydrogels promoted the engraftment of encapsulated BASCs in the myocardium and improved cardiac tissue organization and echocardiographic functions. Various types of cells, such as neonatal CMs, BASCs, human-induced pluripotent stem cell (hiPSC)-derived CMs, and human coronary artery endothelial cells (HCAECs), have been encapsulated in CNT-based conductive hydrogels and studied as engineered cardiac tissues.^{52,117–119} CMs in or on CNT-based conductive hydrogels showed enhanced cell-cell electrical coupling, synchronous beating, and CM maturation (eg, high expression of sarcomeric α -actinin and gap junction protein). Furthermore, CNTs have been functionalized with various moieties to improve their miscibility with polymer chains and/or to provide additional cues to promote cardiac regeneration. For example, conductive hydrogels composed of hydrazide-functionalized CNTs and the pericardial matrix enhanced the maturation of hiPSC-derived cardiomyocytes. Hydrogels with positively charged hydrazide-functionalized CNTs increased cellular alignment, Connexin-43 expression, and sarcomere organization of hiPSC-derived CMs, which was speculated to be due to enhanced interactions between the positively charged CNTs and negatively charged cellular membrane.¹¹⁸ (Figure 4A–C) In another study, Izadifar et al fabricated a cell-laden hydrogel cardiac patch consisting of HCAECs, carboxyl-functionalized CNTs, and alginate.¹¹⁹ The incorporation of carboxyl-functionalized CNTs significantly improved the viscoelastic behavior and electrical conductivity of the composite hydrogels. Furthermore, CNTs aligned within hydrogel matrices can induce cellular orientation and differentiation. Ahadian et al fabricated CNT-aligned GelMA hydrogels via dielectrophoresis and found that these hydrogels showed higher conductivity and promoted cardiac differentiation (eg, expression of cardiac markers and beating) of embryonic bodies compared to pure GelMA and randomly aligned CNT/GelMA hydrogels.¹²⁰

Although the mechanisms by which CNTs influence the behavior of CMs have not been clearly elucidated, several mechanisms have been proposed. Sun et al found that neonatal CMs in SWCNT-incorporated collagen hydrogels exhibited enhanced cell adhesion, intercalated disc (IDs)-related protein expression, ID assembly, and functionality.^{121,122} In particular, the β 1-integrin-mediated FAK and RhoA signaling pathways were suggested to be responsible for upregulating the electrical and mechanical junction proteins of CMs in the hydrogels, respectively. Lee et al prepared three different types of carbon-nanomaterial-based hydrogels (CNT-, graphene oxide (GO)-, and reduced GO (rGO)-GelMA) and explored CM maturation on individual hydrogels.¹²³ They suggested that hydrogels with higher electrical conductivity (CNT- and rGO-GelMA) enhanced CM maturation compared with the less conductive hydrogel (GO-GelMA). Interestingly, the CM phenotypes were different on these conductive hydrogels. For example, CMs on CNT-GelMA, GO-GelMA, and rGO-GelMA showed ventricular-like, atrial-like, and ventricular/atrial mixed phenotypes, respectively. Also, cardiac tissues produced on CNT-GelMA showed expression levels of maturation markers that were similar to those of native cardiac tissues, as examined by gene expression analyses, and showed increased functionality through integrin-mediated mechanotransduction via YAP/TAZ. (Figure 4D and E) In vivo studies on CNT-based hydrogels for cardiac patch and intramyocardial injection are still insufficient. Most studies have focused on the effects of CNT-based hydrogels on in vitro feasibility, such as cytotoxicity. (Table 1) Particularly, the safety and performance of CNT-based conductive hydrogels in cardiac repair remain unclear. In the future, in-depth studies on CNT-based conductive hydrogels for in vivo cardiac applications and clinical translation are necessary.

Graphene and Its Derivatives

Graphene is a two-dimensional (2D) carbon sheet with a hexagonal aromatic structure composed of sp^2 -hybridized carbon atoms.^{124,125} Graphene displays excellent electrical conductivity and mechanical strength, with a Young's modulus of 1.0 TPa.¹²⁶ Graphene and its derivatives (eg, GO and rGO) have been widely used to produce electrically conductive materials.¹²⁷ Large graphene sheets are usually produced by chemical vapor deposition, which is mostly used in the electronics industry.¹²⁸ For biomedical applications, graphene derivatives are commonly obtained from graphite via exfoliation under strong acidic and oxidizing conditions.¹²⁷ The oxidized product was called GO. However, this oxidative process leads to defects in graphene structures with the formation of oxygenated functional groups (eg, carboxylic, hydroxyl, and epoxy groups) at the edges and planes.¹²⁹ Although GO is well dispersed in aqueous solutions or polar solvents, it has poor electrical conductivity due to the defects in the sp^2 carbons.¹³⁰ The sp^2 -carbons in GO can

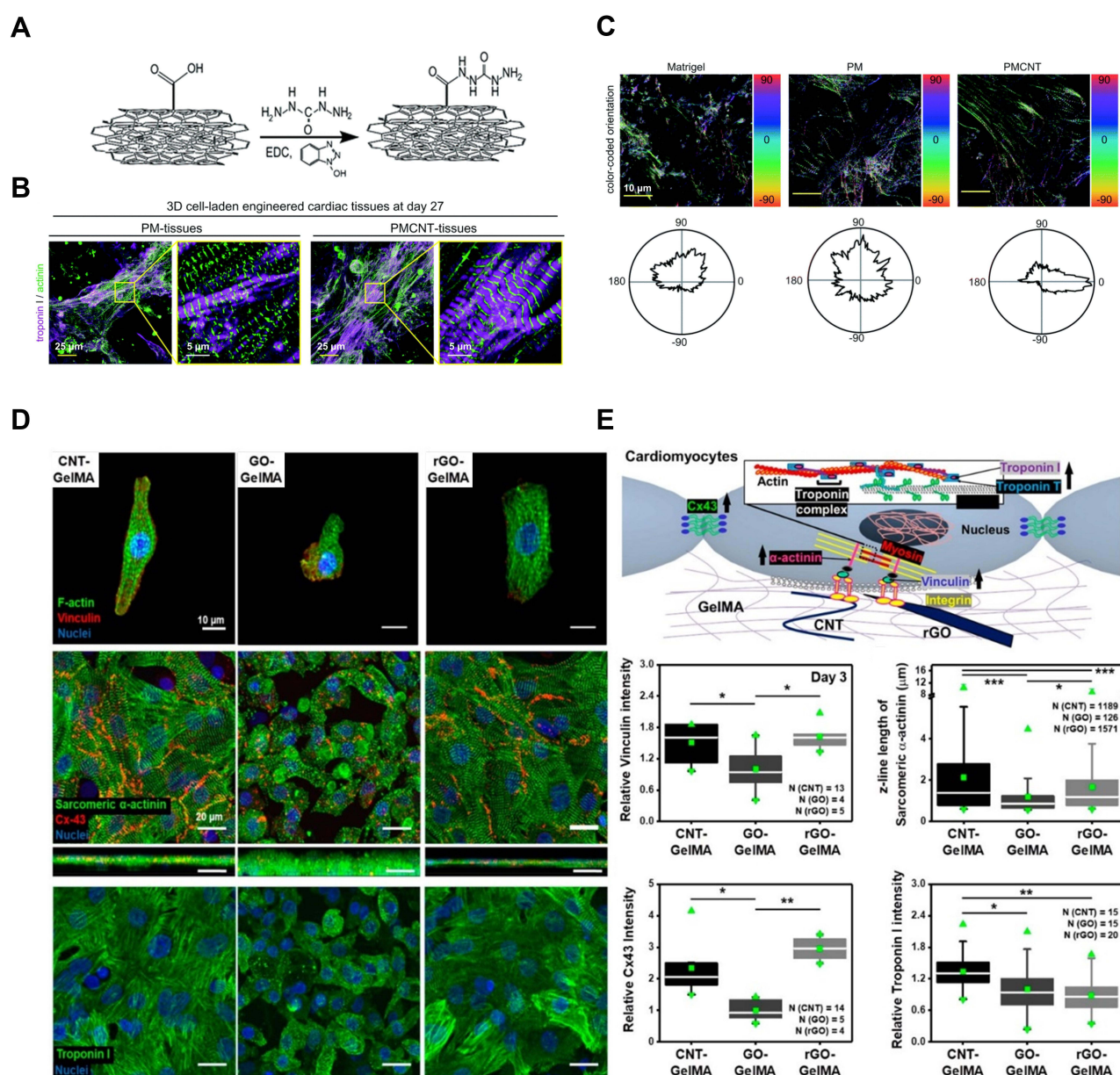


Figure 4 CNT-based hydrogels for cardiac repair. **(A)** Schematic illustration of the synthesis of hydrazide-functionalized MWCNTs. **(B)** Confocal images of hiPSC-derived CM-laden tissue constructs stained for Troponin I and Sarcomeric α -Actinin. hiPSC-derived CMs were cultured pm pericardial tissue (PM-tissues) tissues and conductive hydrogels composed of hydrazide-functionalized CNTs and pericardial matrix (PMCNT-tissues) were cultured for 27 and stained. **(C)** Representative color-coded immunofluorescence images and radar graphs indicating orientation distribution in individual images on day 7. The CMs in the conductive hydrogels showed promoted cellular alignment, Connexin 43 expression, and sarcomere organization. **(D)** Immunostaining of CMs cultured on various carbon nanomaterials-based conductive hydrogels (CNT-, GO-, and rGO-GelMA). CMs cultured on different conductive hydrogels were stained for cardiac specific markers (ie, Vinculin, Sarcomeric α -actinin, Connexin 43 and Troponin (I)) on day 5. **(E)** Schematic illustration of the proteins for CM maturation on the conductive hydrogels. And the relative intensities of the proteins (ie, Vinculin, Sarcomeric α -actinin, Cx43, and Troponin (I)) for CMs cultured on various samples for 5 days (* $P < 0.05$, ** $P < 0.005$, *** $P < 0.005$).

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be partially restored to rGO by various reduction methods (eg, chemical and thermal reduction).^{131,132} The resulting rGO exhibits enhanced electrical conductivity and hydrophobicity. To prepare conductive hydrogels using GO or rGO, it is important to appropriately select the GO or rGO considering both dispersion within hydrophilic polymer chains and electroactivity.

Table 1 Summary of Studies Reviewed That Used CNT-Based Hydrogels for Cardiac Repair

Conductive Component (wt%)	Hydrogel Component	Major Application	Cell Type	Electrical Property (*Difference)	Young's Modulus (kPa) (*Difference)	Improvements	in vitro/ in vivo	Reference
MWCNT (0.01%)	GelMA	Tissue engineering	CM	Contraction rate = $\sim 50 \text{ min}^{-1}$ (~ 2.5 times)	~ 20 (~ 2 times)	Upregulation of junction proteins, maturation, Ca^{2+} transient	in vitro	[122]
MWCNT (2%)	Collagen	Tissue engineering	CM	$ Z = \sim 4 \text{ k}\Omega$ (10 Hz) (~ 1.4 times)	1.9 (23 times)	Synchronization, beating properties	in vitro	[117]
MWCNT (0.5%)	Decellularized pericardial matrix	Tissue engineering	hiPSC-derived CM	$\sigma = 1.46 \text{ S/m}$ (2.2 times)	0.6 (1.7 times)	Maturation, cellular alignment	in vitro	[118]
MWCNT (0.5%)	Synthetic polymer (polyester)	Tissue engineering	CM	$R = 60.9 \text{ k}\Omega$ (1.6 times)	1600 (0.44 times)	Maturation, structural support	in vitro	[172]
MWCNT (0.05%)	GelMA	Tissue engineering, electrical stimulation	EB	$ Z = \sim 20 \text{ k}\Omega$ (1 Hz) (~ 3 times)	30.6 (1.9 times)	Differentiation, beating properties	in vitro	[120]
MWCNT (0.1%)	GelMA	Cardiac patch, tissue engineering	CM	$ Z = \sim 3 \text{ k}\Omega$ (10^3 Hz) (~ 3 times)	~ 25 (~ 2.5 times)	Synchronization, beating properties, cell adhesion, maturation	in vitro	[46]
SWCNT (0.0069%)	Gelatin, chitosan	Cardiac patch, tissue engineering	CM	$\text{CV} = 22.0 \text{ cm/s}$ (4.2 times)	15.1 (1.3 times)	Maturation, synchronization, Conduction velocity	in vitro	[173]
MWCNT (6%)	Collagen, alginate	Cardiac patch, tissue engineering	HCAEC	$ Z = \sim 0.1 \text{ k}\Omega$ (5 Hz) (~ 2.1 times)	~ 1200 (~ 2 times)	Proliferation, migration, differentiation	in vitro	[119]
CNT (Undefined.)	GelMA	Cardiac patch, tissue engineering	hiPSC-derived CM	$R = 6.1 \text{ k}\Omega$ (-)	~ 600 (~ 2 times)	Cardiac function, histological assessment	in vitro/ in vivo	[77]
MWCNT (2%)	GelMA, elastic-MA	Cardiac patch	CM	$ Z = \sim 1 \text{ k}\Omega$ (1 Hz) (~ 11 times)	40 (80% strain) (21 times)	Cardiac function, histological assessment, Ca^{2+} transient, shape-memory	in vitro/ in vivo	[25]
SWCNT (0.026%)	Synthetic polymer (PNIPAAm)	Intramyocardial injection, tissue engineering	BASC	$R = 9.3 \text{ k}\Omega$ (100 times)	-	Cell adhesion, maturation, proliferation, differentiation	in vitro/ in vivo	[52]
MWCNT (Undefined.)	Synthetic polymer (PNIPAAm)	Intramyocardial injection, tissue engineering	CM	$R = 144.3 \text{ k}\Omega$ (1.6 times)	-	Maturation, alignment, Ca^{2+} transient, beating properties	in vitro	[116]

Notes:*Difference according to the presence or absence of conductive component.

Abbreviations: R, resistance; Z, impedance; σ , conductivity; CNT, carbon nanotube; MWCNT, multi-walled CNT; SWCNT, single-walled CNT; GelMA, gelatin methacrylate; CM, cardiomyocyte; hiPSC, human induced pluripotent stem cell; EB, embryoid body; HCAEC, human coronary artery endothelial cell; MA, methacrylate; PNIPAAm, poly(N-isopropylacrylamide); BASC, brown adipose stem cell.

Atomically thin 2D structures of graphene derivatives offer effective interactions with various biomolecules and biopolymers, improving the capacity to load drug molecules and strengthening their mechanical properties.^{133,134} In particular, the hydrogels formulated with graphene derivatives have been shown to be beneficial for drug delivery, tissue engineering, and other biomedical applications.^{50,135,136} The characteristics of graphene-based hydrogels can be further tailored to improve their functions (eg, mechanical, electrical, chemical, and biological) by adjusting the graphene content and/or controlling interactions between the hydrogel network and graphene derivatives. For example, the functionalization of GO (or rGO) and/or the reduction degree of GO substantially influences the uniformity and electroactivity of composite hydrogels, resulting in dramatic changes in the mechanical and electrical characteristics. Hydrogels prepared by blending GO or rGO with pre-gel solution typically increase elastic modulus (1.1~10 times) and electrical conductivity (2.3~1000 times) compared to GO-free pristine gel. (Table 2) In the case of rGO-based hydrogels, hydrophobic rGO readily aggregates in hydrogels, frequently resulting in a low electrical conductance.¹³⁷ Although GO is well mixed with hydrophilic polymers, its intrinsically poor electrical properties hinder the production of conductive hydrogels. To overcome these issues, sequential gelation and mild chemical reduction can be used to produce conductive, uniform hydrogels. For instance, our group previously developed a simple and effective strategy to produce conductive rGO-containing hydrogels; a GO-based hydrogel was first prepared by gelation of a pregel solution containing GO and subsequently reduced.^{43,138} This process substantially increased the electrical conductivity while maintaining the rGO distribution within the matrix without severe aggregation. Various rGO-containing hydrogels could be prepared via subsequent gelation and reduction procedures for muscular and neural tissue engineering.^{43,138,139}

Graphene hydrogels can be fabricated to display mechanical and electrochemical characteristics similar to myocardial tissue; such biomimetic graphene-hydrogels can be utilized as cardiac patches and intramyocardial implants to regenerate an infarcted heart. In addition to electrical properties, other beneficial properties of graphene derivatives, including large surface area and various molecular interactions, have enabled the production of hydrogels presenting various interesting characteristics, such as self-healing, anti-oxidant, and antibacterial effects, and delivery of therapeutic agents, for cardiac repair.^{140–143} By taking these advantages from graphene derivatives, various graphene-based hydrogels have been developed and utilized for cardiac regeneration.^{137,140,144–147} Jing et al prepared chitosan/GO hydrogels and further reduced them using dopamine.¹⁴⁰ The resultant hydrogels (chitosan/rGO/polydopamine (PDA)) showed excellent electrical conductivity (0.122 S/m) and elasticity (0.75 kPa), and promoted the cell viability and proliferation of human embryonic stem cell-derived fibroblasts (HEF1) and CMs. They observed that the spontaneous beating rate was faster in the chitosan/GO/PDA group than that in the control group (GO-free hydrogel), implying the favorable effects of electrical conductance on cardiac functional maturation. Moreover, a micro-patterned graphene-based hydrogel has been created to additionally provide topographical cues.^{138,146} Zhang et al patterned microstructures on gelatin/GO hydrogels using a microcontact printing technique.¹⁴⁶ They found that the patterned gelatin/GO hydrogel significantly promoted the alignment and maturation of CMs. Interestingly, introduction of GO and surface features synergistically enhanced contraction amplitude, synchronization, and cardiac gene expression of CMs.

Graphene derivatives have been frequently functionalized and used for formulating conductive hydrogels.^{142,145} Functionalized graphene derivatives can participate in physical or chemical bonding with the hydrogel network and/or interact with various therapeutic agents. For example, Mousavi et al formulated 3-(2-aminoethyl amino) propyltrimethoxysilane (APTMS)-functionalized rGO with oxidized alginate (OA) and decellularized extracellular matrix (dECM).¹⁴⁵ Amine groups in the rGO formed covalent bonds with the aldehyde group of OA through Schiff-base reaction, which significantly improved the physical and electrochemical properties of the composite hydrogels. The conductivity of the APTMS-rGO/OA/dECM hydrogel was 110 times higher compared to that of the APTMS-free hydrogel control. (Table 2) Functionalized GO in hydrogel can act as a carrier of specific therapeutics for MI treatment. Paul et al produced polyethylenimine (PEI)-functionalized GO/GelMA hydrogels as a gene delivery vehicle for MI treatment.¹⁴² They incorporated DNA-loaded PEI-GO in the low-modulus GelMA hydrogels. Intramyocardial injection of the PEG-GO/DNA/GelMA hydrogel to the peri-infarct regions of the infarcted heart of a rat substantially induced neovascularization, reduced scar area, and improved cardiac functions.

Graphene based-conductive hydrogels have been examined for in vivo intramyocardial injection to the heart post-MI.^{82,83,142,148} Zhu et al fabricated injectable hydrogels composed of GelMA, oxidized dextran, and rGO. Injection of

Table 2 Summary of Studies Reviewed That Used Graphene-Based Hydrogels for Cardiac Repair

Conductive Component (wt%)	Hydrogel Component	Major Application	Cell Type	Electrical Property (*Difference)	Young's Modulus (kPa) (*Difference)	Improvements	In vitro/in vivo	Reference
rGO (0.3%)	GelMA	Tissue engineering	CM	$ Z = \sim 3 \text{ k}\Omega$ (10Hz) (~3 times)	22.6 (11 times)	Maturation, proliferation, viability, synchronization, beating properties	in vitro	[137]
GO (0.015%)	Chitosan	Tissue engineering	H9C2	$\sigma = 1.3 \times 10^{-1} \text{ S/m}$ (82 times)	-	Cell adhesion, upregulation of junction proteins	in vitro	[144]
rGO (0.05%)	Chitosan, PDA	Tissue engineering	HEF1, CM	$\sigma = 1.2 \times 10^{-1} \text{ S/m}$ (2.1 times)	~ 0.8 (2.5 times)	Cell adhesion, proliferation, viability, beating properties, synchronization, self-healing	in vitro	[140]
rGO (0.0025%)	Alginate, dECM	Tissue engineering	HUVEC	$\sigma = 1.9 \times 10^{-2} \text{ S/m}$ (110 times)	38.8 (1.1 times)	Physicochemical, eletrochemical properties	in vitro	[145]
GO (0.025%)	Gelatin	Tissue engineering	CM	-	96.8 (1.8 times)	Maturation, synchronization, beating properties, cardiac gene expression	in vitro	[146]
rGO (0.066%)	GelMA, PDA	Tissue engineering, electrical stimulation	CM	$ Z = \sim 2.5 \text{ k}\Omega$ (10Hz) (~1.4 times)	23.6(2.0 times)	Cell adhesion, maturation, viability, beating properties, Ca^{2+} transient	in vitro	[147]
rGO (0.08%)	Collagen	Cardiac patch	HUVEC, CM.	$\sigma = 1.2 \times 10^{-4} \text{ S/m}$ (-)	1100 (9.2 times)	Antibacterial properties, upregulation of cardiac-related gene	in vitro	[143]
GO (0.05%)	GelMA	Intramyocardial injection, gene delivery	HUVEC, H9C2	-	0.2 (2.5 times)	Cardiac function, histological assessment, neovascularization	in vitro/in vivo	[142]
GO (0.05%)	Synthetic polymer (PEG)	Intramyocardial injection, tissue engineering	ADSC	$\sigma = 0.0284 \text{ S/m}$ (2.3 times)	0.075 (2.3 times)	Cardiac function, histological assessment, neovascularization, differentiation	in vitro/in vivo	[82]
GO (0.1%)	Synthetic polymer (PEG)	Intramyocardial injection	-	$\sigma = 0.424 \text{ S/m}$ (4.7 times)	-	Cardiac function, histological assessment, neovascularization, Ca^{2+} transient	in vitro/in vivo	[148]
rGO (0.05%)	GelMA, ODEX	Intramyocardial injection, tissue engineering	UCMSC	$\sigma = 2.4 \times 10^{-2} \text{ S/m}$ (~1000 times)	~ 200 (~4 times)	Cardiac function, histological assessment, neovascularization, differentiation	in vitro/in vivo	[83]

Notes:*Difference according to the presence or absence of conductive component.

Abbreviations: GO, graphene oxide; rGO, reduced GO; σ , conductivity; Z , impedance; GelMA, gelatin methacrylate; CM, =cardiomyocyte, H9C2=CM cell line; PDA, =polydopamine, HEF1=human embryonic stem cell-derived fibroblasts; dECM, decellularized extracellular matrix; HUVECs, human umbilical vein endothelial cells; PEG, polyethylene glycol; ADSC, adipose-derived stromal cell; ODEX, oxidized dextran; UCMSC, umbilical cord mesenchymal stem cell.

a mixture of the precursor solutions led to spontaneous gelation in the body through Schiff base and UV crosslinking.⁸³ (Figure 5A) They encapsulated umbilical cord mesenchymal stem cells (UCMSCs) with GelMA/oxidized dextran/rGO gels and injected them into infarcted myocardium of a rat. They observed significant improvement of the ejection fraction (EF), reduction of myocardial infarct areas, and enhanced expression levels of cardiac markers (cardiac Troponin I and connexin 43) in the USCMSs with GelMA/oxidized dextran/rGO group compared to the control groups (rGO free hydrogels). (Figure 5B and C) However, studies on graphene-based cardiac patches are few. While graphene-based-hydrogels have been employed,^{137,143} most studies mainly demonstrated the possibility based on in vitro results as proof-of-concept studies, with minimal investigation of therapeutic effectiveness for cardiac treatment in vivo. (Table 2).

MXene

Two-dimensional transition metal carbide/nitride (MXene) has been highlighted as a new 2D nanomaterial since Gogotsi et al proposed it in 2011.¹⁴⁹ MAX is a group of ternary carbides and nitrides in a layered structure, where “M” stands for the early transition metal layer (eg, Ti, Nb, Cr, and Mo), “A” stands for A-group (mostly group IIIA and IVA elements of the periodic table) metal layer, and “X” stands for C or N elements.^{150,151} MXene is prepared by etching an “A” metal layer in the MAX phase.¹⁵² During the etching process, 2D nano-layered MXenes with surface functional groups (eg, –F, –OH, –O, and –Cl) are obtained.¹⁵³ MXene exhibits excellent properties such as metallic conductivity,¹⁵⁴ optical¹⁵⁵ and mechanical¹⁵⁶ properties, hydrophilicity, chemical stability, and large surface area.¹⁵⁷

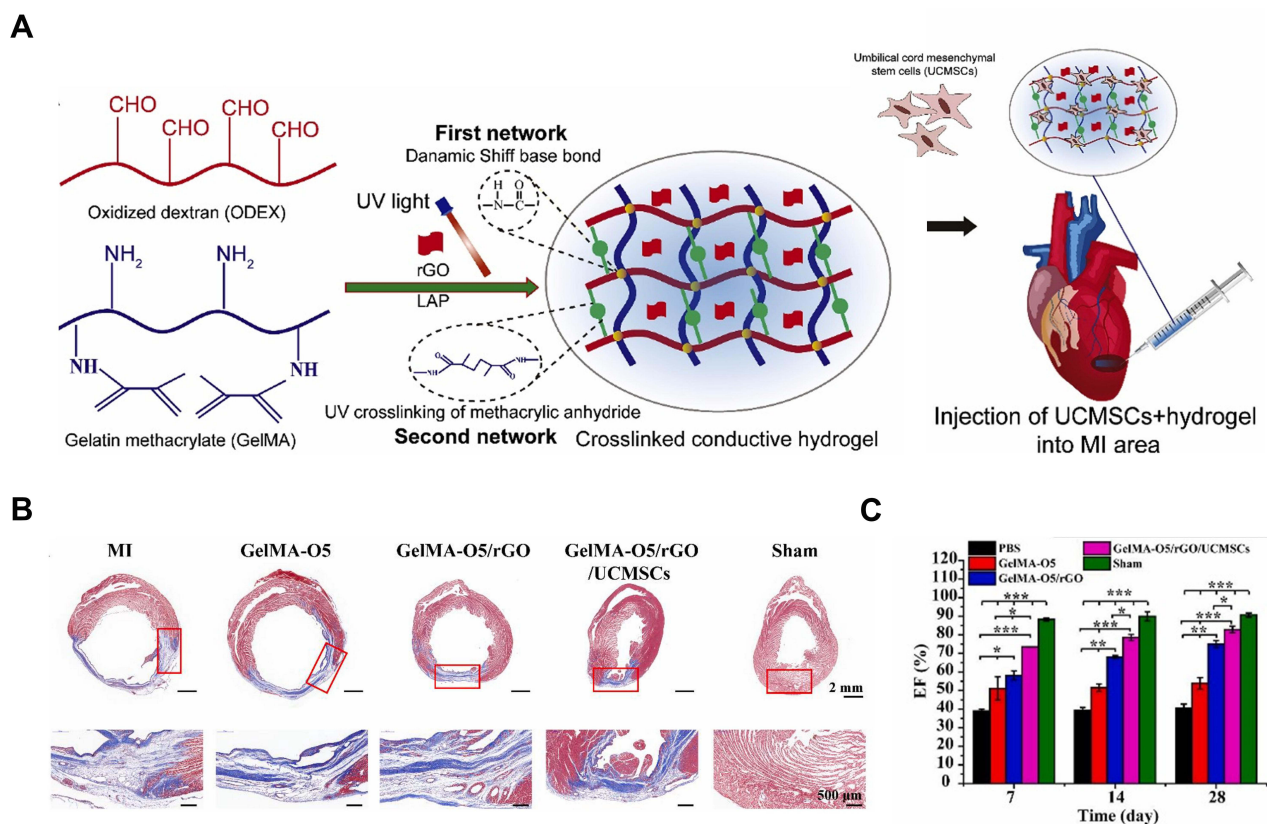


Figure 5 Graphene-based conductive hydrogels for cardiac repair. **(A)** An injectable, conductive hydrogel composed of GelMA, oxidized dextran, and rGO. The gel could be formed through in situ Schiff base and UV crosslinking post injection. UCMSCs were encapsulated in the GelMA/oxidized dextran/rGO gels and injected into MI area. **(B)** Histological micrographs of heart tissues treated with various samples and controls. **(C)** Ejection fraction (EF) of various groups treated with various samples. (*P < 0.05, **P < 0.01, ***P < 0.001).

Notes: Reprinted with permission from Zhu S, Yu C, Liu N et al. Injectable conductive gelatin methacrylate/oxidized dextran hydrogel encapsulating umbilical cord mesenchymal stem cells for myocardial infarction treatment. *Bioact Mater*. 2022;13:119–134.⁸³ © 2021 The Authors. Publishing services by Elsevier B.V. on behalf of KeAi Communications Co. Ltd. Under a Creative Commons Licence.

MXenes and MXene-based materials have been actively studied for biomedical applications such as tissue engineering.¹⁵⁸ MXene has outstanding hydrophilicity, unlike other 1D and 2D nanomaterials, such as CNTs and graphene, and is well dispersed in hydrogels. MXene-based conductive hydrogels show excellent electrical, chemical, and mechanical properties. Hence, MXene-based hydrogels can provide an electrical microenvironment and mechanical support to the myocardium for cardiac tissue regeneration. Basara et al fabricated patterned $\text{Ti}_3\text{C}_2\text{T}_x$ MXene-PEG hydrogels by printing MXene onto PEG hydrogels to mimic the ordered structure of the native ECM and electrical conductivity of the myocardium.⁵¹ CMs cultured on the 3D-printed MXene hydrogels exhibited significantly increased expression of cardiac-related genes (ie, MYH7, SERCA2, and TNNT2) and improved synchronous beating. Ye et al produced a CM-seeded MXene cryogel cardiac patch by formulating PEG, GelMA, and Ti_2C MXene.¹⁵⁹ The MXene-incorporated cryogels exhibited higher mechanical strength compared to MXene-free cryogels. The cryogel with a moderate MXene proportion (0.8%) was found to have mechanical properties and conductivity similar to the natural myocardium. (Table 3) The MXene cryogel showed no cytotoxicity and promoted the functional maturation of CMs, including beating. In vivo transplantation of MI rats revealed that the MXene cryogel cardiac patch significantly suppressed the inflammatory reaction and improved cardiac function. (Figure 6) In addition, Ti_3C_2 MXene quantum dots (MQD) in hydrogels can provide additional functions, such as anti-inflammatory properties and promotion of cellular activity. Rafieerad et al fabricated MQD-containing chitosan hydrogels as injectable shape memory hydrogels for stem cell delivery.¹⁶⁰ They reported that MQD-containing hydrogels are promising for tissue repair and treatment of inflammatory and degenerative diseases, including for cardiac applications.

Although MXene-based hydrogels display excellent physicochemical, conductive, and immunosuppressive properties that are appropriate for cardiac tissue repair, their in vivo and in vitro studies are insufficient compared with carbon nanomaterials (eg, CNTs and graphene). Therefore, the fabrication of various MXene-containing hydrogels and their efficacy tests are of great interest for cardiac repair after MI.

Emerging Nanomaterials

Recently, various inorganic nanomaterials such as black phosphorus (BP) and molybdenum disulfide (MoS_2) have been discovered and studied for biomedical applications.^{63,161–163} These materials have rarely been used for cardiac tissue engineering; however, these new nanomaterials are expected to contribute to the development of new functional biomaterials for cardiac repair, including conductive hydrogels. BP nanosheets are a type of 2D nanomaterial that was discovered in 2014 after graphene.¹⁶⁴ BP nanosheets exhibit several beneficial properties, such as high electrical conductance and mechanical strength, for tissue regeneration, drug delivery, photothermal therapy, and photodynamic therapy.^{163,165–169} Xu et al prepared BP-containing hydrogels as a conductive platform for neural tissue engineering.⁶³ BP-GelMA hydrogel had 4-fold higher conductivity (0.2 S/m) than BP-free GelMA hydrogels. They suggested that

Table 3 Summary of Studies Reviewed That Used MXene Based Hydrogels for Cardiac Repair

Conductive Component (wt %)	Hydrogel Component	Major Application	Cell Type	Electrical Property (*Difference)	Young's Modulus (kPa) (*Difference)	Improvements	in vitro/ in vivo	Reference
Ti_3C_2 deposition (1 μm thick)	Synthetic polymer (PEG)	Cardiac patch, tissue engineering	hiPSC-derived CM	$\sigma = 1.1 \times 10^4 \text{ S/m}$ (1000 times)	17.5 (2.5 times)	Synchronization, maturation, beating properties, Ca^{2+} transient, cardiac gene expression	in vitro	[51]
Ti_2C (0.8%)	GelMA, PEG	Cardiac patch, tissue engineering	CM	$\sigma = 8.7 \times 10^{-2} \text{ S/m}$ (~9 times)	10.1 (~7 times)	Cardiac function, histological assessment, angiogenesis, maturation	in vitro/ in vivo	[159]
Ti_3C_2 QDs (0.00013%)	Chitosan	Tissue engineering	MSC, hiPSC-derived fibroblast	$\sigma = 3.5 \times 10^{-6} \text{ S/m}$ (~4 times)	-	Immunomodulatory properties	in vitro	[160]

Notes: *Difference according to the presence or absence of conductive component.

Abbreviations: σ , conductivity; PEG, polyethylene glycol; hiPSC, human induced pluripotent stem cell; GelMA, gelatin methacrylate; QD, quantum dot; MSC, mesenchymal stem cell.

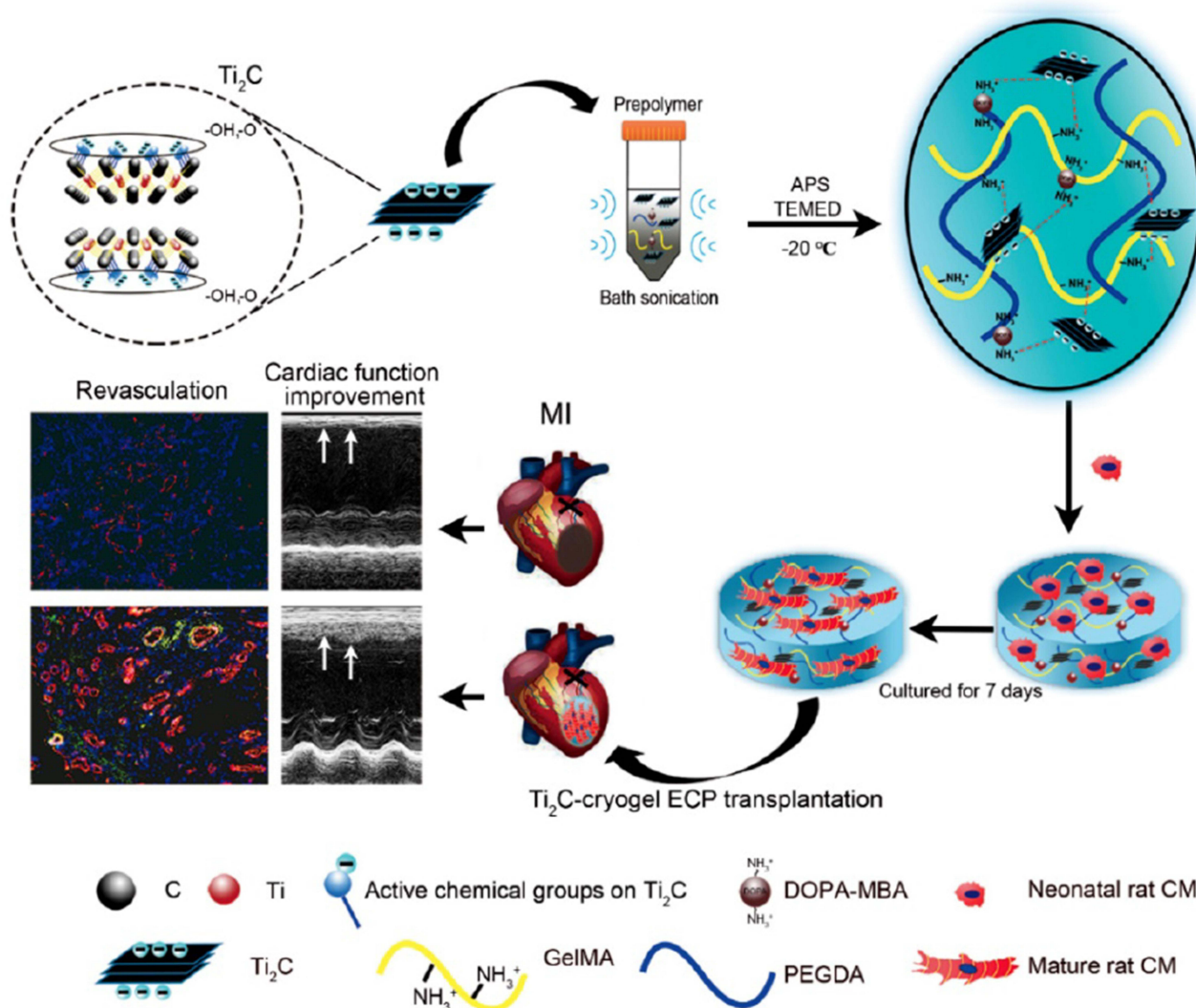


Figure 6 MXene-based hydrogels for cardiac repair. MXene Ti_2C -cryogels were produced as cardiac patches using PEG, GelMA and Ti_2C MXene, seeded with CMs, and implanted on the surface of infarcted heart. These hydrogels improve cardiac functions and revascularization.

Notes: Reprinted with permission from Ye G, Wen Z, Wen F et al. Mussel-inspired conductive Ti_2C -cryogel promotes functional maturation of cardiomyocytes and enhances repair of myocardial infarction. *Theranostics*. 2020;10(5):2047–2066.¹⁵⁹ Copyright © The author(s) Creative Commons Attribution License (<https://creativecommons.org/licenses/by/4.0/>). Ivyspring International Publisher.

conductive BPs within the composite hydrogel may be useful for improving the regeneration of other electroactive tissues, such as cardiac and skeletal muscle tissues, as well as neural tissues. However, studies on BP-based hydrogels for cardiac applications have not yet been reported.

MoS_2 is a new-generation nanosheet with a large surface area, high electrical conductivity, optical properties, and biocompatibility.¹⁷⁰ MoS_2 has been employed in several biomedical applications including photothermal therapy, drug delivery, and biosensors. Several scaffolds with MoS_2 have been studied for bone and neural tissue engineering, as MoS_2 was found to induce osteogenic and neural differentiation of MSCs.^{161,162} Nazari et al fabricated nylon6 electrospun nanofibers incorporated with MoS_2 nanosheets and observed enhanced mechanical properties and electrical conductivity.¹⁷¹ They found that mouse embryonic cardiac cells (mECCs) on the MoS_2 -scaffolds showed improved maturation and upregulation of cardiac functional genes (eg, GATA-4, c-TnT, Nkx 2.5, and α -MHC) compared to those on pristine nylon scaffolds. These MoS_2 -reinforced scaffolds have been suggested as promising materials for cardiac tissue engineering. However, MoS_2 -based hydrogels have not yet been developed for cardiac tissue engineering and

repair. Additional trials and toxicity and performance evaluations are required to use these 2D nanomaterial (BP and MoS₂)-incorporated hydrogels for cardiac repair.

Conclusion

Development of novel functional biomaterials that can facilitate cardiac tissue repair after cardiovascular diseases is highly required due to the lack of current effective treatment. Electrically conductive hydrogels can mimic the characteristics of native cardiac tissues and induce cardiac regeneration by providing mechanical and electrical cues to infarcted heart tissue. Low-dimensional inorganic nanomaterials (CNT, graphene derivatives, and MXenes) have been used to fabricate conductive hydrogels for cardiac applications (injection into the myocardium or pericardial cavity, and attachment on the heart). Conductive hydrogels composed of individual nanomaterials and various polymers exhibit unique characteristics such as excellent electrical conductivity, mechanical strength, and biological activities. Nanomaterial-containing conductive hydrogels have been proven to be promising materials for cardiac tissue repair. The newly discovered 2D nanomaterials (BP and MoS₂) are expected to offer potentials to facilitate the fabrication of functional conductive hydrogels for cardiac repair. Biocompatibility of low-dimensional nanomaterials has not been clearly determined yet although numerous materials containing various nanomaterials have successfully demonstrated their utilities for various biomedical applications. In particular, nanomaterial-based conductive hydrogels for cardiac tissue repair are emerging and even their animal studies are not sufficient for their clinical translation. Overall, future studies on further material engineering, therapeutic efficacy, and biocompatibility of nanomaterial-based conductive hydrogels are necessary. In addition, these conductive hydrogels can be used for the regeneration of other electrically active tissues such as nerves and muscles.

Abbreviations

MI, myocardial infarction; CMs, cardiomyocytes; ECM, extracellular matrix; TA-PEG, tetraaniline-polyethylene glycol; HA-SH, thiolated hyaluronic acid; ADSCs, adipose-derived stem cells; CNT, carbon nanotube; SWCNTs, single-walled CNTs; MWCNTs, multi-walled CNTs; GelMA, gelatin methacrylate; PNIPAAm, poly(N-isopropylacrylamide); BASCs, brown adipose stem cells; hiPSCs, human-induced pluripotent stem cells; HCAECs, human coronary artery endothelial cells; IDs, intercalated discs; GO, graphene oxide; rGO, reduced GO; R, resistance; Z, impedance; σ , conductivity; EB, embryoid body; HEF1, human embryonic stem cell-derived fibroblasts; APTMS, 3-(2-aminoethyl amino) propyltrimethoxysilane; OA, oxidized alginate; dECM, decellularized extracellular matrix; PEI, polyethylenimine; UCMSCs, umbilical cord mesenchymal stem cells; EF, ejection fraction; PDA, polydopamine; ODEX, oxidized dextran; MQDs, MXene quantum dots; BP, black phosphorus; MoS₂, molybdenum disulfide; mECCs, mouse embryonic cardiac cells.

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Disclosure

The authors report no conflicts of interest in this work.

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