

# Porous SiO<sub>2</sub>-Based Reactor with Self-Supply of O<sub>2</sub> and H<sub>2</sub>O<sub>2</sub> for Synergistic Photo-Thermal/Photodynamic Therapy

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**Purpose:** Although the combined photo-thermal (PTT) and photodynamic therapy (PDT) of tumors have demonstrated promise as effective cancer therapy, the hypoxic and insufficient H<sub>2</sub>O<sub>2</sub> supply of tumors seriously limits the efficacy of PDT, and the acidic environment reduces the catalytic activity of nanomaterial in the tumor microenvironment. To develop a platform for efficiently addressing these challenges, we constructed a nanomaterial of Aptamer@dox/GOD-MnO<sub>2</sub>-SiO<sub>2</sub>@HGNs-Fc@Ce6 (AMS) for combination tumor therapy. The treatment effects of AMS were evaluated both in vitro and in vivo.

**Methods:** In this work, Ce6 and hemin were loaded on graphene (GO) through  $\pi$ - $\pi$  conjugation, and Fc was connected to GO via amide bond. The HGNs-Fc@Ce6 was loaded into SiO<sub>2</sub>, and coated with dopamine. Then, MnO<sub>2</sub> was modified on the SiO<sub>2</sub>. Finally, AS1411-aptamer@dox and GOD were fixed to gain AMS. We characterized the morphology, size, and zeta potential of AMS. The oxygen and reactive oxygen species (ROS) production properties of AMS were analyzed. The cytotoxicity of AMS was detected by MTT and calcein-AM/PI assays. The apoptosis of AMS to a tumor cell was estimated with a JC-1 probe, and the ROS level was detected with a 2',7'-Dichlorodihydrofluorescein diacetate (DCFH-DA) probe. The anticancer efficacy in vivo was analyzed by the changes in the tumor size in different treatment groups.

**Results:** AMS was targeted to the tumor cell and released doxorubicin. It decomposed glucose to produce H<sub>2</sub>O<sub>2</sub> in the GOD-mediated reaction. The generated sufficient H<sub>2</sub>O<sub>2</sub> was catalyzed by MnO<sub>2</sub> and HGNs-Fc@Ce6 to produce O<sub>2</sub> and free radicals ( $\bullet$ OH), respectively. The increased oxygen content improved the hypoxic environment of the tumor and effectively reduced the resistance to PDT. The generated  $\bullet$ OH enhanced the ROS treatment. Moreover, AMS depicted a good photo-thermal effect.

**Conclusion:** The results revealed that AMS had an excellent enhanced therapy effect by combining synergistic PTT and PDT.

**Keywords:** nanomaterial, photo-thermal therapy, photodynamic therapy, hypoxia

## Introduction

Reactive oxygen species (ROS) is an important intracellular signaling molecule in biological processes.<sup>1</sup> At normal concentrations, ROS can regulate cell growth, apoptosis, and differentiation; it also participates in proliferation, DNA damage, and other living activities. However, congestion of the plethora of ROS can lead to oxidative damage and, ultimately, apoptosis.<sup>2</sup> Breaking the ROS content threshold to trigger tumor apoptosis has attracted extensive interest in tumor therapy.<sup>3-5</sup>

ROS-based methods have demonstrated considerable potential in cancer therapeutics.<sup>6-8</sup> Photodynamic therapy (PDT), which uses photosensitizers to generate ROS by laser activation, is generally regarded as a scheme for ROS-based tumor therapeutics.<sup>9-11</sup> However, the hypoxic nature of tumor tissue is very harmful to a photosensitizer, which

requires oxygen molecules to exert cytotoxicity. In addition, the consumption of  $O_2$  by the photosensitizer will increase the tumor site hypoxia in the PDT process, resulting in a weakening effect of PDT for cancer treatment.<sup>12–15</sup> Many programs have been developed to ameliorate the hypoxic condition to improve the therapeutic effect.<sup>16–20</sup> Using nanomaterials as catalysts to improve the oxygen concentration of tumor sites has attracted increasing interest.<sup>21–23</sup>

Some treatment methods, such as PTT, PDT, and CDT, have been combined to further improve anti-tumor efficiency.<sup>24–26</sup> Doxorubicin (dox), which can embed into DNA to inhibit the synthesis of nucleic acids, has been widely used as an anti-tumor antibiotic. Under aerobic conditions, dox can activate nicotinamide adenine dinucleotide phosphate (NADPH) oxidase to trigger and generate superoxide radicals ( $O_2^{\bullet-}$ ) in the reaction. The produced  $O_2^{\bullet-}$  can oxidize the damaged cell components to induce cancer cell death.<sup>27,28</sup> However, the hypoxic condition of the tumor tissue reduces the therapeutic effect of dox. Therefore, alleviating the hypoxic environment can increase the sensitivity of tumor cells to dox and improve the anti-tumor efficacy of CDT.<sup>29–32</sup>

Nanozymes have recently been developed for novel photo-thermal and photodynamic tumor therapy. Compared with natural enzymes, nanozymes have the advantages of tunable size and high stability in harsh environments and can produce cascading catalytic effects in tumor treatment. In the nanoenzyme mediated reaction, the abundant of  $H_2O_2$  can be catalyzed to generate the highly oxidizing  $\bullet OH$  radicals by the nanozyme, which can cause efficient chemotherapy effects on tumor cells. Wang have constructed an amorphous  $NiB@IrOx$  nanozymes that possess a high therapeutic efficiency via catalyze  $H_2O_2$  to  $\bullet OH$  and  $O_2$ .<sup>33</sup> Xu have developed a hollow silica nanozymes for robust oxidative phosphorylation, which possess treatment effect significantly through dual enzyme-like activities.<sup>34</sup> Liu constructed the nanomaterial of SS-DMONS/DOX-Ce6@MIPs, which possess an excellent tumor targeting and dual responsive drug release.<sup>35</sup> Zhang constructed a reactor that  $SiO_2$  encapsulated upconversion material for photo-thermal photodynamic therapy of tumor.<sup>36</sup>

Herein, we fabricated a hollow mesoporous silica-based nanoplatfrom that possessed excellent photo-thermal and photodynamic treatment (Scheme 1). In the nanomaterial, HGNs-Fc@Ce6 was encapsulated in the mesoporous  $SiO_2$ , PDA and  $MnO_2$  were immobilized on the surface of  $SiO_2$ , and doxorubicin-loaded AS1411-aptamer and GOD were modified via the amide bond between the amino of dopamine and the carboxyl of GOD and aptamer. The Aptamer@dox/GOD- $MnO_2$ - $SiO_2$ @HGNs-Fc@Ce6 (AMS) degraded glucose into  $H_2O_2$  through the GOD-mediated process in the tumor microenvironment, and the generated  $H_2O_2$  was decomposed into oxygen ( $O_2$ ) by  $MnO_2$ . Meanwhile, AMS could be used to generate  $^1O_2$  by Ce6 under the 660 nm laser irradiation, which can efficiently kill tumor cells. The generated  $O_2$  could overcome tumor hypoxia and enhance PDT. The PDA was cracked in the acidic environment, and the released HGNs-Fc@Ce6 catalyzed  $H_2O_2$  to generate ROS to kill tumor cells. Moreover, AMS exhibited good photo-thermal and photodynamic effects under laser irradiation.

## Materials and Methods

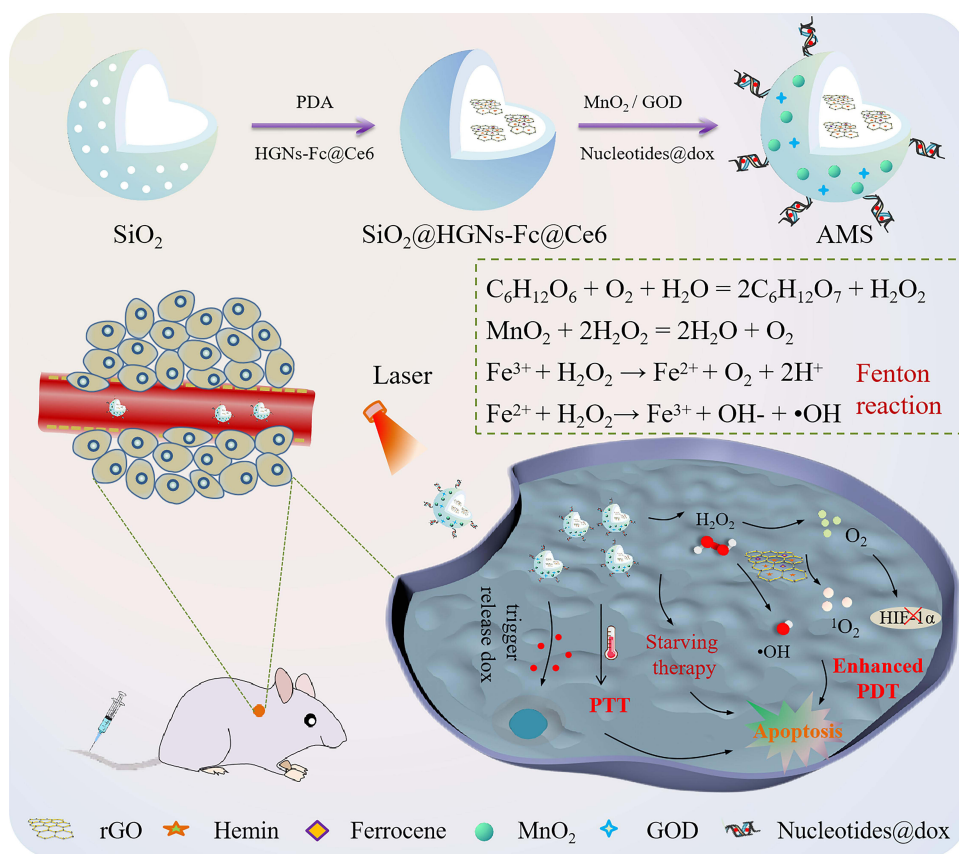
### Materials

Chlorine e6 (Ce6), glucose oxidase (GOD), Hemin, 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT), 2',7'-dichlorofluorescein diacetate (DCFH-DA), JC-1 reagent test kit, propidium iodide (PI), and 1, 3-diphenylisobenzofuran (DPBF) were purchased from Sigma-Aldrich. Graphene oxide (GO) was obtained from Xianfeng Nano Materials Tech Co. Ltd. (Nanjing, China). The nucleic acid sequence was obtained from Takara Biomedical Technology Co., Ltd. (Beijing, China). Human hepatocarcinoma cell lines (HepG2) and human normal liver cells (7702) were purchased from the Chinese Academy of Medical Sciences (Beijing, China).

### Preparation of AMS

#### Preparation of $SiO_2$

First, 3 mL of ethyl orthosilicate (TEOS) was added to the ethanol (36 mL) and ammonia (1.60 mL) solution and stirred at 30 °C for 50 min. Then, a mixture of TEOS (2.5 mL) and perfluorodecane (CF, 1.0 mL) was added drop-wise into the above solution, and it was further continuously stirred for 80 min in a 30 °C water bath. The pellet was obtained via centrifugation (10,000 rpm, 10 min). The precipitate was placed in a  $Na_2CO_3$  solution (50 mL, 0.6 M) and etched at 80 °C for 10–20 min. The mixed solution was centrifuged (8000 rpm for 10 min) and washed with  $H_2O$  to obtain the hollow mesoporous  $SiO_2$ .



**Scheme 1** Schematic illustrations for the fabrication of AMS and synergistic anti-tumor effect.

### Preparation of HGNs-Fc@Ce6

Hydrazine (80%, 5  $\mu\text{L}$ ) and hemin (2 mg) were added to 1 mL of graphene oxide (10 nm, GO) solution (1 mg/mL) and incubated for 4 h in the water bath at 60  $^{\circ}\text{C}$ . The hemin was loaded onto the GO via  $\pi$ - $\pi$  conjugated covalent bond. The mixed solution was centrifuged to remove the supernatant; thus, the HGNs were obtained. A mixture of 0.1 mg of chitosan (CS, CAS: 9012-76-4, 10-50kDa), 1 mL of HGNs (1 mg/mL), 50-mM EDC, and NHS was stirred for 2 h. The solution was centrifuged to gain precipitates, and then 0.2 mg of ferrocene, 100  $\mu\text{L}$  of 50-mM EDC, and NHS were added to the above re-dispersed solution while stirring for another 2 h. The supernatant was removed from the mixed solution and re-dispersed to form a 1-mg/mL HGNs-Fc solution. The HGNs-Fc was synthesized via the dehydration condensation reaction, that the amino group of CS is connected with the carboxyl group of HGNs and Fc through the chemical bond of amide bond.<sup>37</sup>

Next, 0.5 mg of Ce6 was dissolved in 2 mL of dimethyl sulfoxide (DMSO) and added to the HGNs-Fc solution (1 mg/mL, 2 mL). The mixed solution was stirred for 12 h and centrifuged to remove the excess Ce6.

### Preparation of $\text{MnO}_2$ - $\text{SiO}_2$ @HGNs-Fc@Ce6

The HGNs-Fc@Ce6 solution (2.0 mg/mL, 5 mL) was injected into the  $\text{SiO}_2$  dispersion (1.0 mg/mL, 5 mL) and stirred for 24 h. The solution was centrifuged and washed to gain  $\text{SiO}_2$ @HGNs-Fc@Ce6. A mixture of 5 mL of  $\text{SiO}_2$ @HGNs-Fc@Ce6 (1.0 mg/mL) and 3 mL of dopamine (1.0 mg/mL) was stirred for 12 h. The mixture was centrifuged to gain the precipitates, and then, 1.5 mL of potassium permanganate ( $\text{KMnO}_4$ , 0.1 mg/mL) was added to the above re-dispersed solution, stirring for 1 h. Next, ascorbic acid (0.5 mM) was added dropwise into the above solution to reduce  $\text{KMnO}_4$  to manganese dioxide ( $\text{MnO}_2$ ). This reaction was manipulated until the color of the solution changed from dark red to brownish black. The mixed solution was centrifuged to remove the supernatant and obtain  $\text{MnO}_2$ - $\text{SiO}_2$ @HGNs-Fc@Ce6.

## Preparation of AMS

Next, 500  $\mu\text{L}$  of FITC-labeled AS1411-aptamer@dox (100 nM), GOD (0.5 mg/mL, 1 mL), 100  $\mu\text{L}$  of EDC, and NHS aqueous (50 mM, 4:1) were added to the above  $\text{MnO}_2\text{-SiO}_2\text{@HGNS-Fc@Ce6}$  solution. The mixed aqueous solution was stirred for 12 h and centrifuged at 10,000 rpm for 20 min to obtain AMS.

Sequences of the FITC-AS1411-aptamer: 5'-FITC-GGT GGT GGT GGT TGT GGT GGT GGT GG NNNNN NNNNNNNNNNNNTTTTTTTT-SH-3' (The AS1411-aptamer sequences in the oligonucleotides are underlined.).

Complementary strand: 5'-NNNNNNNNNNNTTTTTTTT ACA ACC ACC ACC ACC-1-3'.

## Oxygen Generation

Next, 100  $\mu\text{L}$  of  $\text{H}_2\text{O}_2$  (150  $\mu\text{M}$ ) or a glucose solution (150  $\mu\text{M}$ ) was added to AMS solutions of different concentrations (10, 20, 30, 60, and 90  $\mu\text{g/mL}$ ) without oxygen, and then, the dissolved  $\text{O}_2$  concentration was measured with an oxygen meter.

## Measurement of Singlet Oxygen ( $^1\text{O}_2$ )

DPBF was used to measure  $^1\text{O}_2$  production by AMS in the absence or presence of the  $\text{H}_2\text{O}_2$  solution under 660-nm laser irradiation. First, 100  $\mu\text{L}$  of  $\text{H}_2\text{O}_2$  (5 mM) and 50  $\mu\text{L}$  of DPBF (1 mg/mL, dissolved in DMSO) were added to 3 mL of the AMS (100  $\mu\text{g/mL}$ , pH = 5.5) solution. Similarly, 100  $\mu\text{L}$  of glucose (5 mM) and 50  $\mu\text{L}$  of DPBF (1 mg/mL, dissolved in DMSO) were added to 3 mL of the AMS (100  $\mu\text{g/mL}$ , pH = 5.5) solution. The generated  $^1\text{O}_2$  of AMS was evaluated by the UV-visible absorption of DPBF under 660-nm laser irradiation (0.2  $\text{W cm}^{-2}$ ).

## Measurement of $\bullet\text{OH}$

A TMB coloration assay was used to measure the produced  $\bullet\text{OH}$ . First, 100  $\mu\text{g/mL}$  of  $\text{H}_2\text{O}_2$  (10 mM) and the glucose solution (20 mM) were injected into the AMS solution (100  $\mu\text{g/mL}$ , pH = 5.5) and 0.5 mg/mL of TMB, respectively. The absorbance peak at 652 nm was recorded with a microplate reader.

Electron spin resonance (ESR) was used for the measurement of  $\bullet\text{OH}$ . First, 100  $\mu\text{L}$  of  $\text{H}_2\text{O}_2$  (5 mM) was added to the AMS solution (100  $\mu\text{g/mL}$ , pH = 5.5), including the capture agent of DMPO. An ESR signal was detected at a different time by a Bruker EMX1598 spectrometer.

## Photo-Thermal Performance

To analyze the photo-thermal effect, AMS solutions with a range of concentrations (0, 50, 100, 200, and 300  $\mu\text{g/mL}$ ) were irradiated with an 808-nm laser at a power density of 1.6  $\text{W/cm}^2$  for 10 min. Different power densities of the 808-nm laser (0.4, 0.8, 1.2, 1.6, and 2.0  $\text{W/cm}^2$ ) were also used to evaluate the thermal effect of the AMS solution (100  $\mu\text{g/mL}$ ). In addition, the photo-thermal efficiency of AMS was monitored by repeated on/off under the irradiation of an 808-nm laser.

## Cell Culture

HepG2 cells (human hepatoma cells) and 7702 cells (human liver cells) were purchased from the Chinese Academy of Sciences. The cell lines were cultured in a DMEM medium (Gibco, USA) containing 10% fetal bovine serum (FBS, Gibco, USA) at 37 °C and 5%  $\text{CO}_2$  cell incubator.

## Targeted Analysis of AMS

The HepG2 cells ( $1 \times 10^5$  cells) were incubated in a confocal dish at 37 °C, 5%  $\text{CO}_2$  for 24 h. Then, they were treated with AMS (100  $\mu\text{g/mL}$ ) for 30 min. The dish was washed with PBS (0.01 M) and imaged with a confocal laser scanning microscope (CLSM).

## In vitro Reactive Oxygen Species (ROS) Production

A DCFH-DA probe was used to measure intracellular ROS. The HepG2 cells ( $10^5$  cells per dish) were co-incubated with the AMS solution (100  $\mu\text{g/mL}$ ) for 30 min in a dish. Then, the DMEM containing DCFH-DA (1  $\mu\text{M}$ ) was added, and the



sample was incubated for 30 min. Subsequently, the HepG2 cells were treated with laser (660 nm,  $0.2 \text{ W cm}^{-2}$ ) and imaged with CLSM.

## In vitro Toxicity Assessment of AMS

The HepG2 and 7702 cells (8000 cells per well) were incubated in 96-well plates for 24 h and processed with a series of therapeutic regimens. First, 10  $\mu\text{L}$  of CCK-8 (5 mg/mL) was added to the plates, and they were further incubated for 4 h. The toxicity was evaluated with a microplate reader. (Therapeutic regimen: control: cells handled by PBS or laser irradiation;  $\text{SiO}_2$ : cells treated with  $\text{SiO}_2$ ; HGNS-Fc@Ce6: cells treated with HGNS-Fc@Ce6; AMS: cells treated with AMS; AMS + 660 L: cells were irradiated with the 660-nm laser ( $0.2 \text{ W cm}^{-2}$ ) after treatment with AMS; AG NPs + 808 L: cells were irradiated with the 808-nm laser ( $1.6 \text{ W cm}^{-2}$ ) after treatment with AMS; AMS + 660 nm + 808 nm L: cells were irradiated with the 660-nm laser ( $0.2 \text{ W cm}^{-2}$ ) and the 808-nm laser ( $1.6 \text{ W cm}^{-2}$ ) after treatment with AMS). Similarly, different concentrations of  $\text{SiO}_2$ , HGNS-Fc@Ce6, and AMS were used for detecting cell toxicity under laser irradiation.

The calcein-AM and PI dye was used to assess and analyze the live/dead cells. HepG2 cells ( $1 \times 10^5$  cells per dish) were incubated in a confocal dish for 24 h. Then, the cells were treated with the above mentioned treatment prescription. Subsequently, the culture medium containing calcein-AM (10  $\mu\text{g/mL}$ ) and PI (5  $\mu\text{g/mL}$ ) was injected into the dish and cultured for 20 min. The dish was washed with PBS (0.01 mM) and imaged with CLSM.

The JC-1 probe was used as a detection indicator in the early apoptosis of tumor cells. HepG2 cells ( $10^5$  cells per well) were incubated in a confocal dish and handled with PBS,  $\text{SiO}_2$  (100  $\mu\text{g/mL}$ ), HGNS-Fc@Ce6 (100  $\mu\text{g/mL}$ ), AMS (100  $\mu\text{g/mL}$ ), AMS (100  $\mu\text{g/mL}$ ) with the 660-nm laser ( $0.2 \text{ W cm}^{-2}$ ), AMS (100  $\mu\text{g/mL}$ ) with the 808-nm laser ( $1.6 \text{ W cm}^{-2}$ ), and AMS (100  $\mu\text{g/mL}$ ) with the 660-nm laser ( $0.2 \text{ W cm}^{-2}$ ) and the 808-nm laser ( $1.6 \text{ W cm}^{-2}$ ). Then, a JC-1 solution ( $1 \times$ , 1 mL) was added to the above mentioned eight dishes and incubated at  $4^\circ\text{C}$  for 20 min. The dishes were washed with the JC-1 buffer and imaged with CLSM.

## Construction of Tumor-Bearing Mouse Model

Nude mice (4–6 weeks old, an equal number of males and females) were obtained from Guangxi Medical University. All the animal experiments were performed under protocols approved by the Animal Care and Use Committee. Furthermore, 100  $\mu\text{L}$  of PBS containing HepG2 cells ( $1 \times 10^6$ ) was subcutaneously seeded on the backs of the nude mice to develop a hepatic carcinoma tumor model.

## In vivo Fluorescence Imaging

Fluorescence imaging was conducted using an MSOT scanner in a small-animal imaging system. First, 200  $\mu\text{L}$  of an AMS solution (100  $\mu\text{g/mL}$ ) was injected into the mice via the tail vein (anesthetized with 3% isoflurane). The fluorescence signal of AMS in the tumor-bearing mice was recorded at different time points (0, 1, 4, 8, 12, 24, and 48-h post-injection). Next, 200  $\mu\text{L}$  of random sequence modified-GOD-MnO<sub>2</sub>-SiO<sub>2</sub>@HGNS-Fc@Ce6 (RMS) (100  $\mu\text{g/mL}$ ) was injected into mice via the tail vein to record the fluorescence signal, which acted as the control signal.

## In vivo Anti-Tumor Effect

The tumor-bearing mice were randomly divided into six groups ( $n = 6$ ) as follows: (a) PBS, (b) laser irradiation, (c) AMS, (d) AMS + 660 nm laser, (e) AMS + 808 nm laser, (f) AMS + 660 nm + 808 nm laser. The prepared AMS (100  $\mu\text{g/mL}$ ) was injected into the mice via the tail vein. After 4 h, the 660-nm laser ( $0.2 \text{ W cm}^{-2}$ , 5 min) or the 808-nm laser ( $1.6 \text{ W cm}^{-2}$ , 5 min) was used to irradiate the tumor site of the mice. The tumor volumes and body weights were measured every two days. After treatment, the tumors of tumor-bearing mice were dissected and used for a hematoxylin and eosin (HE) staining assay and Ki-67.

## Statistical Analysis

The results were presented as mean  $\pm$  standard deviation. Furthermore, *t*-tests were used to analyze the comparison between different groups.  $*p < 0.05$ ,  $**p < 0.01$ , and  $***p < 0.001$  were regarded as statistically significant.

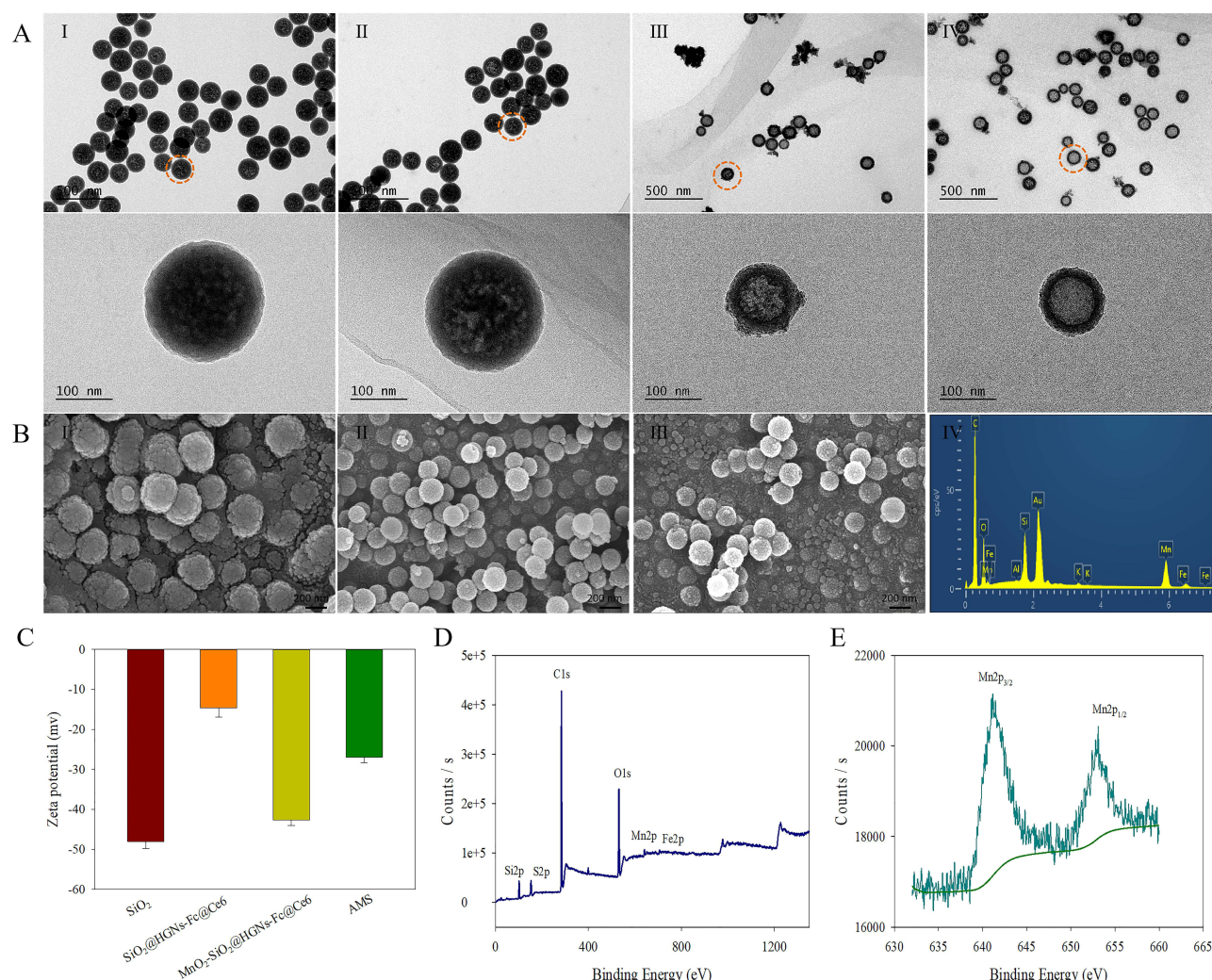
## Results and Discussion

### Preparation and Characterization

The HGNs-Fc was synthesized via the amide bond between the amino of CS and the carboxyl of HGNs and Fc.<sup>37</sup> The thickness and the average size were approximately 21 nm and 18 nm, respectively ([Figures S1 and S2, Supporting Information](#)). In the FT-IR spectrum of HGNs-Fc, 943  $\text{cm}^{-1}$  is a characteristic peak of the Fc ring vibration, and the peaks at 1236 and 1452  $\text{cm}^{-1}$  represent the C-O and N-H vibrations. The peak at 1710  $\text{cm}^{-1}$  was the characteristic absorption peak of the amide bond (CO-NH) ([Figure S3, Supporting Information](#)). In the UV-vis spectrum of HGNs-Fc, the peak at 221 nm was ascribed to the  $\pi$ - $\pi$  transitions of aromatic C=C bonds, and the peaks at 274 and 320 nm were the characteristic peaks of Fc ([Figure S4, Supporting Information](#)). Similarly, the Raman spectra of both GO and HGNs-Fc had two characteristic bands at 1353  $\text{cm}^{-1}$  (D band) and 1596  $\text{cm}^{-1}$  (G band), respectively ([Figure S5, Supporting Information](#)). The HGNs-Fc nanozymes exhibited excellent catalase activities, which could generate  $\bullet\text{OH}$  for the ROS therapy through the Fenton reaction. 3, 3', 5, 5'-Tetramethylbenzidine (TMB) was used to evaluate the catalytic performance of HGNs-Fc, which could be oxidized into blue oxidized TMB (oxTMB) in the presence of the peroxidase-like activity of the materials and the  $\text{H}_2\text{O}_2$  solution. A variation of the TMB absorption value with time was detected in a solution of 2 mL of HGNs-Fc (100  $\mu\text{g/mL}$ ) containing 10.0-mM  $\text{H}_2\text{O}_2$  and 0.5-mM TMB. The TMB absorption of HGNs-Fc reached the maximum value at 3 min and then gradually decreased, indicating that the HGNs-Fc had an efficient catalytic effect on  $\text{H}_2\text{O}_2$  ([Figure S6, Supporting Information](#)). After the modification of Ce6 on the HGNs-Fc by the  $\pi$ - $\pi$  stacking interaction, the catalytic performance remained almost unchanged ([Figure S7, Supporting Information](#)). Subsequently, HGNs-Fc@Ce6 was encapsulated in  $\text{SiO}_2$ , and then, PDA and  $\text{MnO}_2$  were covered on the surface of  $\text{SiO}_2$  @HGNs-Fc@Ce6 in turn. The concentration of doxorubicin loaded in the aptamer was optimized, and the characteristic absorption peak reached the maximum at the concentration of 14 mg ([Figure S8, Supporting Information](#)). Finally, AS1411-aptamer@dox and GOD were co-modified on  $\text{MnO}_2$ - $\text{SiO}_2$ @ HGNs-Fc@Ce6, and the final product was obtained. As displayed in [Figure 1A and B](#), the TEM images of  $\text{SiO}_2$  exhibited spherical morphology and a hollow structure. The size was approximately 160 nm, and the zeta potential was -47.5 mV. The pore size of  $\text{SiO}_2$  measured by BET reached 29.4 nm. When the HGNs-Fc@Ce6 and PDA were modified in the  $\text{SiO}_2$ , the morphological structure of the material did not change, and the zeta potential value was -15.2 mV. After  $\text{KMnO}_4$  was reduced by ascorbic acid, a layer of  $\text{MnO}_2$  particles could be observed around the  $\text{SiO}_2$  surface. The particle size was then 130 nm, and the zeta potential became -44.2 mV. To increase the biocompatibility and multiple functions of  $\text{SiO}_2$ , AS1411-aptamer@dox and GOD were coated on the surface of  $\text{SiO}_2$ . The particle size of the prepared AMS remained at approximately 140 nm, which was attributed to the fact that both the oligonucleotides and the enzymes were small molecules. The SEM images of the modified  $\text{SiO}_2$  demonstrated a spherical morphology, and the particle size was consistent with that obtained using TEM. The energy spectrum was also detected to analyze the elemental composition of AMS, and the representative elements of C, O, Fe, Mn, Si, and P could be observed, as illustrated in [Figure 1C](#). The zeta potential value increased to -27.6 mV ([Figure 1C](#)). The elements Fe, Mn, Si, and S co-existed in the XPS spectra, indicating that AMS was successfully synthesized ([Figure 1D](#)). The  $\text{Mn}^{2+}$  peaks (644.4 eV) in Mn (2p) further indicated that  $\text{Mn}^{2+}$  was modified in the AMS, as displayed in [Figure 1E](#) of XPS Mn (2p). The infrared spectrum also provided evidence of the synthesis of AMS ([Figure S9, Supporting Information](#)). In addition, the hydrodynamic size of AMS was detected by dynamic light scattering (DLS) in PBS or the cell culture medium within seven days, which indicated that the AMS had good dispersion and stability ([Figure S10, Supporting Information](#)).

### Detection of Produced Oxygen

To analyze the oxygen production capacity of AMS, the oxygen content was monitored after the injection of AMS solutions of different concentrations into  $\text{H}_2\text{O}_2$  or glucose solution. Negligible oxygen content was detected in PBS. However, the oxygen generation increased with an increase in the concentration of AMS in the  $\text{H}_2\text{O}_2$  or glucose solution ([Figure 2A and B](#)), demonstrating that AMS could efficiently catalyze glucose to  $\text{H}_2\text{O}_2$  and that the generated  $\text{H}_2\text{O}_2$  could be oxidized to produce  $\text{O}_2$  by  $\text{MnO}_2$ . The photographs of the addition of AMS solutions of different concentrations to the  $\text{H}_2\text{O}_2$  or glucose solution are illustrated in [Figures S11 and S12](#). The higher concentrations of AMS produced more



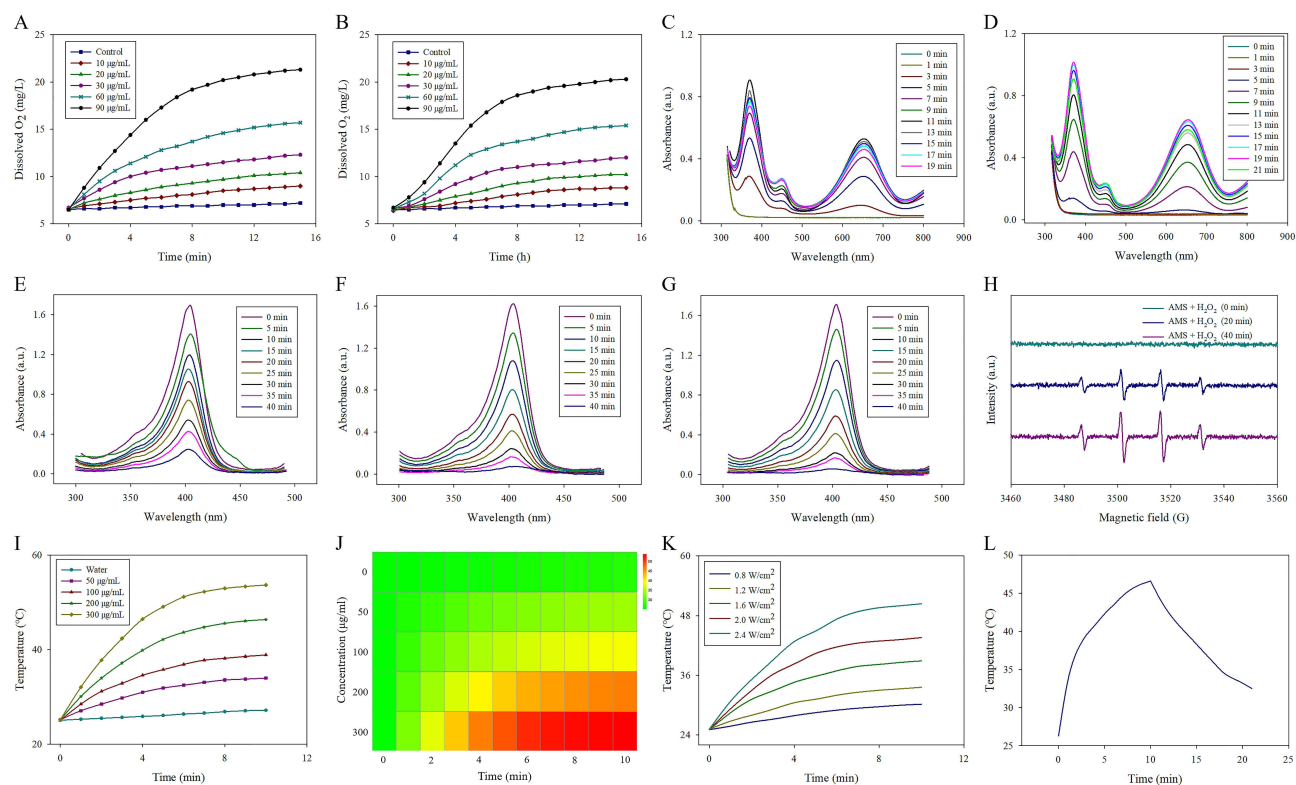
**Figure 1** Characterization of AMS. (A) TEM images of SiO<sub>2</sub> (I), SiO<sub>2</sub>@HGNs-Fc@Ce6 (II), MnO<sub>2</sub>-SiO<sub>2</sub>@HGNs-Fc@Ce6 (III), AMS (IV), respectively. Scale bar: 500 nm. The corresponding enlarged view of the above of TEM images. Scale bar: 100 nm. (B) SEM images of SiO<sub>2</sub> (I), MnO<sub>2</sub>-SiO<sub>2</sub>@HGNs-Fc@Ce6 (II), AMS (III), and energy dispersive spectroscopy (EDS) of AMS (IV), respectively. Scale bar: 200 nm. (C) Zeta potentials of the different modified SiO<sub>2</sub>. (D) XPS spectrum of AMS. (E) XPS spectrum of Mn 2p.

bubbles. The results revealed that AMS could consume glucose in the tumor microenvironment and “starved” the tumor cells. Simultaneously, the produced O<sub>2</sub> could overcome the hypoxic environment of tumors, synergistically improving and enhancing the effect of the tumor treatment.

## Catalytic Performance of AMS

TMB was applied to measure the peroxidase-like activity of AMS. The absorption peaks at 652 nm were observed when 10-mM H<sub>2</sub>O<sub>2</sub> and 0.5-mM TMB were added to the AMS (100 µg/mL, pH = 5.5) solution, in which the chitosan of AMS degraded in the acidic environment and released the HGNs-Fc catalyzed to produce •OH to oxidize TMB (Figure 2C). Similarly, the absorption value at 652 nm was recorded in the mixed solution (20-mM glucose, 0.5-mM TMB, and 100-µg/mL AMS). In this process, AMS consumed glucose to generate H<sub>2</sub>O<sub>2</sub> and gluconic acid through the GOD-mediated reaction, polydopamine was degraded, and HGNs-Fc catalyzed H<sub>2</sub>O<sub>2</sub> to produce •OH for the TMB oxidation (Figure 2D). The results demonstrated that AMS exhibited CAT-like and POD-like activities, which could produce O<sub>2</sub> to overcome tumor hypoxia and decompose glucose into H<sub>2</sub>O<sub>2</sub> and then catalyze H<sub>2</sub>O<sub>2</sub> to •OH for an enhanced ROS treatment.





**Figure 2** (A) The generated oxygen of different concentrations AMS in  $\text{H}_2\text{O}_2$  solution. (B) The generated oxygen of different concentrations AMS in glucose solution. (C) Time-dependent TMB absorption in AMS solution including 10 mM  $\text{H}_2\text{O}_2$  and 0.5 mM TMB. (D) Time-dependent TMB absorption in AMS solution including 20 mM glucose and 0.5 mM TMB. (E) Absorption spectrum of DPBF upon 660 nm laser irradiation in AMS solution. (F) Absorption spectrum of DPBF upon 660 nm laser irradiation in AMS solution with  $\text{H}_2\text{O}_2$ . (G) Absorption spectrum of DPBF upon 660 nm laser irradiation in AMS solution with glucose. (H) ESR spectra of DMPO/ $\cdot\text{OH}$  collected from  $\text{H}_2\text{O}_2$  with AMS solution. (I) Temperature curves of different concentrations AMS under 808 nm laser irradiation ( $1.6 \text{ W/cm}^2$ ). (J) Thermal infrared photograph of different concentrations AMS under laser irradiation. (K) Temperature curves of AMS solutions under different power density laser irradiation. (L) Temperature changes curve of AMS under 808 nm laser irradiation ( $1.6 \text{ W/cm}^2$ ) for 10 min, and then turned off the laser.

## Measurement of $^1\text{O}_2$

The DPBF was used to analyze the  $^1\text{O}_2$  production ability of AMS. The absorption values of DPBF hardly changed under laser irradiation alone over 40 min (Figure S13, Supporting Information). The DPBF absorption of the AMS solution (100  $\mu\text{g/mL}$ , pH = 5.5) at 410 nm decreased upon 660-nm laser irradiation ( $0.2 \text{ W cm}^{-2}$ ) for 40 min (Figure 2E). Meanwhile, the DPBF absorption of the AMS solution (100  $\mu\text{g/mL}$ , pH = 5.5) containing 20-mM  $\text{H}_2\text{O}_2$  at 410 nm was detected to analyze the effect of  $\text{H}_2\text{O}_2$  on the  $^1\text{O}_2$  production. The increase in the  $^1\text{O}_2$  yield of AMS with  $\text{H}_2\text{O}_2$  was higher than that without  $\text{H}_2\text{O}_2$ , revealing that the  $\text{O}_2$  produced from the reaction of  $\text{MnO}_2$  and  $\text{H}_2\text{O}_2$  could increase the oxygen concentration and improve the production of the reactive oxygen species (ROS) generated by AMS (Figure 2F). In contrast, no significant difference in the DPBF absorption of Ce6 was found in the presence or absence of  $\text{H}_2\text{O}_2$ , which could be attributed to the fact that Ce6 did not catalyze  $\text{H}_2\text{O}_2$  to generate  $\text{O}_2$  in the  $\text{H}_2\text{O}_2$  solution. In addition, the DPBF absorption of the AMS solution (100  $\mu\text{g/mL}$ ) containing 20-mM glucose was detected for the  $^1\text{O}_2$  generation. Compared with the AMS solution (100  $\mu\text{g/mL}$ , pH = 5.5), AMS with had a relatively high  $^1\text{O}_2$  yield in the glucose solution. Glucose was decomposed to  $\text{H}_2\text{O}_2$  and gluconic acid through a GOD-mediated reaction; the generated  $\text{H}_2\text{O}_2$  was catalyzed to  $\text{O}_2$  by  $\text{MnO}_2$ , enhancing ROS production (Figure 2G). To analyze the properties of AMS to generate  $\cdot\text{OH}$ , DMPO/ $\cdot\text{OH}$  was captured by the trapping probe of dimethyl pyridine N-oxide (DMPO) and recorded by electron spin resonance (ESR). The four-line spectra of DMPO/ $\cdot\text{OH}$  were obtained by the AMS treatment. At the start of the reaction, no response signal had been detected. With the extension of time, the spectrum intensity increased, indicating that the AMS was gradually cracked, resulting in higher  $\cdot\text{OH}$  generation (Figure 2H).

## Photothermal Effect of AMS

To test the photo-thermal effect, AMS solutions of different concentrations were exposed for 10 min under the 808-nm laser irradiation. The concentration-dependent temperature rise curve and the thermal infrared photograph are presented in [Figures 2I and J](#); the temperature rose to 32.5, 37.2, 46.0, and 57.0 °C at the concentration of 50, 100, 200, and 300 µg/mL, respectively. For comparison, the water temperature only increased by 2.1 °C. The photo-thermal efficiency of AMS under the different intensities of laser irradiation was also analyzed, exhibiting a laser-power-dependent manner ([Figure 2K](#)). The photo-thermal conversion efficiency of AMS reached 41.3% ([Figure 2L](#)). The temperature of the material could be used to kill tumor cells.<sup>38–40</sup> The temperature that treated with cells reached to 50°C, the activity of tumor cells decreases, leading to apoptosis effects in the tumor cells. The results demonstrated that both AMS solutions had a good photo-thermal effect. In addition, the temperature change of AMS that treated by repeating on/off laser every other 5 min in ten cycles was within an acceptable range, indicating that AMS had a good photo-thermal stability ([Figure S14, Supporting Information](#)).

## Targeting Study of AMS and Drug Release

To investigate the targeting, AMS (100 µg/mL) was added to the HepG2 cells and incubated for different periods ([Figure 3A](#)). FITC-labeled AMS was aggregated to the HepG2 cells. At the incubation time of 3 min, the red fluorescence was barely visible. With the prolongation of the incubation time, the red fluorescence of dox was significantly enhanced and accumulated in the cell nuclei, demonstrating that the intracellular dox released after the structural changes of the oligonucleotide within the trigger after the cellular uptake of AMS. The prepared AMS could target to tumor cells, and released the doxorubicin. The released doxorubicin could induce cell DNA damage and increase the apoptosis rate of tumor cells. However, AMS had less damage to normal cells. This indicated that AMS had an efficient anti-tumor effect.

## Toxicity Assessment of AMS

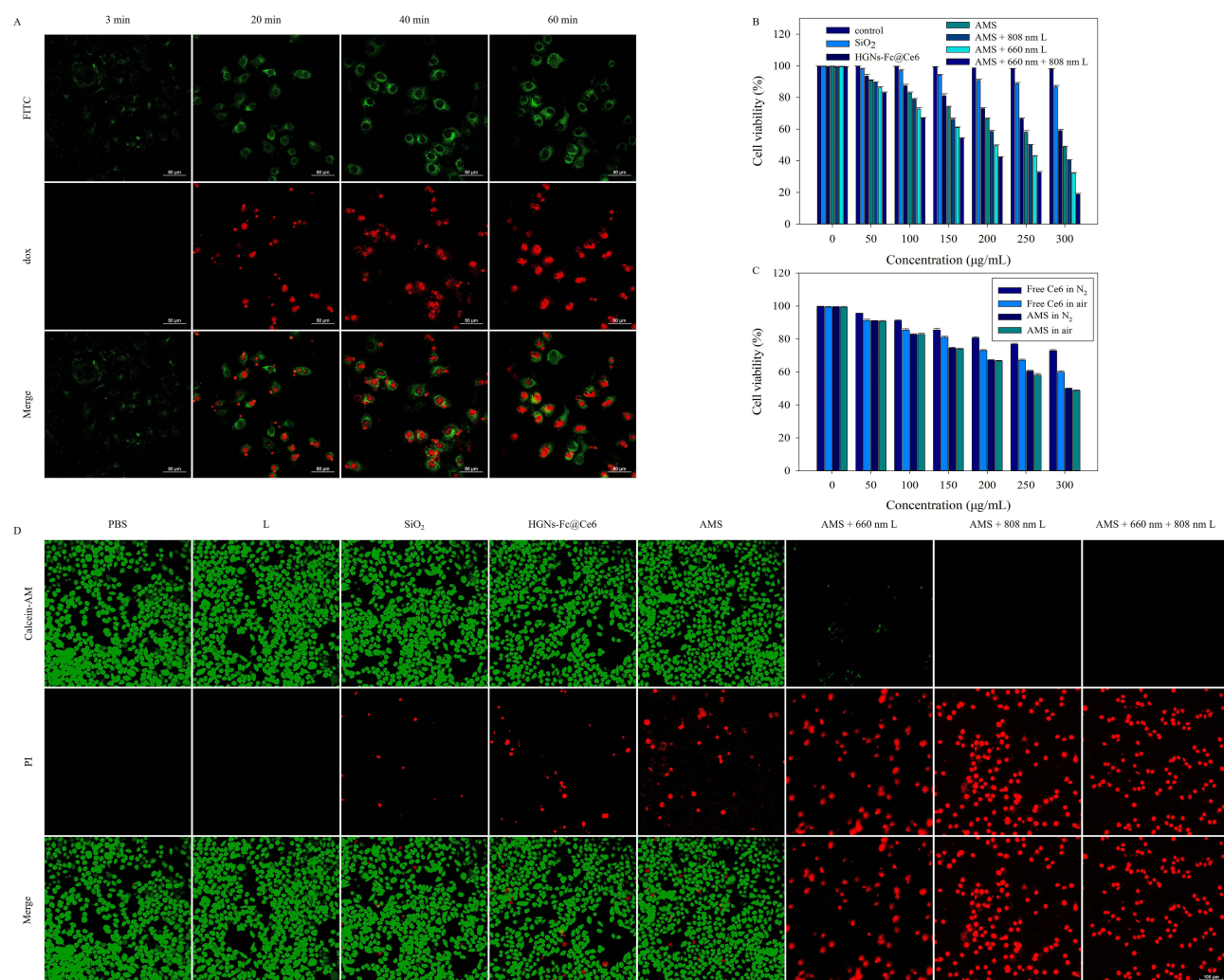
The toxicity of AMS was assessed by using the MTT test. HepG2 cells that were treated with PBS or laser irradiation exhibited no cell damage, and the cells treated with SiO<sub>2</sub> or HGNS-Fc@Ce6 exhibited mild toxicity. Compared with the AMS group, these cells exhibited varying degrees of toxicity ([Figure 3B](#)). The cell viability gradually decreased after treatment with increased concentrations of AMS with 808-nm laser irradiation, 660-nm laser irradiation, or 808- and 660-nm laser irradiation, and the cell viability at the concentration of 300 µg/mL reduced to 18% under the 660-nm and 808-nm laser irradiation, which was lower than that under the 660-nm laser irradiation (32%) or the 808-nm laser irradiation (40%). For comparison, 7702 cells were treated with the abovementioned nanomaterial under the same conditions, which exhibited relatively low toxicity ([Figure S15, Supporting Information](#)). The phototoxicity of AMS and Ce6 was found in air, while AMS exhibited an excellent photodynamic effect in an oxygen-deficient environment, which could be attributed to the O<sub>2</sub> production from AMS by oxidizing the abundant H<sub>2</sub>O<sub>2</sub> in the HepG2 cells ([Figure 3C](#)).

The calcein-AM and PI staining assays were used to assess the live/dead cells. As displayed in [Figure 3D](#), green fluorescence was observed in group of PBS or laser irradiation, indicating no apoptosis. While green fluorescence doped with red fluorescence was found in the cells treated with SiO<sub>2</sub>, rGO-Fc@Ce6, or AMS. The red proportion of the fluorescence increased after treatment with increased concentrations of AMS upon the 808-nm laser irradiation, 660-nm laser irradiation, or 808-nm and 660-nm laser irradiation, which indicated that the photo-thermal and photodynamic effect of AMS induced cell membrane rupture, leading to tumor cell apoptosis. The results revealed that combining the photo-thermal and photodynamic treatments could significantly improve the anti-tumor effect.

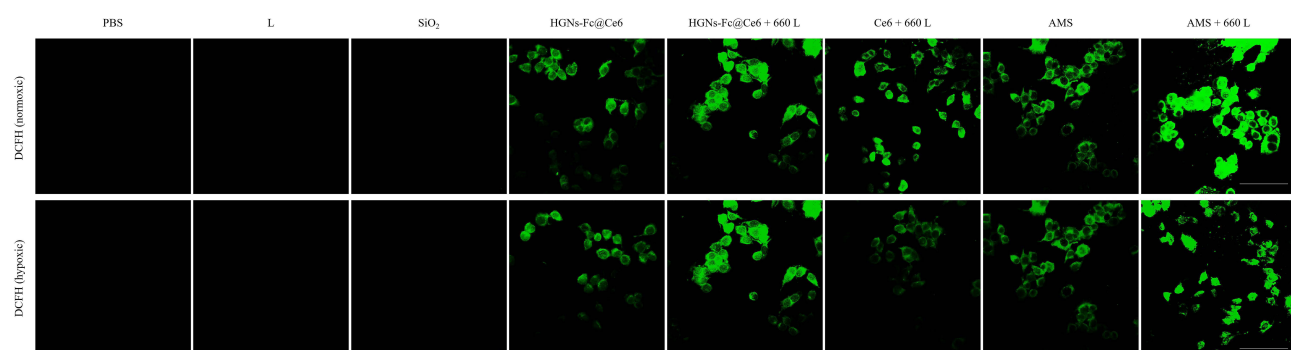
## Detection of ROS in vitro

DCFH-DA was oxidized into the green fluorescence of DCF by ROS, which could be used to detect cellular ROS. As displayed in [Figure 4](#), almost no fluorescence was found in the control group, laser irradiation group, or only the SiO<sub>2</sub> group, while green fluorescence was found in the HGNS-Fc@Ce6 group, which was attributed to the Fenton reaction between ferrocene and the H<sub>2</sub>O<sub>2</sub> over-expressed in tumor cells. The group of AMS + 660 nm or AMS + 660 nm + 808 nm irradiation had brighter green fluorescence than the HGNS-Fc@Ce6 group and the AMS group, which could be attributed to the production of <sup>1</sup>O<sub>2</sub> from Ce6 and •OH from ferrocene. The results depicted that the AMS exhibited an





**Figure 3 (A)** CLSM images of released dox at different time that incubated with AMS solution (100 µg/mL). Scale bar: 50 µm. **(B)** Cells viability of HepG2 cells that incubated with different concentrations of material (SiO<sub>2</sub>, HGNS-Fc@Ce6, AMS) with 808 nm laser irradiation (1.6 W/cm<sup>2</sup>), 660 nm laser irradiation (0.2 W/cm<sup>2</sup>) or both 808 nm and 660 nm laser irradiation. Scale bar: 100 µm. **(C)** Cells viability of HepG2 cells that incubated with different concentrations of free Ce6 and AMS in air and nitrogen. **(D)** Calcein-AM/PI dual staining images of HepG2 cells that incubated with different material (SiO<sub>2</sub>, HGNS-Fc@Ce6, AMS) with or without laser irradiation. Scale bar: 100 µm.



**Figure 4** CLSM images of ROS generation that HepG2 cells incubated with different material (SiO<sub>2</sub>, HGNS-Fc@Ce6, AMS) with or without laser irradiation in normoxic and hypoxic condition. Scale bar: 100 µm.

excellent photodynamic effect for tumor treatment. However, under the hypoxia condition, only the HepG2 cell group that was treated with AMS under 660-nm laser irradiation emitted bright green fluorescence, which indicated that AMS could increase oxygenation to efficiently stimulate ROS. The produced  $\bullet\text{OH}$  and  $^1\text{O}_2$  increase the ROS content of cells, and the enhanced ROS can produce more significant anti-tumor effect.

## Apoptosis Assessment of AMS

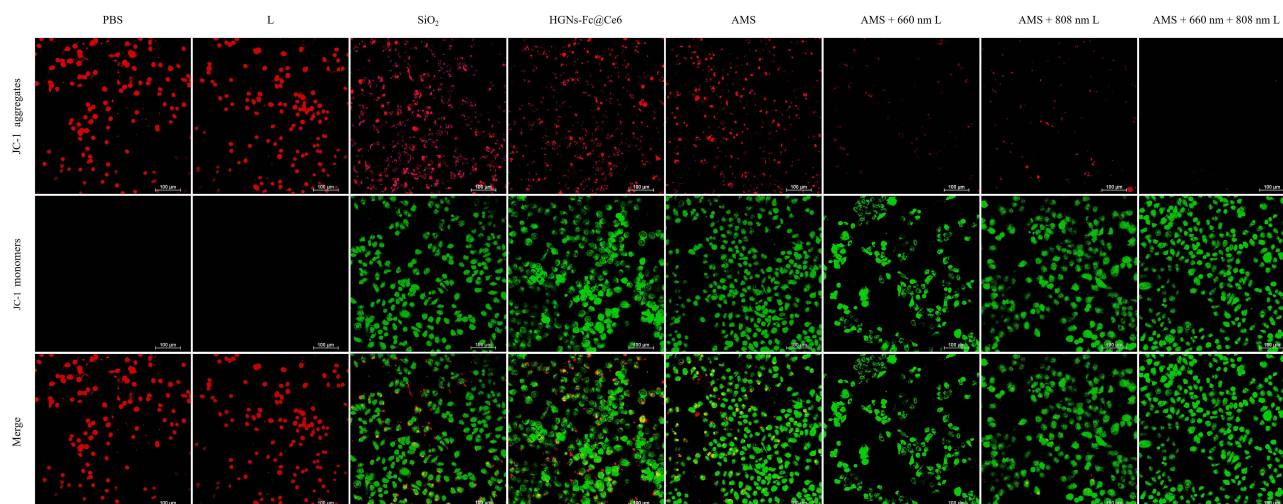
A JC-1 fluorescent probe was used to evaluate cell apoptosis by measuring the changes in the mitochondrial membrane potential. As displayed in [Figure 5](#), compared with the fluorescence emitted by the PBS or laser irradiation group, red fluorescence doped with green fluorescence was exhibited by the rGO-Fc@Ce6 or AMS group, which could be attributed to the generated highly toxic  $\bullet\text{OH}$  that killed the tumor cells. The apoptotic ratio increased in the cells treated with AMS under the 808-nm laser irradiation, 660-nm laser irradiation, or 808-nm and 660-nm laser irradiation, respectively, which demonstrated that AMS had excellent PPT and PDT for the tumor cells. These results were consistent with the MMT assay and the live/dead cell staining assays. The apoptosis rates of cells treated with AMS under 808nm or 660nm irradiation were 37.36%, 32.65%, respectively, which were significantly higher than those of treated with PBS or laser alone. The apoptotic ratios that treated with AMS under 808nm and 660nm laser irradiation was the highest in all schemes, and value reached to 54.74%. The data showed that AMS exhibited good anti-tumor effects under laser irradiation via synergistic photo-thermal and photodynamic treatment ([Figure S16](#), [Supporting Information](#)).

## In vivo Biocompatibility Assessment

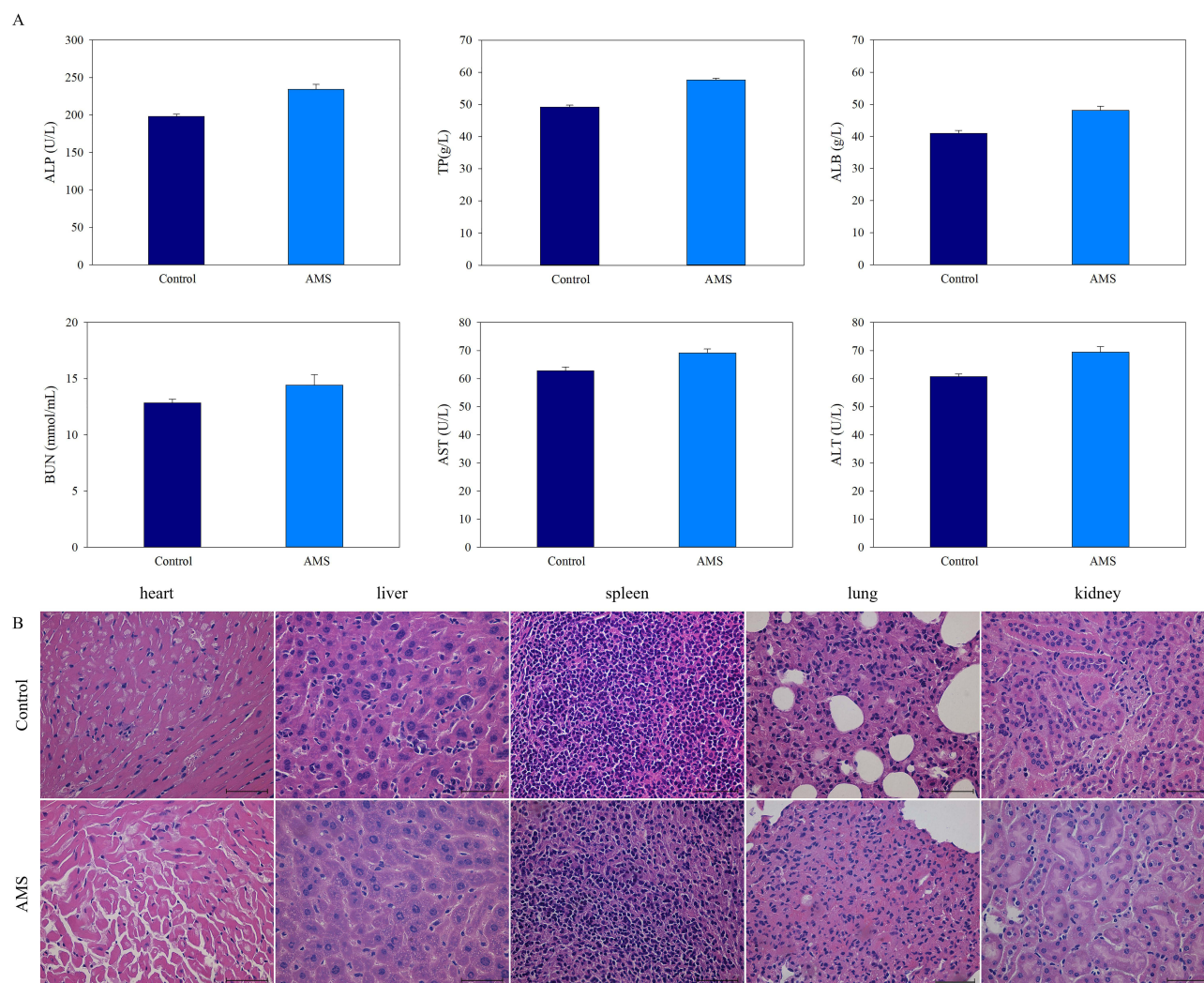
To analyze the biosafety in vivo, the AMS solution (200  $\mu\text{g/mL}$ ) was injected into healthy mice via the tail vein, and the blood biochemical indexes were monitored 24 h after the injection. No significant difference was observed between the AMS group and the PBS group, and the values were maintained in the normal range, which implied that AMS did not have a negative effect at the given doses, also indicated that AMS could be safely used in tumor bearing mice ([Figure 6A](#)). The toxicity of the major organs (kidney, heart, spleen, liver, and lung) was analyzed via the H&E staining assay, indicating the rather limited damage to major organs treated with AMS or PBS ([Figure 6B](#)). Therefore, AMS had good bio-safety and seemed promising for subsequent tumor treatment.

## In vivo Dual-Modal Imaging

To analyze the distribution in vivo, a cy5.5-labeled AMS solution (200  $\mu\text{L}$ , 100  $\mu\text{g/mL}$ ) was intravenously injected into the mice. The fluorescence signal was recorded, and the background signal before the injection was subtracted. The fluorescent-labeled AMS was enriched in the tumor site with blood circulation after the injection, and the fluorescence signal of the



**Figure 5** JC-1 of HepG2 cells that treated with PBS, laser irradiation,  $\text{SiO}_2$  (100  $\mu\text{g/mL}$ ), HGNS-Fc@Ce6 (100  $\mu\text{g/mL}$ ), AMS (100  $\mu\text{g/mL}$ ), AMS + 660 nm L (0.2  $\text{W/cm}^2$ ), AMS + 808 nm L (1.6  $\text{W/cm}^2$ ), AMS + 660 nm (0.2  $\text{W/cm}^2$ ) + 808 nm L (1.6  $\text{W/cm}^2$ ). Scale bar: 100  $\mu\text{m}$ .



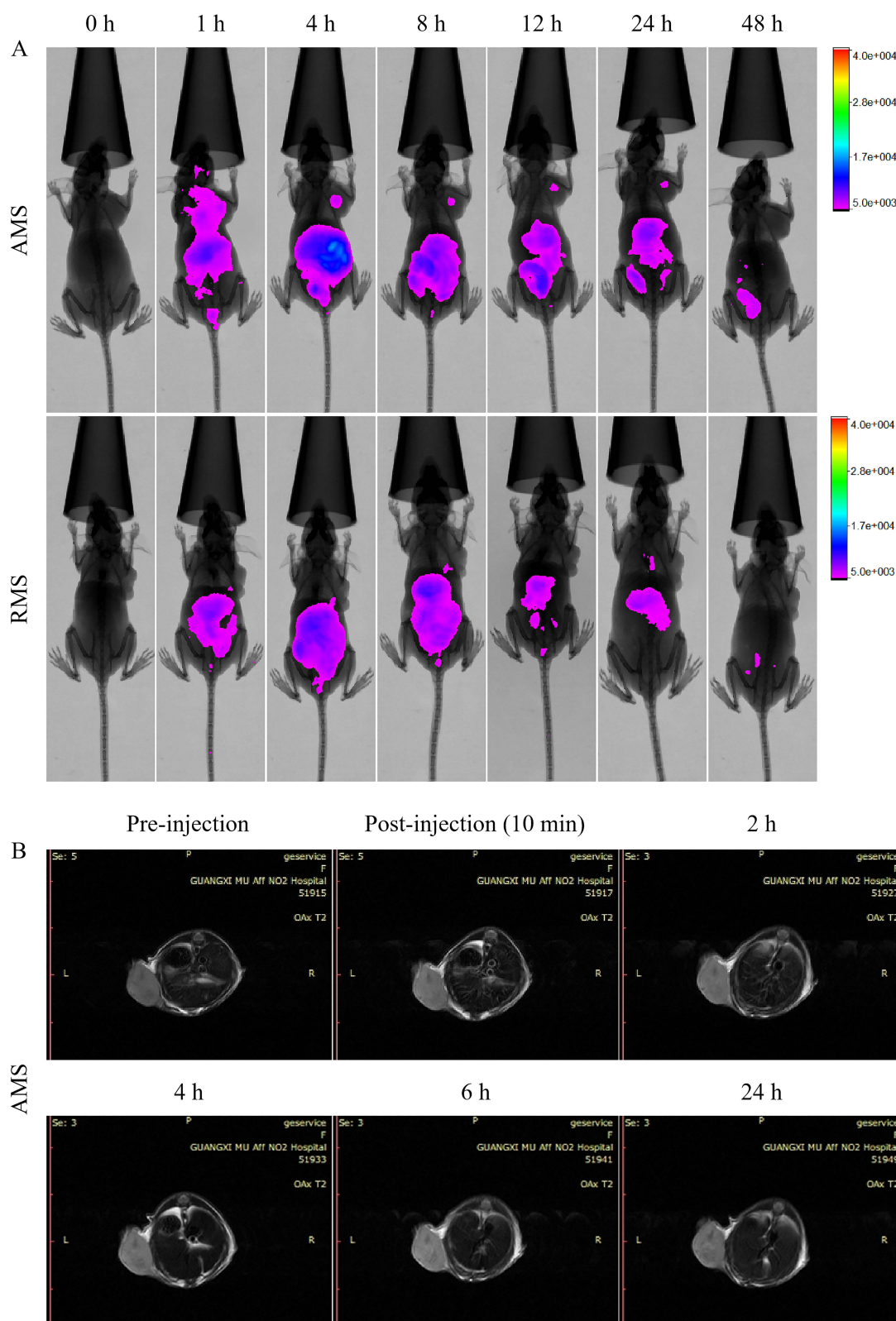
**Figure 6 (A)** Serum biochemistry assay of mice injected with or without AMS. **(B)** H&E of organs including heart, liver, spleen, lung, and kidney that after injection with AMS (100  $\mu$ L, 100  $\mu$ g/mL) solution for 24 h.

tumor cells gradually enhanced. The signal value reached the maximum at 4 h and then gradually weakened. After 72 h, the fluorescence of the tumor site disappeared. The main organs and the tumor were stripped, and the fluorescence intensity was measured to analyze the distribution of AMS in vivo. These results indicated that AMS mainly enriched the tumor site, liver, and kidney. As the control, the labeled random sequence (RMS) barely enriched the tumor sites, and the fluorescent signal remained mainly in the organs of the mice (Figure 7A). MRI imaging was carried out in the HepG2 tumor-bearing mice, and the T2 signal was found in the tumor cells treated with AMS, indicating the good MRI capability of AMS (Figure 7B). The data showed that dual-modal imaging could guide and achieve visual monitoring of tumors. In addition, the photo-thermal imaging of tumor bearing mice was shown in Figure S17. Compared with the control group, the temperature of the mice that treated with AMS reached to 56°C, indicating that AMS had a good photo-thermal performance for photo-thermal therapy.

## In vivo Anti-Tumor Assays

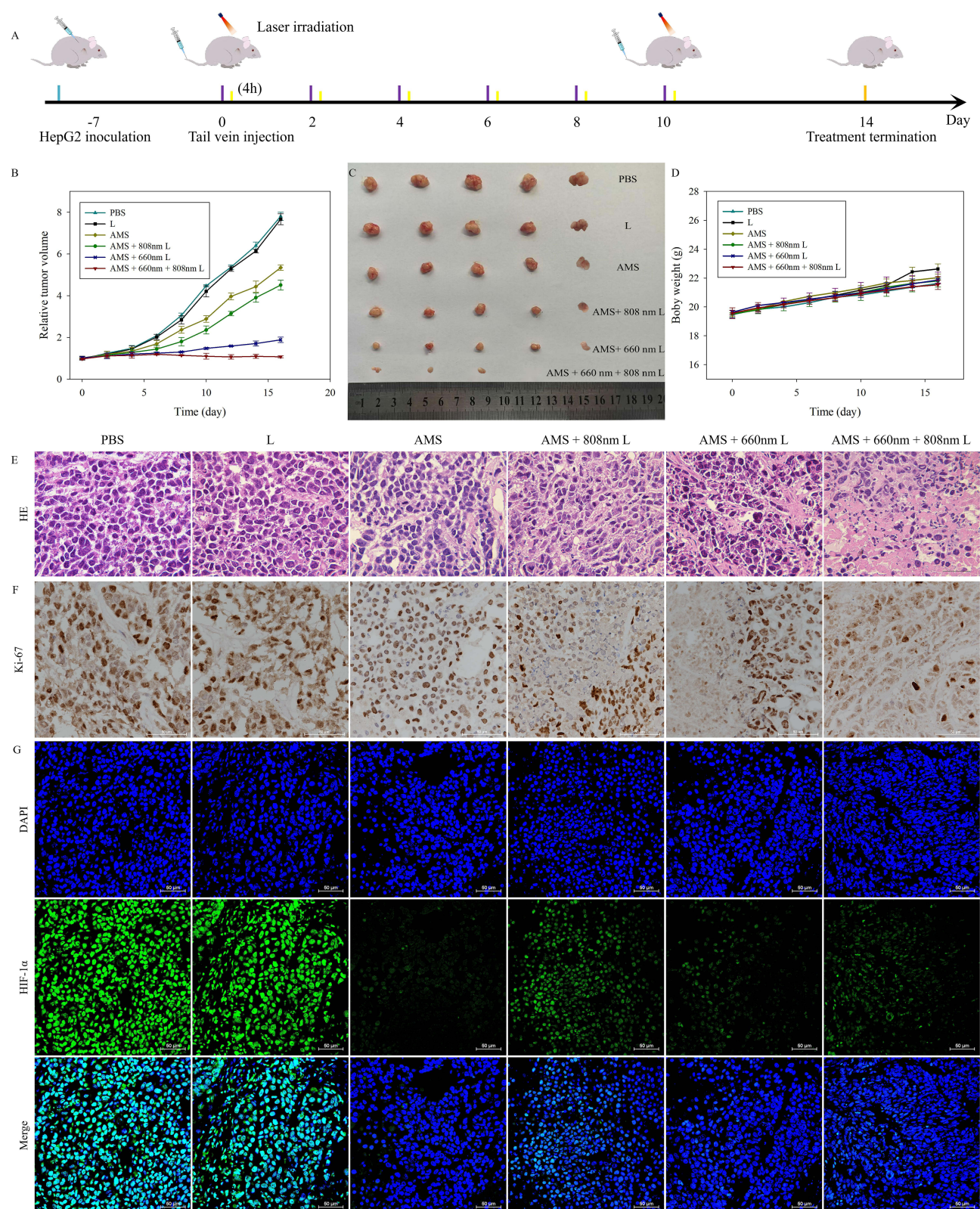
The HepG2 tumor-bearing mice were randomly divided into six groups (N = 6): (1) control group (PBS injection), (2) L group (660 nm + 808 nm laser irradiation), (3) AMS, (4) AMS + 660 nm L, (5) AMS + 808 nm L, (6) AMS + 660 nm + 808 nm L. The mice were injected with AMS (100  $\mu$ L, 200  $\mu$ g/mL) and irradiated with the 808-nm laser (1.6 W  $\text{cm}^{-2}$ , 5 min), 660-nm laser (0.2 W  $\text{cm}^{-2}$ , 5 min), or the 808-nm (1.6 W  $\text{cm}^{-2}$ , 5 min) and 660-nm (0.2 W  $\text{cm}^{-2}$ , 5 min) laser 4 h after the injection. The tumor sizes and body weights of the mice were recorded every two days. The mice were tail vein injected with AMS and irradiated with the laser 4 h after the injection. The figure of treatment schematic diagram was shown in the Figure 8A. The excised tumor





**Figure 7** (A) In vivo fluorescence imaging of mice that intravenous injection of AMS or RMS. (B) MRI imaging of mice after intravenous (i.v.) injection of 100  $\mu$ L AMS (100  $\mu$ g/mL).

photographs and the relative tumor volume after the different treatments are displayed in Figures 8B and C; the tumor volume in the PBS group or the L group continued to increase, which signified that there was no inhibitory effect on the tumor growth. While the AMS group demonstrated a slower tumor growth, which could be attributed to the generated  $\bullet$ OH of the Fenton effect.



**Figure 8** (A) Scheme of in vivo antitumor efficacy of AMS. (B) Relative tumor volume of mice after various treatments as indicated. (C) Photographs of the tumor dissection. (D) Body weight variation with various treatment. (E–G) H&E, Ki-67 and HIF-1α staining of tumor tissue from various treatment. Scale bar: 50 μm.



Compared with that in the AMS group, the tumor suppressive effect was more pronounced in the groups of AMS + 660 nm L and AMS + 808 nm L, which could be attributed to the O<sub>2</sub> production ability of AMS for enhanced photodynamic therapy and the photo-thermal effect of GO and PDA. The tumor suppression rate reached the maximum in the group of AMS + 660 nm + 808 nm L, the generated •OH and <sup>1</sup>O<sub>2</sub> enhance the ROS content and had a ROS killing effect on tumor cells. Simultaneously, the generation of dissolved oxygen could improve the hypoxic environment of tumor cells, increased the catalytic activity of glucose oxidase, and enhance the efficacy of doxorubicin in the tumor site. In addition, the increased O<sub>2</sub> content could enhance the photodynamic effect for the tumor treatment. The data indicated the significant combined photo-thermal therapy and photodynamic therapy effect of AMS in vivo. Moreover, the weight of the mice between the groups had little significant difference during the treatment period (Figure 8D). Compared with the PBS or L groups, the H&E and Ki-67 staining showed the most severe damage to the cells treated in the AMS + 660 nm + 808 nm L group (Figure 8E and F). In addition, because of the excellent CAT-like and POD-like catalytic capability of AMS, the produced O<sub>2</sub> was prospected to ameliorate the hypoxic nature of tumors. The probe of HIF-1α was used to assess the hypoxia improvement in tumors after treatment with AMS. The weak green fluorescence (antipimonidazole antibody) was observed when the tumor was treated with AMS in the presence or absence of laser irradiation, demonstrating that the hypoxia environment had been improved and was conducive to reducing the PDT resistance (Figure 8G), which can produce higher anti-tumor effects than that with PDT alone in previous study.

## Conclusions

We constructed a mesoporous silica-based nanoplatfrom for the combination therapy of tumors, which consisted of HGNS-Fc, MnO<sub>2</sub>, and AS1411-aptamer. In the nanomaterial, HGNS-Fc possessed excellent catalase-like activity, catalyzing H<sub>2</sub>O<sub>2</sub> to generate highly toxic free radicals to kill the tumor cells. The loaded Ce6 on HGNS-Fc could be efficiently released into tumors for enhanced PDT. Under the laser irradiation, the prepared AMS exhibited efficient photo-thermal and photodynamic effects. Moreover, glucose was catalyzed to produce H<sub>2</sub>O<sub>2</sub> and gluconic acid by the GOD-mediated reaction in the tumor microenvironment, and the generated H<sub>2</sub>O<sub>2</sub> was decomposed to produce O<sub>2</sub>. The increased oxygen content could improve the hypoxic environment of the tumor and effectively reduce the resistance to PDT. Compared with the control group, the tumor volume in group that treated with AMS under 808nm and 660nm laser irradiation decreased approximately 80%. The immunohistochemical image of Ki-67 showed that the proliferation rate of tumor cells treated with AMS under 808nm and 660nm laser irradiation was significantly lower than that of the PBS or laser alone group. The immunofluorescence image of HIF-1α showed that the fluorescence intensity of control group was 60% of that AMS + 660 nm + 808 nm laser group, indicating that AMS could improve the content of dissolved oxygen in tumor microenvironment and ameliorate the therapeutic effect of PDT. The data demonstrated that AMS could enrich at the tumor sites and could be combined with photo-thermal and photodynamic therapy to inhibit tumor cell growth.

## Supplementary Materials

Supplementary material of this article can be found in the online.

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## Disclosure

The authors declare no competing interests in this work.

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